TMS as a Tool for Neuroscience

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Non-invasive Brain Stimulation (NIBS)

 NIBS: applying energy to the brain in a noninvasive way to modulate its activity
– here focused on electromagnetic energy





Modulatory effects of TMS

Acute effects - Mapping





Direct activation of circuits

- Elicits observable responses (motor twitch)
- Disrupts (e.g. speech arrest) or facilitates (e.g. speeds RT) ongoing processing

Lasting effects - Modulation

Neuroplasticity

- Synaptic efficacy, LTP/LTD
- Modulation of cortical excitability
- Modulation of functional connectivity

The space of all possible parameters for dosing in therapeutic Rx is extremely large





Target Localization Methods

- Scalp coordinate system: 10-20 EEG system
- Strict Anatomic pick a spot based on a structural MRI
 - Problem: not functional location
- Functional imaging using group analysis
 - Take structural scan, transform to Talairach, find probabilistic location of behavior (from Group study), reverse transform, find the likely spot
 - Problem only in the neighborhood in most subjects
- Functional Imaging on an individual basis
 - Do activation imaging, find region, direct TMS there



Using scalp/external anatomy to target

Squares show extent of possible cortical locations an electrode might end up over on any individual

Homan et al., 1987

Function-guided TMS Frameless Stereotaxy: Neuronavigation



Figure 1: Increases in rCBF in prefrontal cortex while performing a Sternerg



Study comparing 10/20, structural MRI, group fMRI, and individualized fMRI methods



Stroop-like task

Sack et al., 2009, J Cog Neurosci 21: 207-221

Incongruent INeutral Con. 720 670 620 RT (in ms) 570 520 470 420 RIPS Sham UPS

TMS to parietal cortex modulates RT





Individual fMRI targeting results in greatest statistical power for the TMS effect



Targeting precision: Robot Arm



Figure 1. Schematic of the Robot Arm System. System components include: (a) Robot arm (Adept Viper s850) with power supply unit and remote control, (b) control unit for robot arm, (c) NDI Spectra infrared camera, (d) stimulator, (e) chair with neck rest.

Stimulating one cortical site engages a network



Pre-Post imaging with offline TMS

C Concurrent TMS + fMRI / PET



Concurrent imaging/TMS:

TMS/fMRI Interleaving



Exploring long-distance network effects with simultaneous TMS-fMRI



Picture working memory task Faces (FFA activity) Places (PPA activity)

TMS to DLPFC during difficult conditions affects posterior activity



Feredoes et al., PNAS 2011 108: 17510-17515

Overcoming depth limitation of TMS: Noninvasive Focal Deep Brain Stimulation



BA25 of interest as a target of stimulation in depression- but too deep to effectively reach with TMS



Noninvasive deep brain stimulation paradigm: Results



N=10

Individualized targeting



Activation (% ROI w z>2.3) increased with TMS dosage



120% MT – 80% MT contrast; significant cluster (z>2.3, p<.05) in BA25 seed region





Coil Shape

Magnetic Field Characteristics:







Figure 8

Double Cone

Round

Metal Core







Effects of coil orientation:

