Functional MRI Contrast and Limits of Spatial and Temporal Resolution

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&

Functional MRI Facility

http://fmrif.nimh.nih.gov

Functional Contrast

- **Volume (gadolinium)**
- **BOLD**
- **Perfusion (ASL)**
- **$\Delta CMRO_2$**
- **ΔVolume (VASO)**
- **Neuronal Currents**
- **Diffusion coefficient**
- **Temperature**

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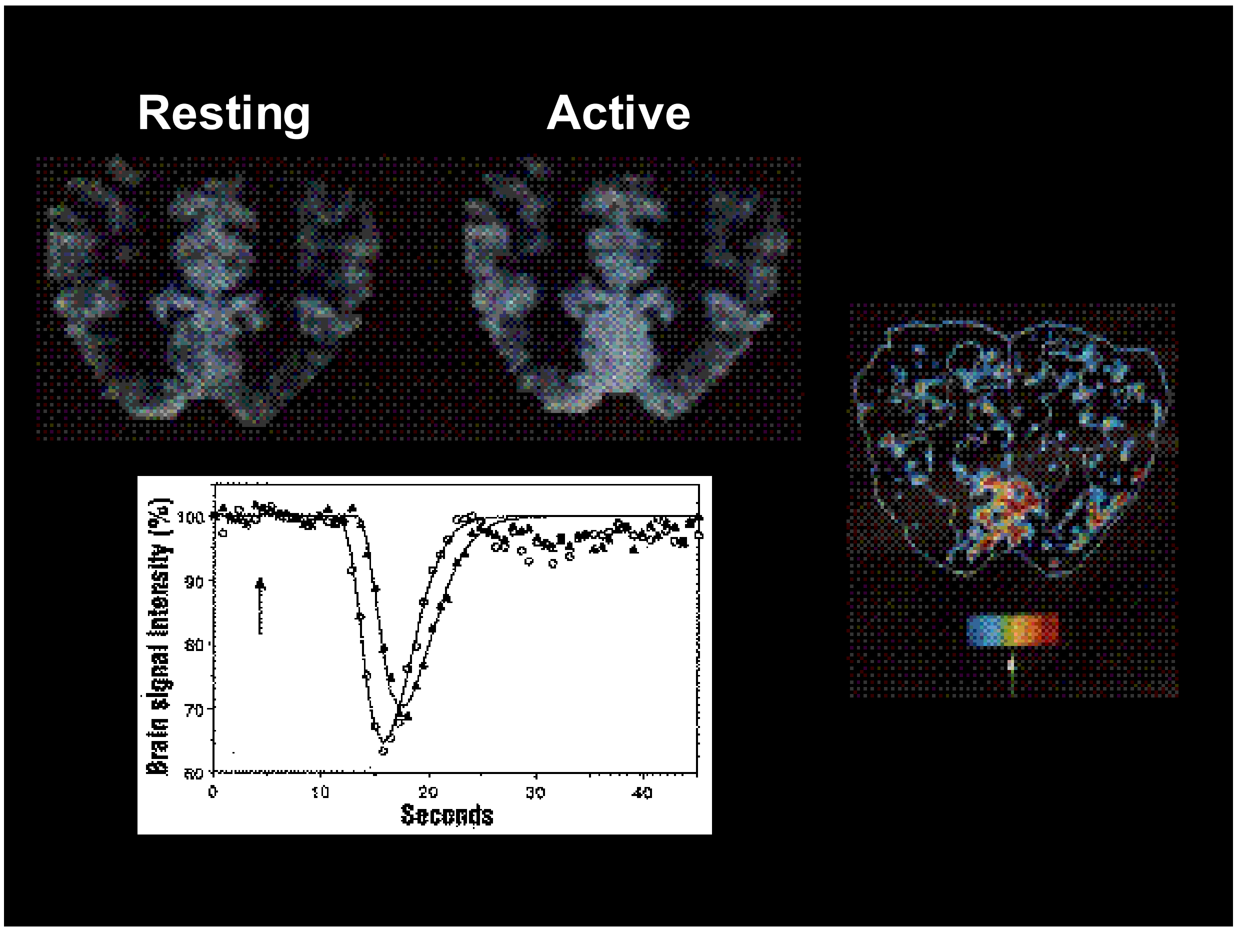
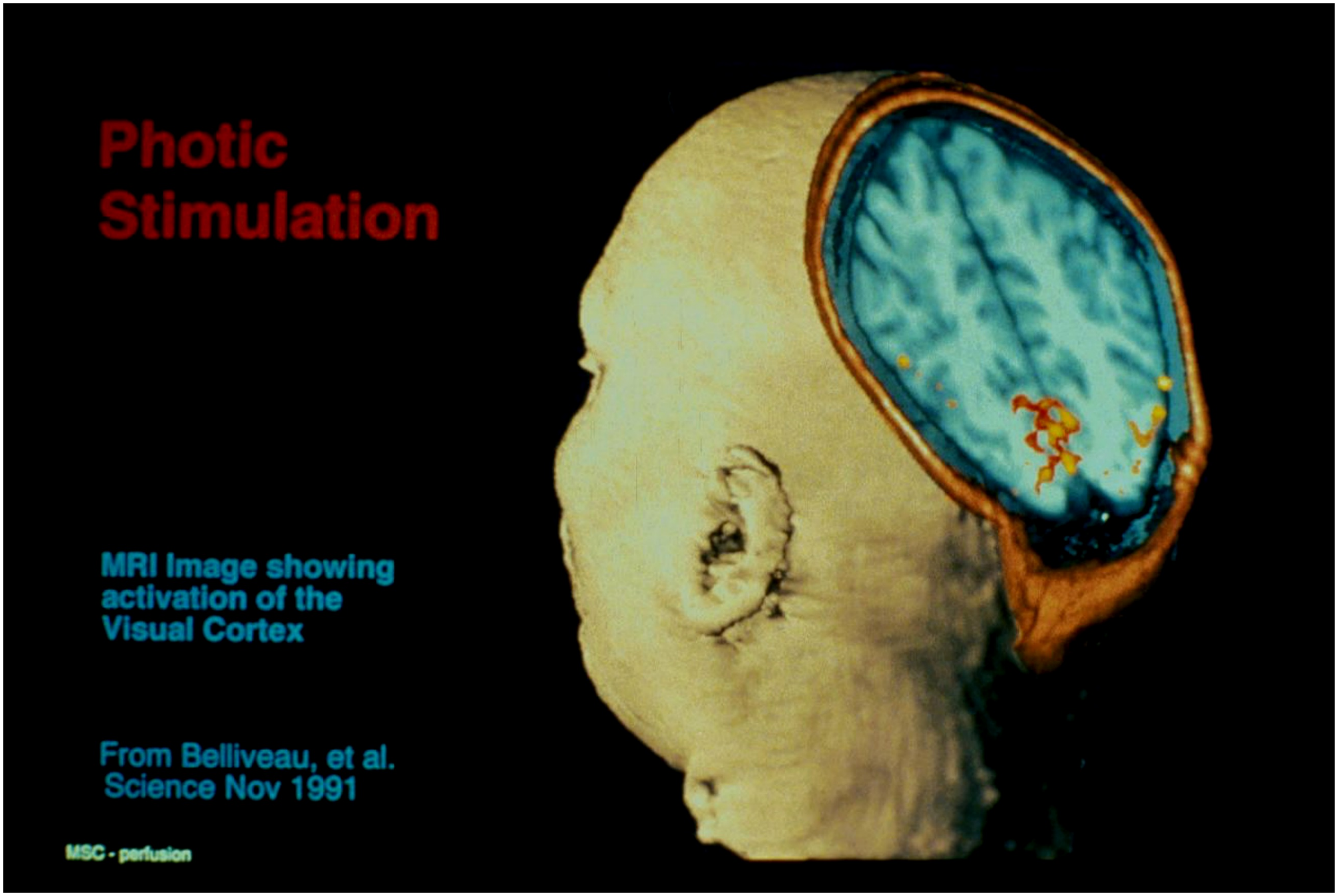
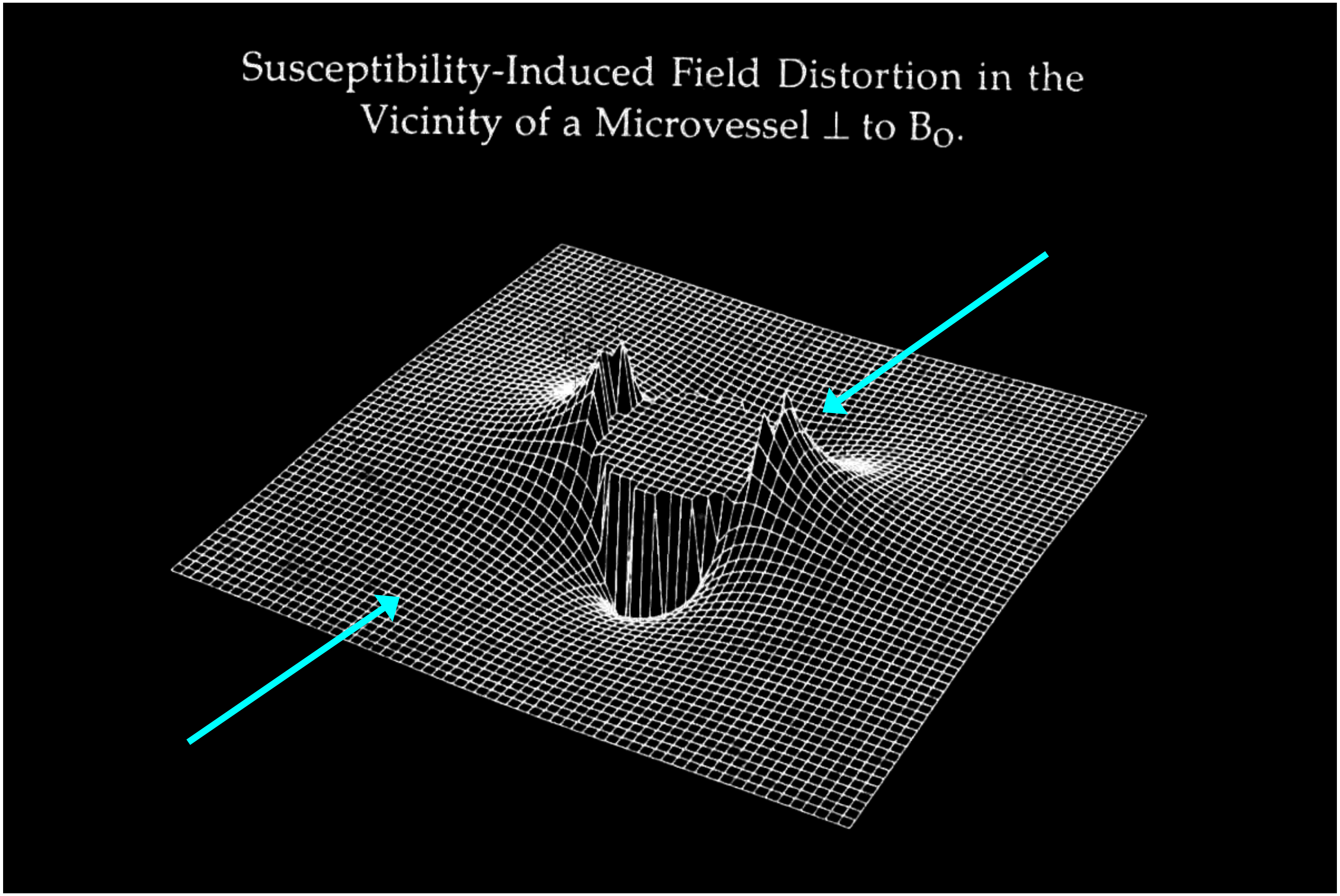
Blood Volume Imaging

Susceptibility Contrast agent bolus injection and time series collection of T2* or T2 - weighted images

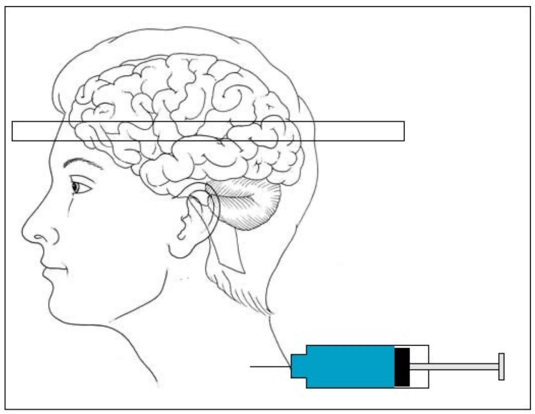


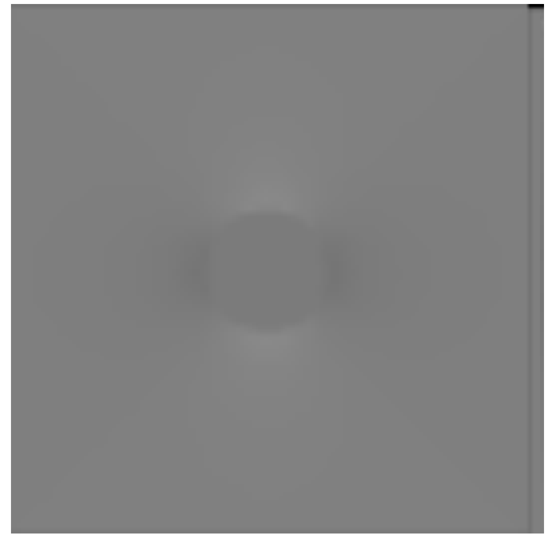

Photic Stimulation
MRI Image showing activation of the Visual Cortex
From Belliveau, et al. Science Nov 1991
MSC - perfusion

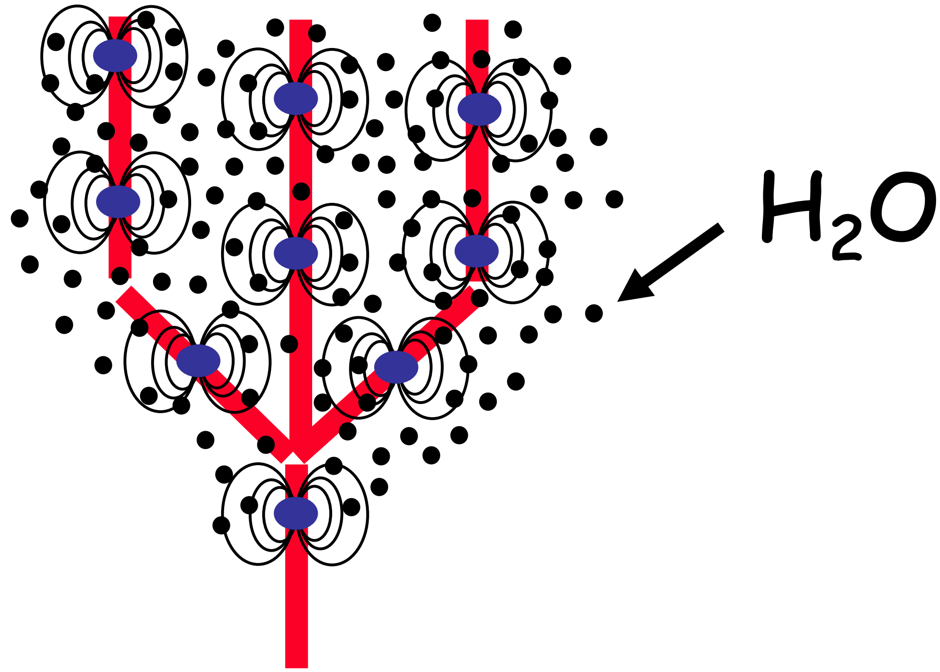
Susceptibility Contrast



Addition of paramagnetic compound to blood







Courtesy Larry Wald

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Cerebral Tissue Activation

Local Vasodilatation

Increase in Cerebral Blood Flow and Volume → **Oxygen Delivery Exceeds Metabolic Need**

Increase in Capillary and Venous Blood Oxygenation

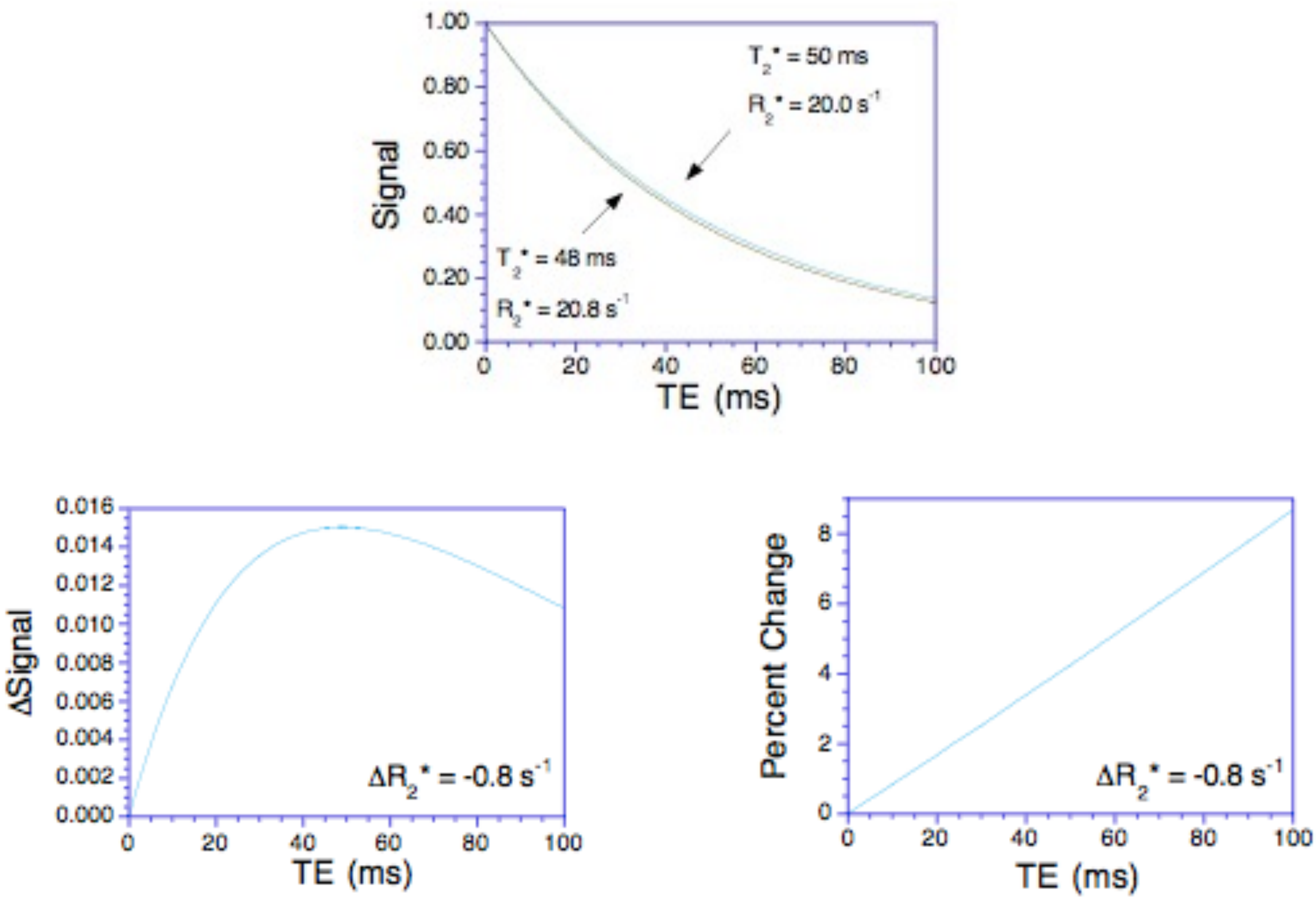
Decrease in Deoxy-hemoglobin

Deoxy-hemoglobin: paramagnetic
Oxy-hemoglobin: diamagnetic

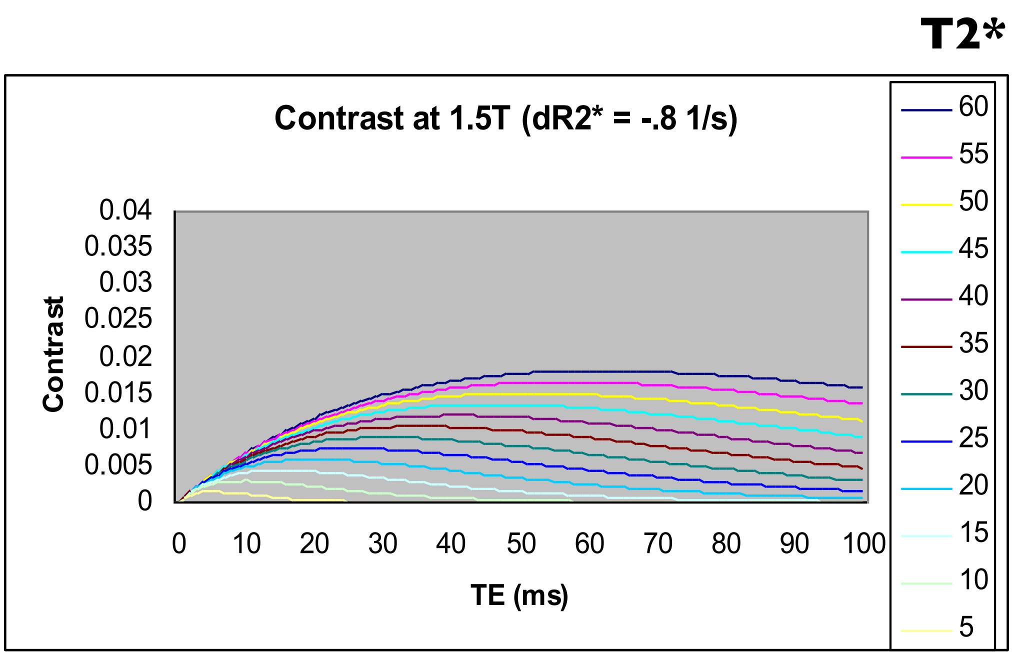
Decrease in susceptibility-related intravoxel dephasing → **Increase in T2 and T2***