Current direction relative to gyri



Inter-individual variability

A. Thielscher et al. / NeuroImage 54 (2011) 234-243



Balslev et al., Journal of Neuroscience Methods 162 (2007) 309-313

| | | | Motor thresholds at 8 coil orientations | | | | | | | | PC |
|------|------|------|---|----|----|----|----|----|----|----|--------|
| Subj | Sess | Corr | А | AL | L | PL | Ρ | PM | м | AM | angle° |
| 5 | 1 | 0.98 | 70 | 70 | 69 | 61 | 67 | 70 | 70 | 70 | 38.50 |
| | 2 | | 70 | 70 | 70 | 60 | 65 | 70 | 70 | 70 | 31.27 |
| 6 | 1 | 0.96 | 63 | 69 | 59 | 48 | 54 | 68 | 61 | 53 | 42.76 |
| | 2 | | 60 | 70 | 59 | 49 | 55 | 70 | 66 | 55 | 37.33 |
| 4 | 1 | 0.95 | 60 | 67 | 54 | 46 | 53 | 65 | 66 | 58 | 37.78 |
| | 2 | | 60 | 69 | 61 | 45 | 55 | 70 | 68 | 58 | 34.24 |
| 7 | 1 | 0.95 | 67 | 66 | 61 | 59 | 59 | 70 | 64 | 60 | 44.20 |
| | 2 | | 69 | 69 | 62 | 57 | 61 | 78 | 71 | 59 | 47.90 |
| 9 | 1 | 0.89 | 66 | 64 | 48 | 44 | 51 | 63 | 58 | 50 | 36.62 |
| | 2 | | 55 | 66 | 48 | 37 | 42 | 62 | 55 | 44 | 49.76 |
| 8 | 1 | 0.88 | 70 | 88 | 78 | 64 | 69 | 76 | 80 | 68 | 60.18 |
| | 2 | | 72 | 86 | 74 | 59 | 68 | 86 | 81 | 62 | 52.28 |
| 2 | 1 | 0.86 | 60 | 70 | 57 | 48 | 56 | 70 | 70 | 56 | 36.30 |
| | 2 | | 59 | 70 | 61 | 54 | 47 | 69 | 70 | 58 | 24.65 |
| 1 | 1 | 0.83 | 65 | 70 | 59 | 46 | 55 | 70 | 61 | 54 | 45.15 |
| | 2 | | 70 | 64 | 55 | 52 | 58 | 67 | 66 | 55 | 53.56 |
| 10 | 1 | 0.78 | 55 | 66 | 54 | 50 | 48 | 60 | 58 | 51 | 35.63 |
| | 2 | | 55 | 60 | 53 | 48 | 48 | 57 | 58 | 58 | 27.35 |
| 3 | 1 | 0.72 | 70 | 70 | 66 | 63 | 68 | 70 | 70 | 66 | 50.18 |
| | 2 | | 65 | 70 | 65 | 64 | 70 | 70 | 70 | 65 | 45.03 |
| 12 | 1 | 0.70 | 59 | 66 | 50 | 52 | 48 | 55 | 60 | 60 | 39.17 |
| | 2 | | 62 | 65 | 52 | 55 | 57 | 67 | 67 | 60 | 42.93 |
| 11 | 1 | 0.60 | 40 | 53 | 53 | 50 | 40 | 50 | 54 | 51 | 88.50 |
| | 2 | | 50 | 54 | 51 | 46 | 46 | 52 | 58 | 50 | 68.50 |
| 13 | 1 | 0.41 | 24 | 29 | 31 | 34 | 24 | 29 | 30 | 37 | 24.95 |
| | 2 | | 32 | 33 | 36 | 36 | 31 | 38 | 36 | 33 | 6.75 |

Intensity

- Direct effects are clear: with greater intensity, have greater effective depth and spread
 - Risk of seizure
- Also more subtle effects: e.g., paired-pulse
 - Subthreshold effects may be profound- As the clear effects of tiny voltage changes caused by tDCS point out
- Dosage: Set relative to individual motor threshold for convenience - no other benchmark readily available

| Hz | 100% | 110% | 120% | 130% | 140% |
|----|-------|-------|------|------|------|
| 1 | >1800 | >1800 | 360 | >50 | >50 |
| 5 | >10 | >10 | >10 | <10 | 7.6 |
| 10 | >5 | >5 | 4.2 | 2.9 | 1.3 |
| 20 | 2.05 | 1.6 | 1.0 | 0.55 | 0.35 |
| 25 | 1.28 | 0.84 | 0.4 | 0.24 | 0.2 |

% Motor Threshold

Wassermann. Electroencephalogr Clin Neurophysiol. 1998 Jan;108(1):1-16.