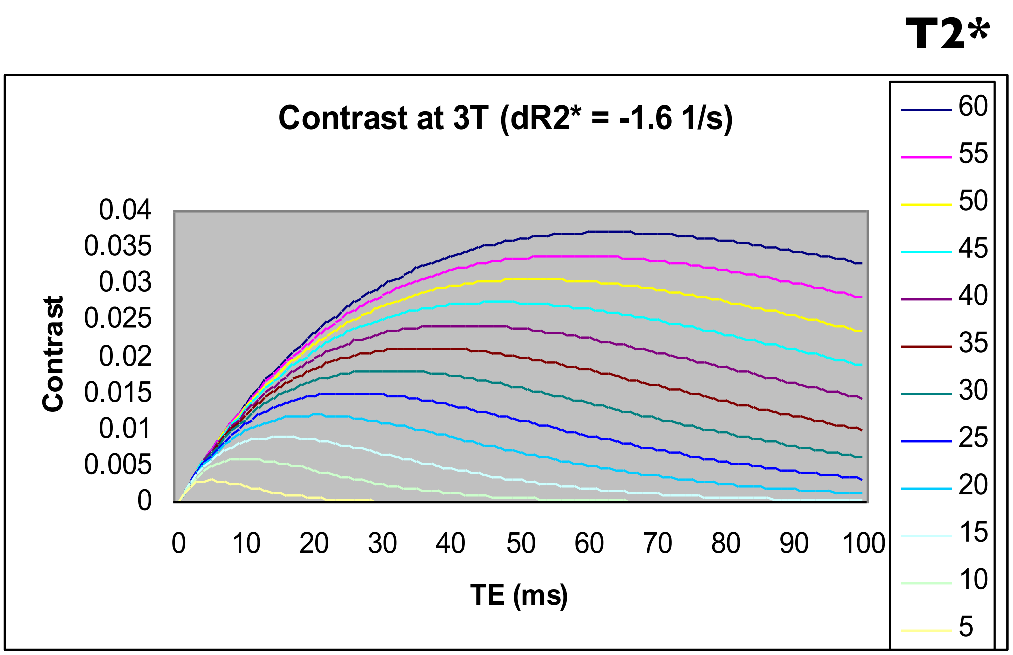
Local Signal Increase in T2 and T2* - weighted sequences

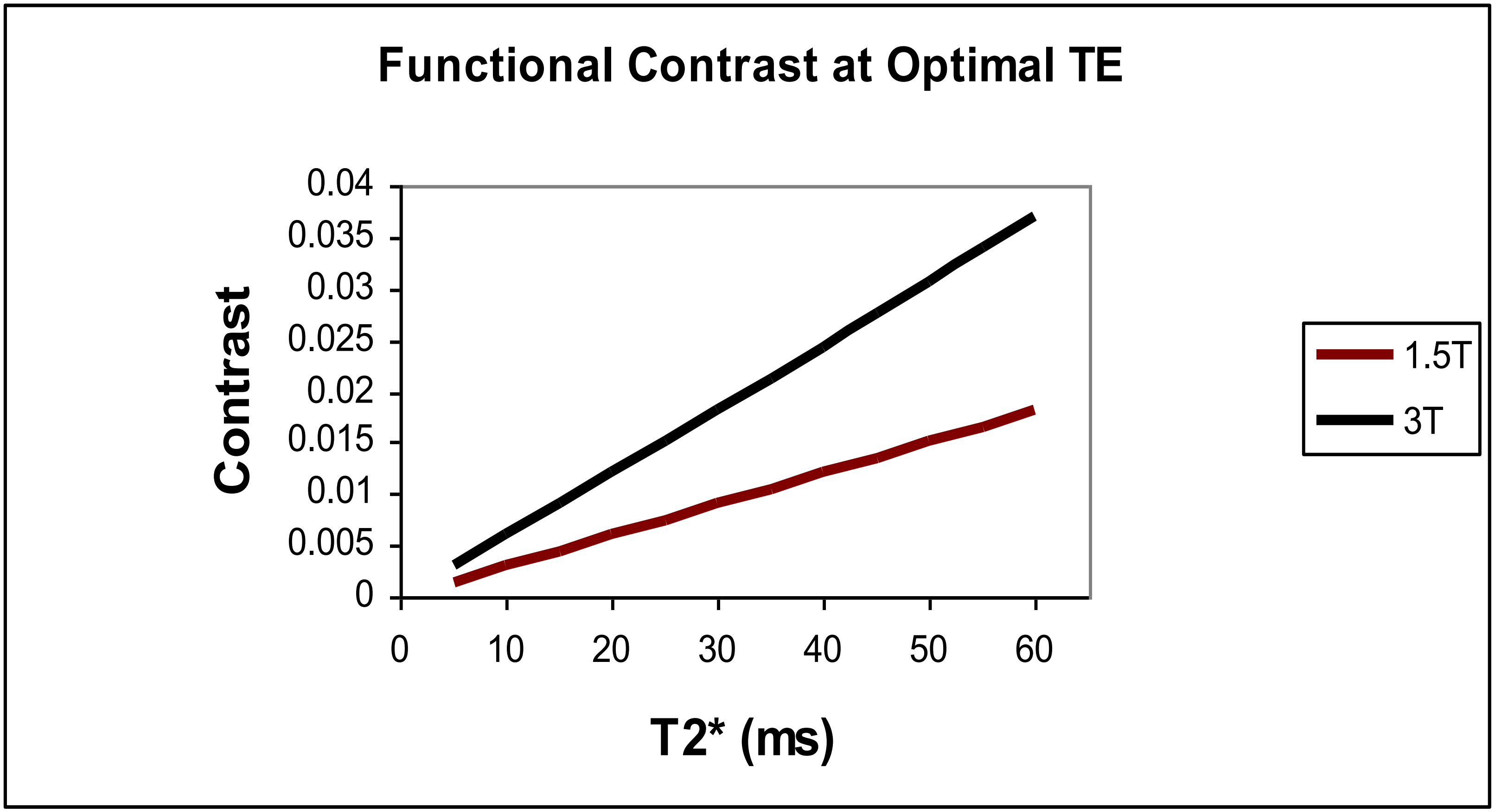
Characteristics of the BOLD signal: T2* effect.



Contrast depends on:
activation-induced changes in T2* *and* resting T2*



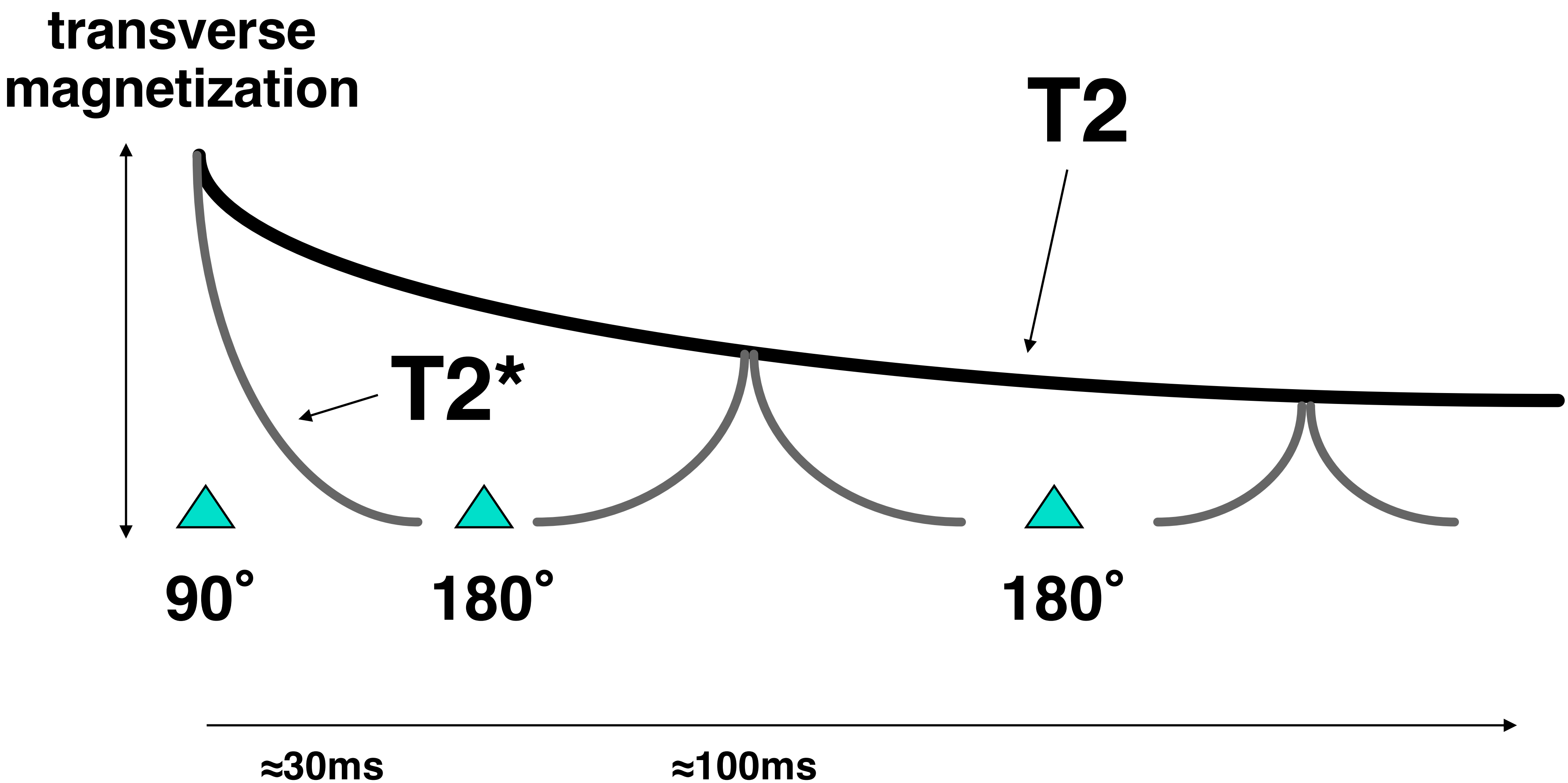


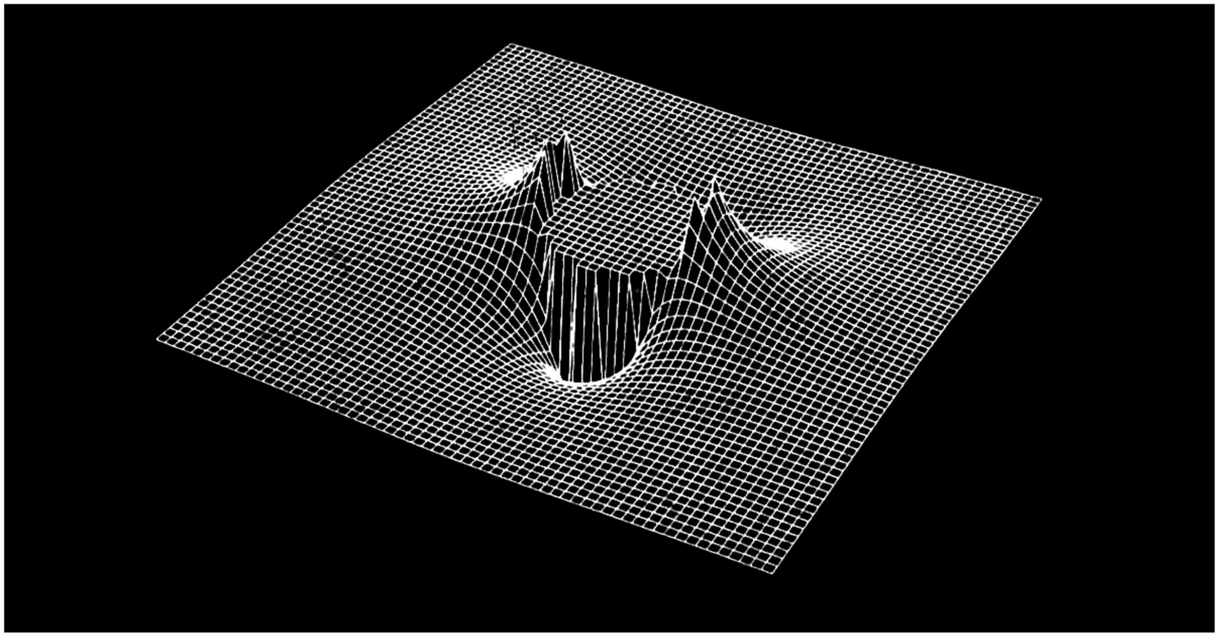

Functional Contrast at Optimal TE
Contrast
0.04
0.035
0.03
0.025
0.02
0.015
0.01
0.005
0
0
10
20
30
40
50
60
T2* (ms)
1.5T
3T