TMS Dosage Parameters

- Spatial/Targeting
 - xyz position in space
 - Target localization method
 - Magnetic field characteristics: Determined by
 - Coil shape
 - Coil orientation
 - Intensity
- <u>Temporal</u>
 - Waveform
 - Frequency
 - Inter-train interval
 - Cumulative effects:
 - train duration
 - # trains/session
 - # sessions



Waveform matters:

A comparison of the standard biphasic (cosine shape) with rectangular bidirectional and unidirectional waveforms



size

Normalized MEP

N = 13 Standard 1 Hz "inhibitory" paradigm

In this case, 1 Hz trains with the standard waveform did not result in lower MEP amplitude, while they did using rectangular waveforms

Goetz et al., 2016

TMS frequency

Rule of thumb:

High frequency (>3Hz) <u>up</u>-regulates cortical excitability

Low frequency (1 Hz) <u>down</u>-regulates cortical excitability





fMRI-guided rTMS paradigm: Working Memory (WM) Task



TMS enhancement of working memory



Site specific effect: mParietal but not DLPFC

Frequency specific effect: 5 Hz rTMS during the retention phase reduced RT for set size 1 and 6 (p<0.01).





Task Phase specific effect: With a new group (N=22), 5Hz to mPar reduced RT only during retention period

mPar active during probe?

Luber et al Brain Research 2007;1128:120-129

TMS Remediation of Memory in Aging





5Hz rTMS to PM <u>before</u> retention period improved RT and accuracy in young group but not elderly 5Hz rTMS to LOC <u>during</u> retention period improved RT in both young group and elderly

Elderly

*p<0.05; n=34

*

Young

LOC

1600

1500

1400

1300

1200

1100

1000

900

800

700

600

Reaction Time (ms)

TMS enhancement: Tapping into brain's oscillatory dynamics?

2 s burst at peak alpha frequency (but not peak-3Hz or 20 Hz) immediately prior to trial increased accuracy of mental rotation

Klimesch et al., 2003 Eur J Neuosci 17: 1129-1133





5 pulses at 10 Hz (but not 5 or 20 Hz) immediately prior to trials enhanced target detection

Romei et al., 2010, J Neurosci 30: 8692-8697

Another frequency effect: Priming of "LTD-like" Inhibition



Interaction of Frequency, Duration and ITI

- Theta Burst Stimulation (TBS)
- 2 nested "natural" frequencies:
 - Burst of 50 Hz (gamma) given at 5 Hz (theta)
- Produces sustained inhibition or facilitation
 - LTP/LTD-like
- Effects require:
 - a much shorter duration (40 s/192 s)
 - a lower intensity (90% active MT)
- Potential clinical applications unexplored



Duration: Cumulative effects

Acute effects - Mapping





Direct activation of circuits

- Elicits observable responses (motor twitch)
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Long-lasting enhancements: creating LTP/LTD-like plasticity effects



Exploring the spatio-temporal dynamics of brain networks with simultaneous TMS-EEG

-Changes in topographic EEG activity due to TMS pulses Illmoniemi et al., 1997



Observing LTP-like effects using simultaneous TMS/EEG



Esser et al., 2006 Brain Res Bull 69: 86-94

100

Transcranial Direct Current Stimulation



- Direct current (1 mA) polarizes cortex
- Anodal facilitates, Cathodal inhibits
- Effects last hrs
- Safe, painless
- Enhances verbal fluency, word recall, recovery of function post stroke
- Cheap, portable



TMS-tDCS Strengths / Limitations

Temporal precision

- TMS: Pulse <1ms, useful complement to imaging & EEG; can modulate frequencies
- tDCS: low resolution: offline, pre-post changes

Spatial resolution

- TMS: ~0.5 cm; has transsynaptic action but E-field cannot be focused at depth
- tDCS: low resolution (although can be improved)

Mechanisms of action

- Both are tools to establish causality, to test hypotheses generated by imaging and EEG
- But TMS has a larger range of effects: a better toolbox

Summary: State of the art and the future

- The science and technology of TMS spatial parameters have become well-developed, in the sense that we can deliver a specific dose with precision
 - Neuronavigation, TMS/fMRI, TMS/EEG, robotic coil positioning, realistic head modeling
- But what happens next- the interaction of the TMS with the brain (the temporal parameters)- is less well-understood
 - TMS waveform <-> membrane time constants
 - TMS frequency <-> endogenous oscillations
 - Train duration and ITI <-> LTP and plasticity
 - Repeated TMS sessions <-> long term network changes
- We can aim, and we know we cause changes- but we are just learning how to direct the changes

NIMH Experimental Therapeutics & Pathophysiology Branch: Noninvasive Neuromodulation Unit (NNU)









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