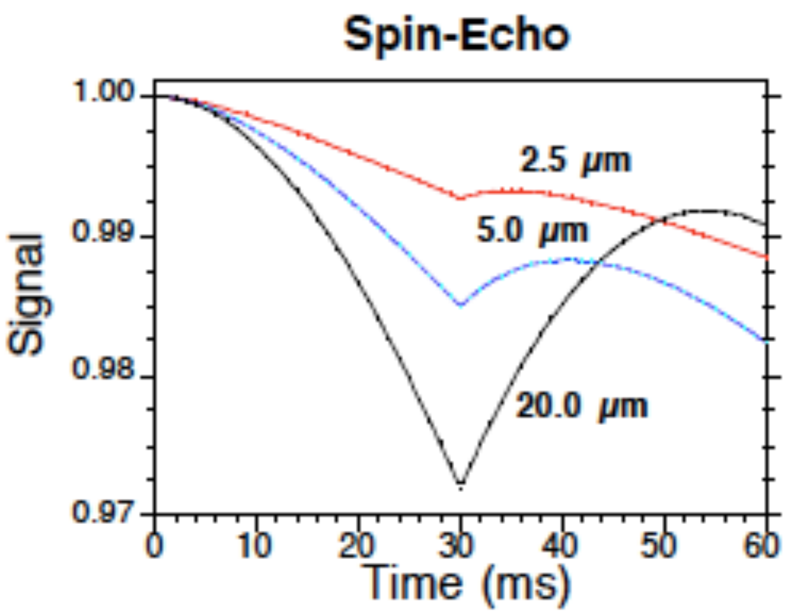
Spin-Echo vs. Gradient-Echo

fMRI

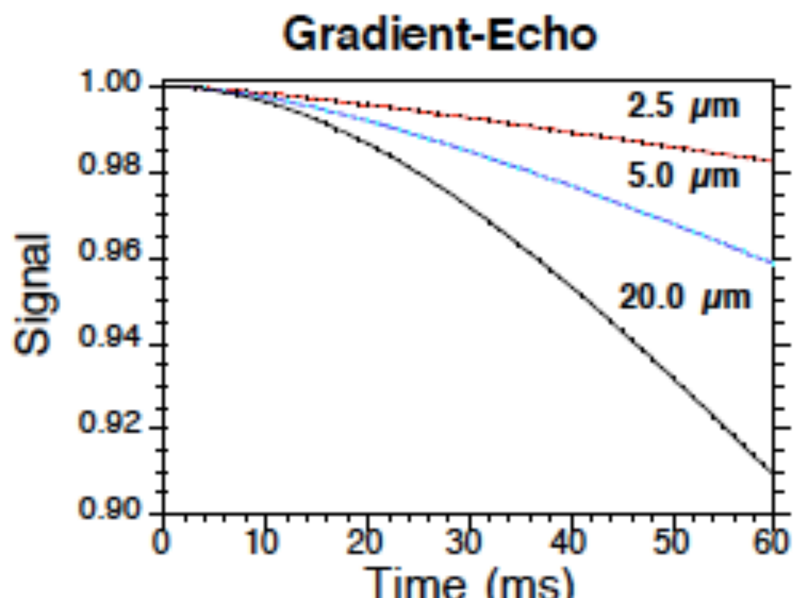
Transverse Relaxation





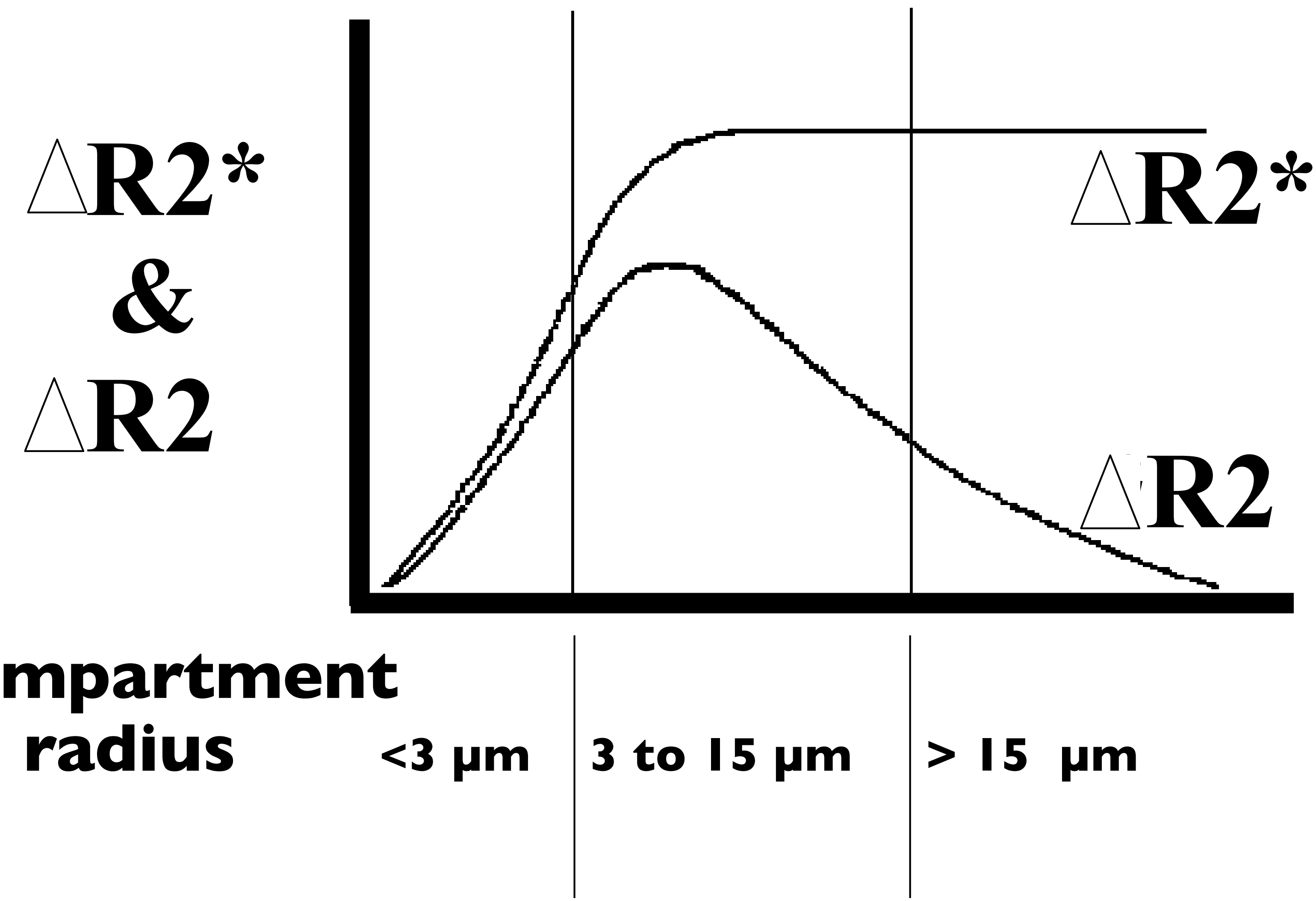


Spin-Echo
1.00
0.99
0.98
0.97
Signal
0
10
20
30
40
50
60
Time (ms)
2.5 μm
5.0 μm
20.0 μm

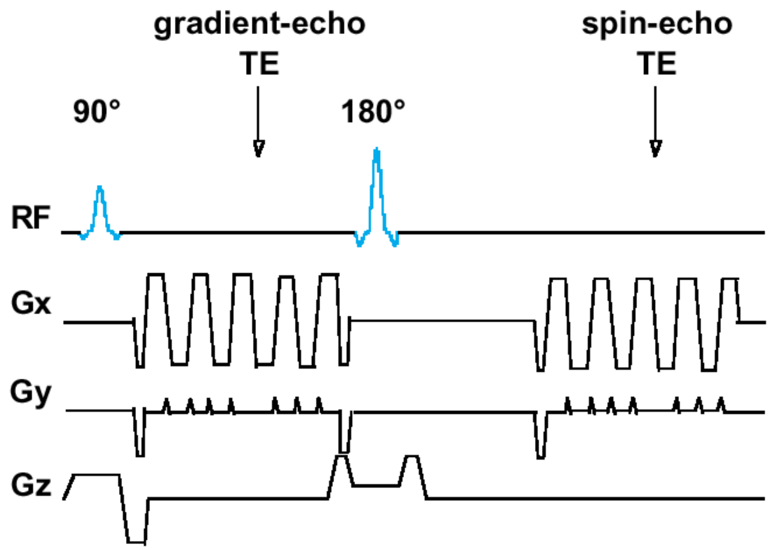


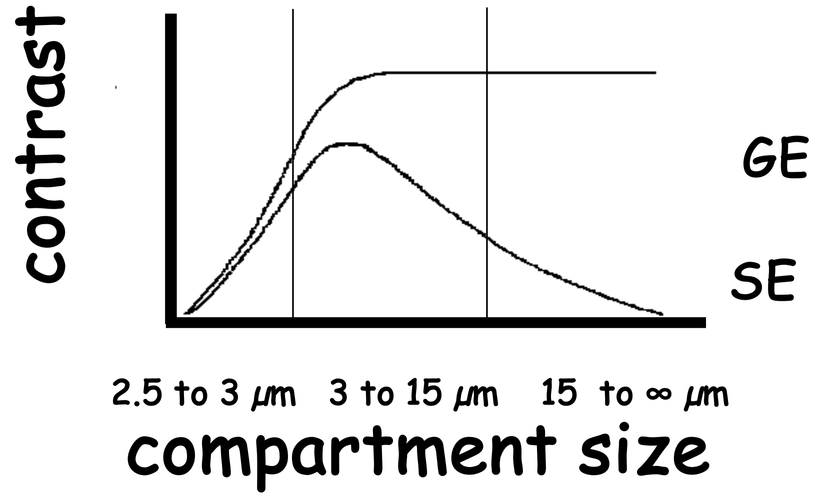
Gradient-Echo
1.00
0.98
0.96
0.94
0.92
0.90
Signal
0
10
20
30
40
50
60
Time (ms)
2.5 μm
5.0 μm
20.0 μm

Spin echo vs. Gradient echo



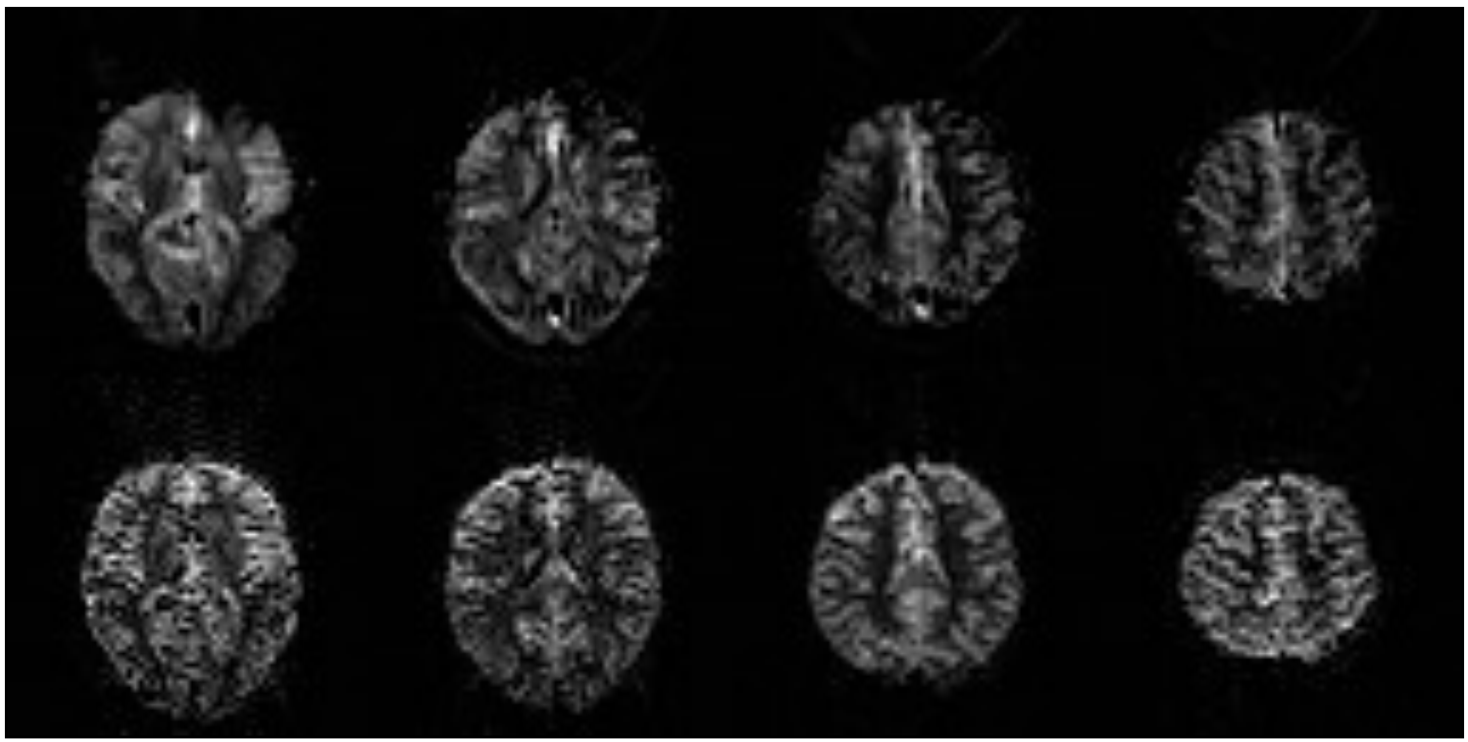
Bolus Injection of Gadolinium

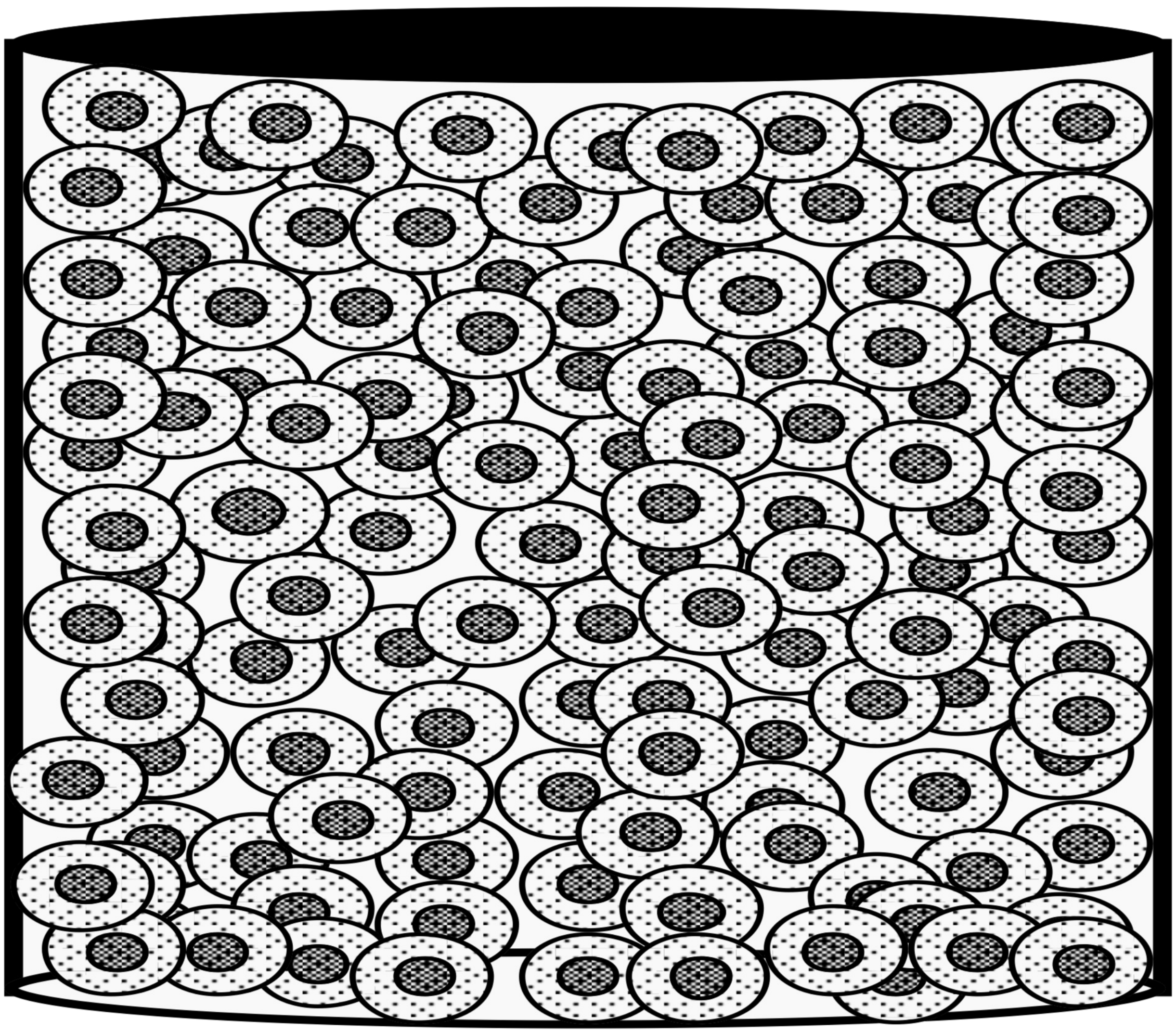




GE
TE = 30 ms

SE
TE = 110 ms





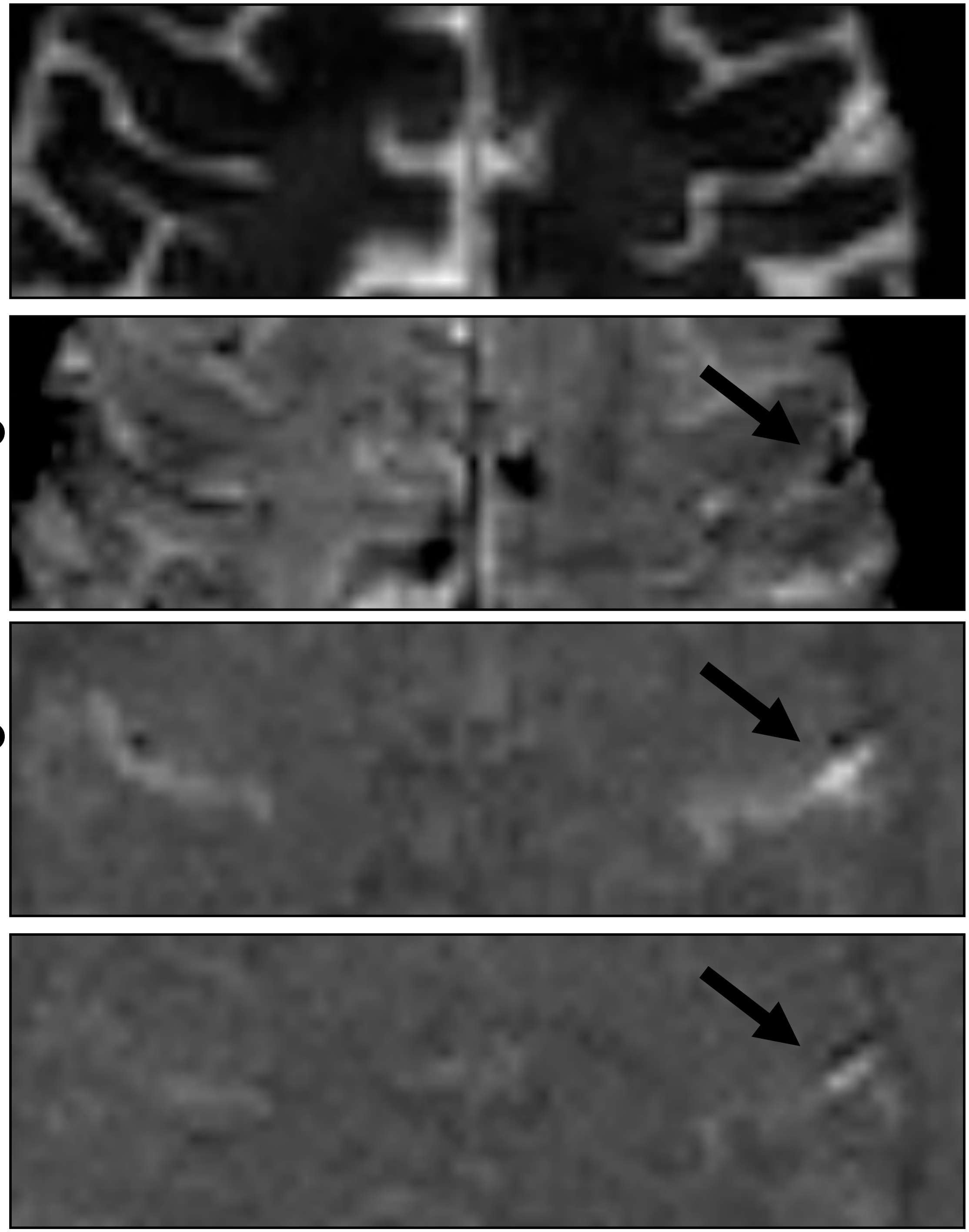
3T

Spin-Echo
TE = 105 ms
TR = ∞

Gradient-Echo
TE = 50 ms

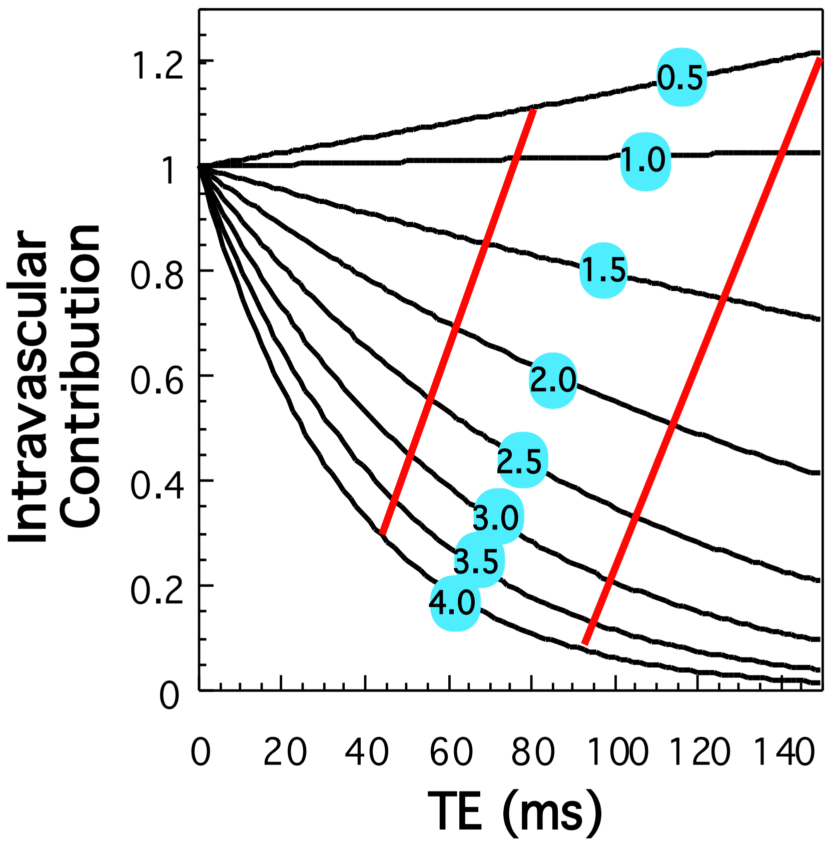
Gradient-Echo
functional
TE = 50 ms

Spin-Echo
functional
TE = 105 ms

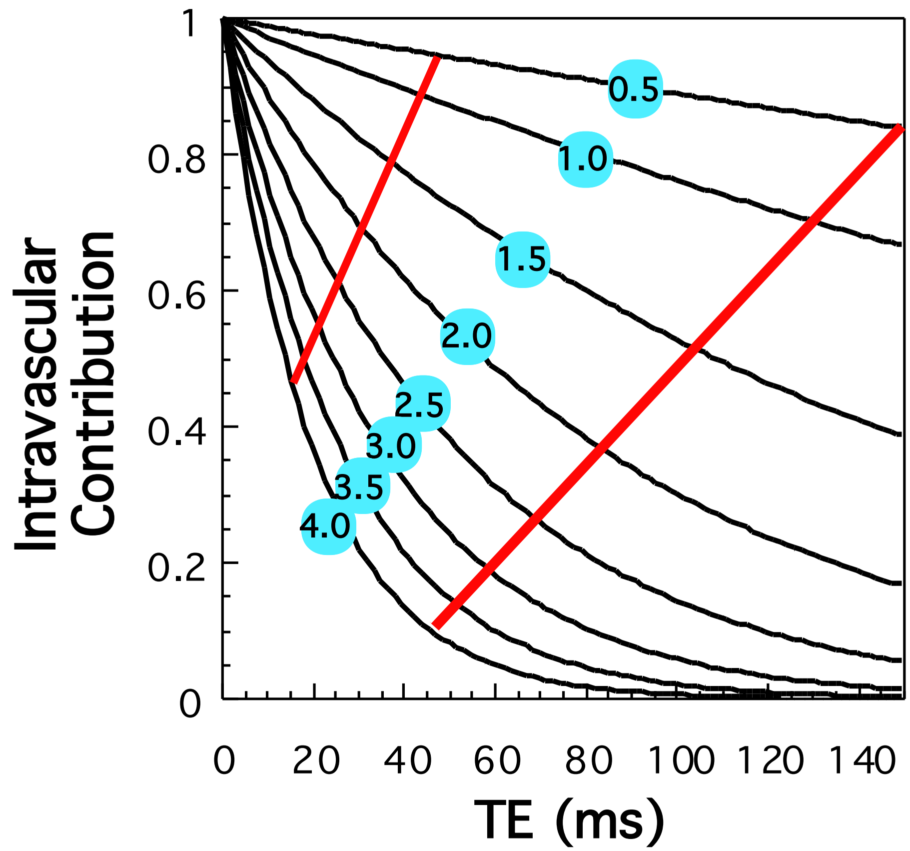


Field strength dependence of intravascular signal

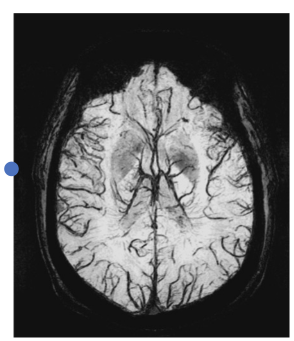
Spin-echo, %HbO_2 = 60



Gradient-echo, %HbO_2 = 60



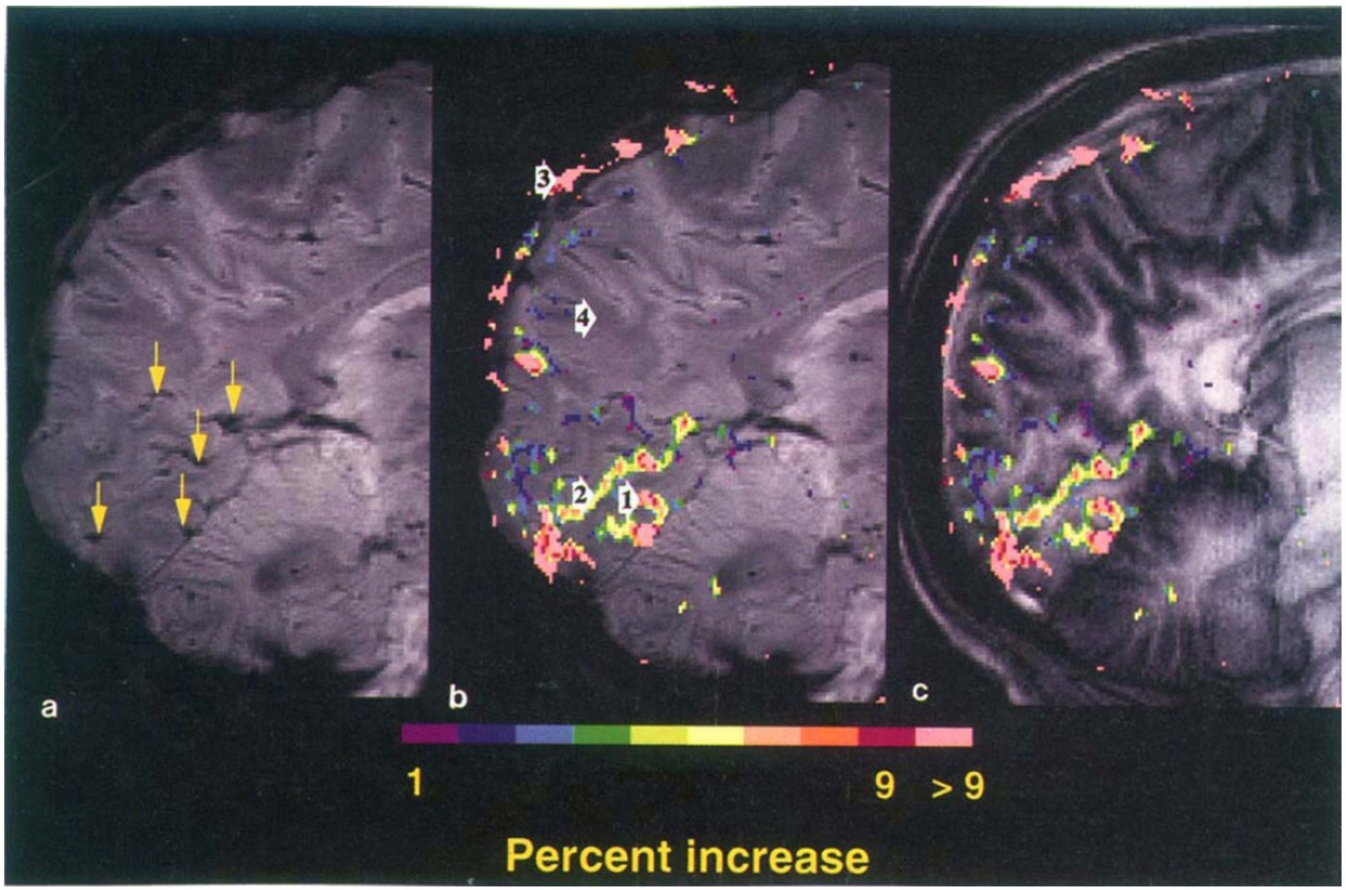
Source of most contrast in venograms..

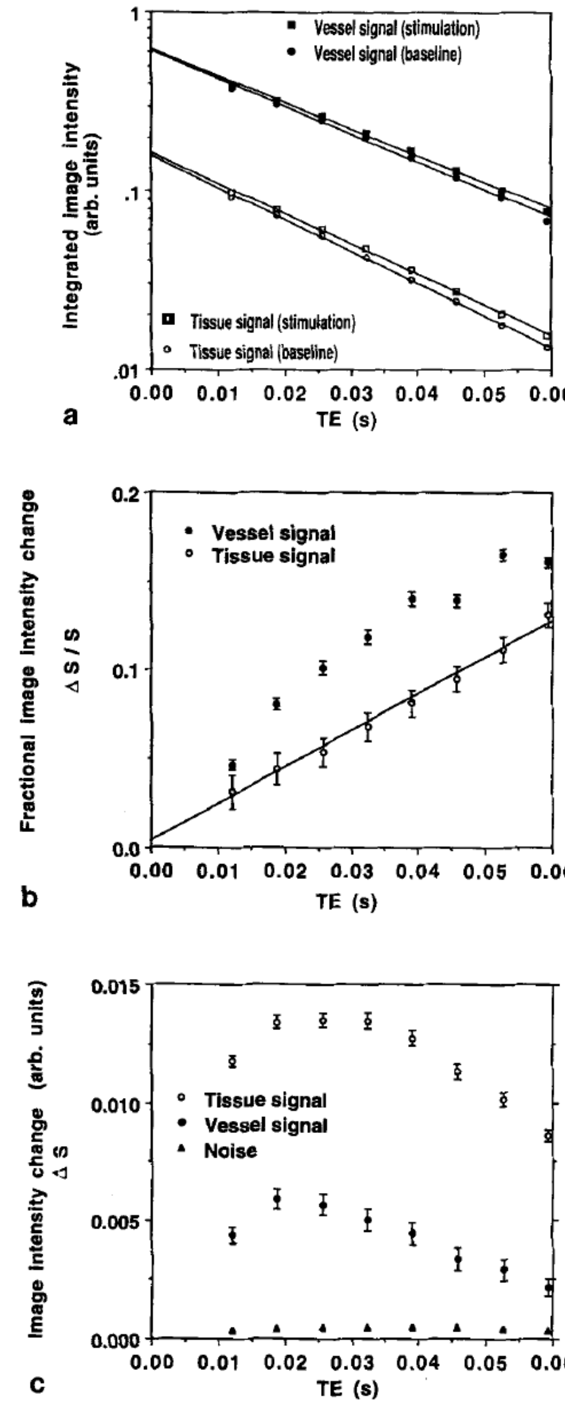


MRM 30:380-386 (1993)

4 Tesla Gradient Recalled Echo Characteristics of Photic Stimulation-Induced Signal Changes in the Human Primary Visual Cortex

Ravi S. Menon, Seiji Ogawa, David W. Tank, Kâmil Uğurbil





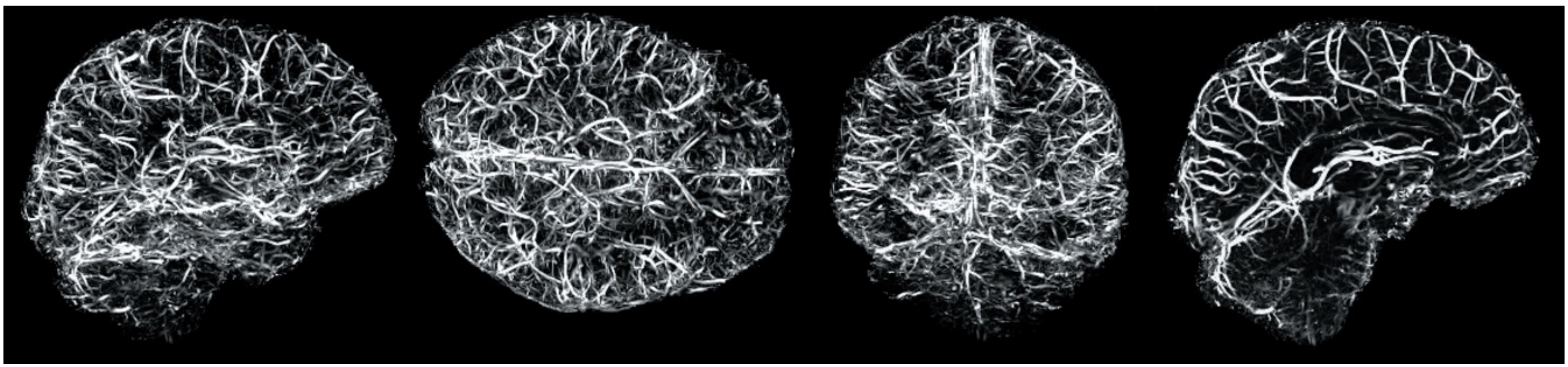
Magnetic Resonance in Medicine 52:612–618 (2004)

Susceptibility Weighted Imaging (SWI)

E. Mark Haacke,[1-4*] Yingbiao Xu,[1,2] Yu-Chung N. Cheng,[1] and Jürgen R. Reichenbach[5]

a

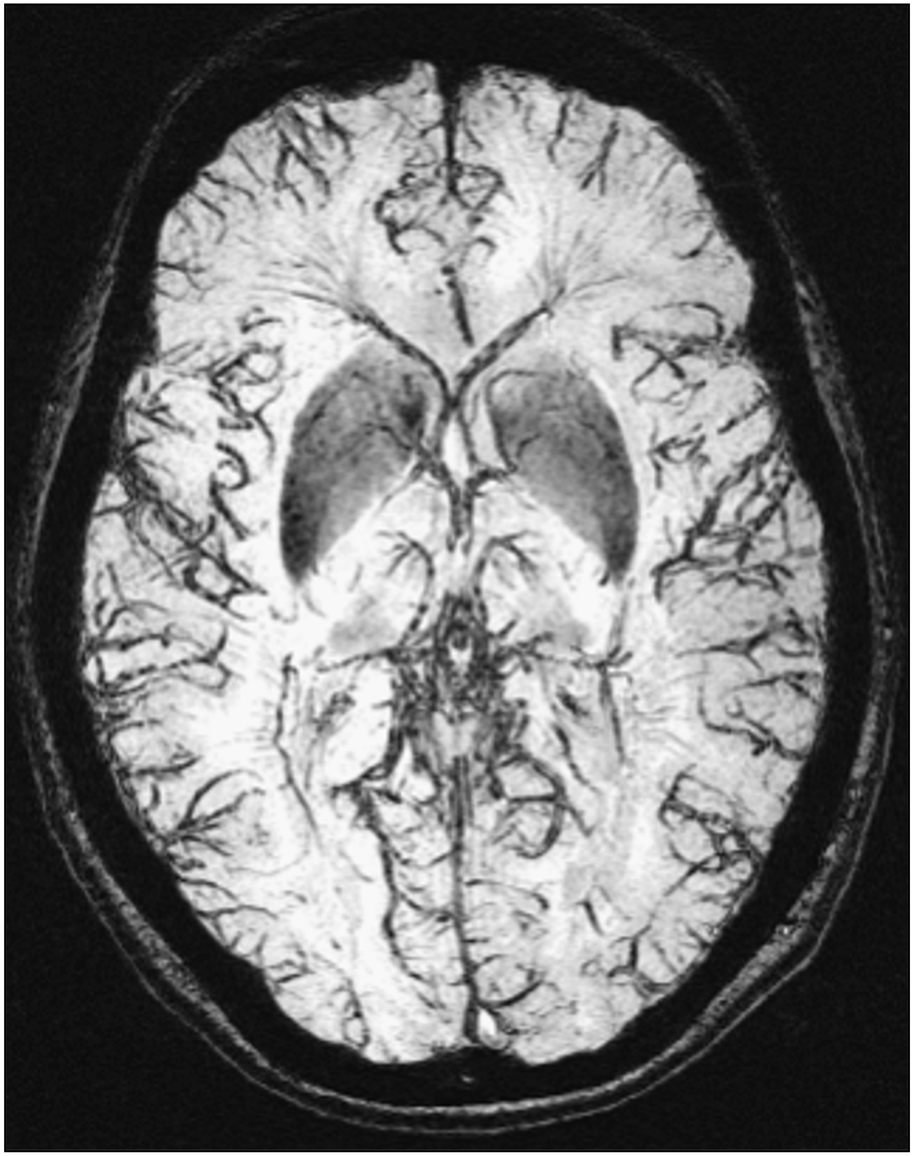
SWI: Susceptibility Weighted Imaging



David Norris,
Marcus Barth

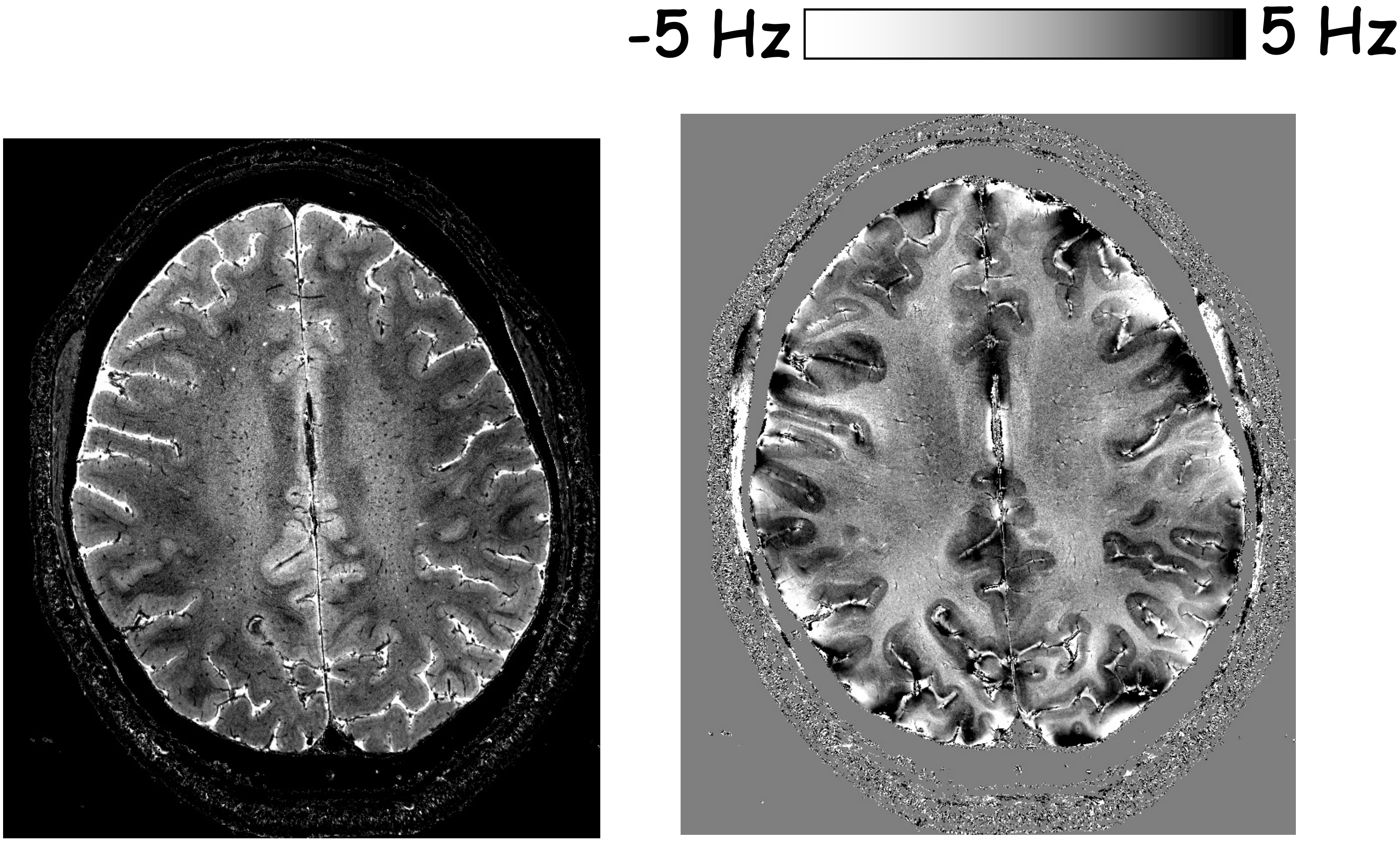
7T
Hahn Institute

BOLD effect to highlight veins: 3 Tesla



Bove-Bettis, et al (2004), SMRT

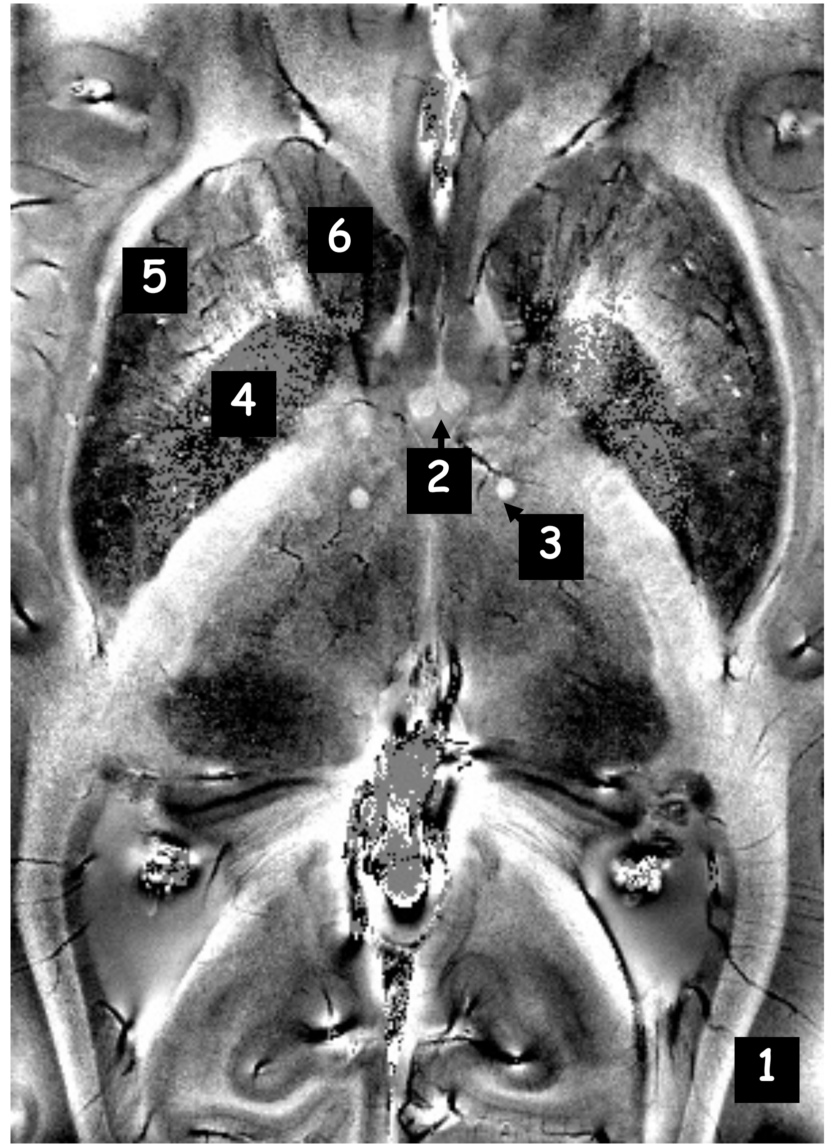
Phase versus Magnitude Contrast



Courtesy :P. Van Geldern and J. Duyn

GRE, magnitude

GRE, phase

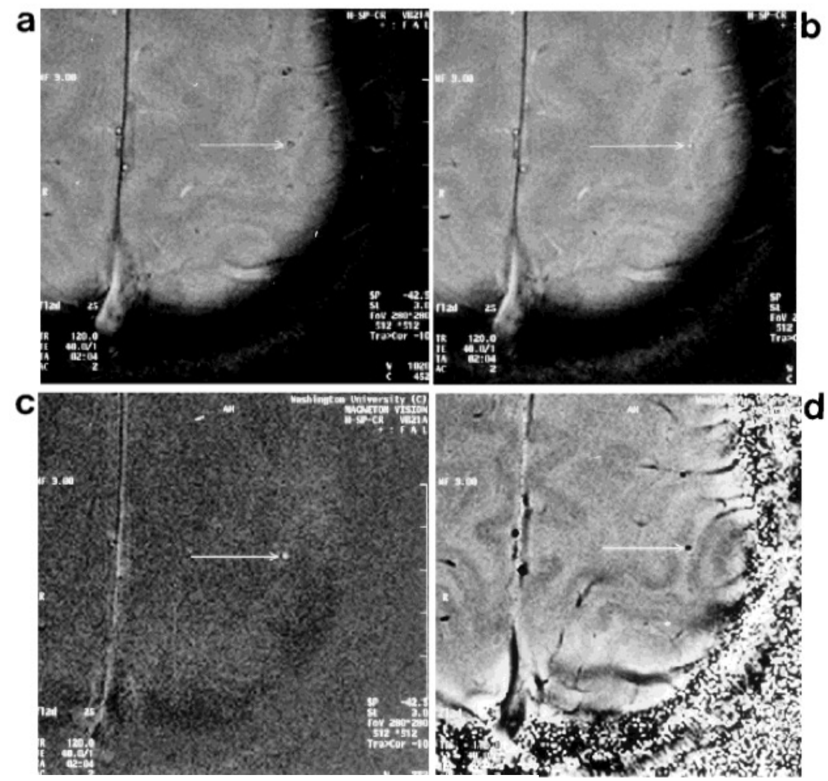


1. veins crossing the optic radiations; 2. anterior column, fornix; 3. cross-section of the mamillothalamic tract; 4. globuspallidus; 5. putamen; 6. head of the caudate nucleus.

Courtesy :P. Van Gelderen and J. Duyn

What information can we extract using MRI / fMRI?

Baseline and Activation-induced Changes in Oxygenation



-assumptions on Hct, geometry
-limited to picking out vessels

E. M. Haacke, et al, HBM 5: 341-346, 1997

TABLE I. Results of phase, susceptibility, oxygenation, and velocity changes in pial veins in 5 volunteers upon motor cortex activation*

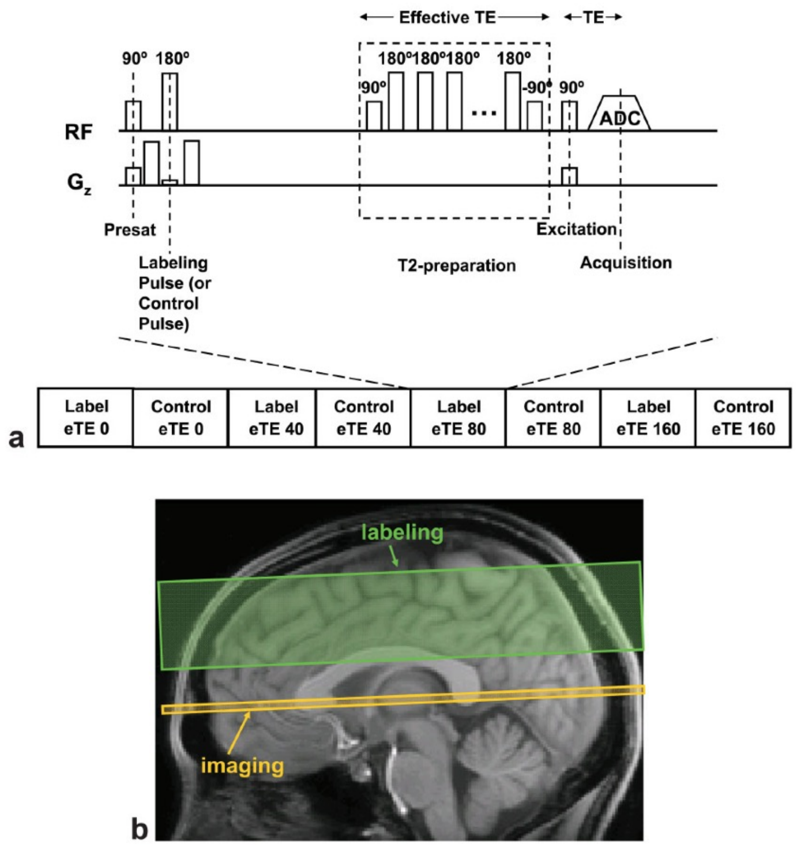
Volunteer number	TE (msec)	$\Delta\phi_{rest-act}$ (deg)	$\Delta\chi_{rest-act}$ (ppm)	ΔY_{susc}	v_{rest} (cm/sec)	v_{act} (cm/sec)	ΔY_{flow}
1	60	20	0.008	0.11	3.1	4.1	0.13
2	40	36	0.012	0.165	3.0	3.7	0.08
3	60	19	0.009	0.13	4.8	7.4	0.16
4	40	42	0.011	0.15	1.2	2.0	0.19
5	40	45	0.012	0.16	1.5	2.3	0.15
Mean ± SD		32.4 ± 12.2	0.01 ± 0.001	0.14 ± 0.02	2.72 ± 1.44	3.90 ± 1.91	0.14 ± 0.04

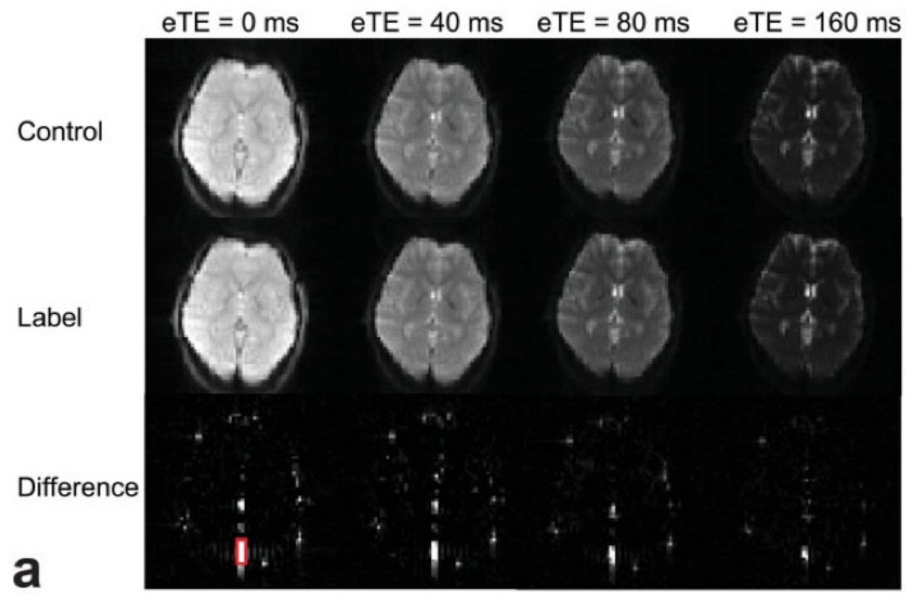
*Where TE is echo time, $\Delta\phi_{rest-act}$ the phase difference fo flow-compensated acquisition. $\Delta\chi_{rest-act}$ and ΔY_{uss} the susceptibility change and corresponding oxygen saturation change extracted from $\Delta\phi_{rest-act}$, while ΔY_{flow} is the oxygen saturation change extracted from the change of flow velocity, i.e., from v_{rest} in the resting state to v_{act} in the activation state.

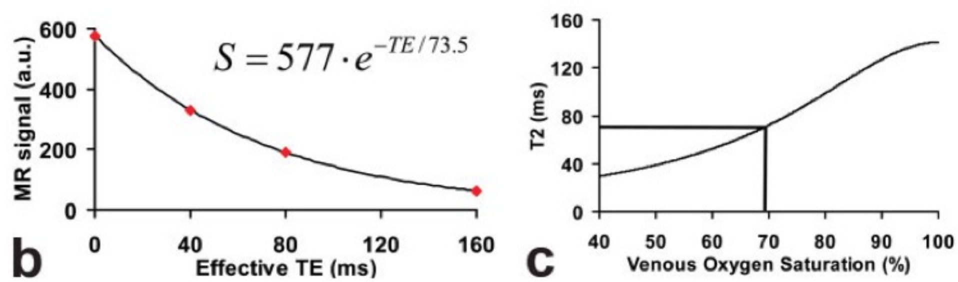
What information can we extract using MRI / fMRI?

Baseline oxygenation with fewer assumptions

-measurement of T2 of ASL- tagged blood
-assumptions of Hct, accuracy of calibration plot







T2-Relaxation-Under-Spin-Tagging
"TRUST" MRI

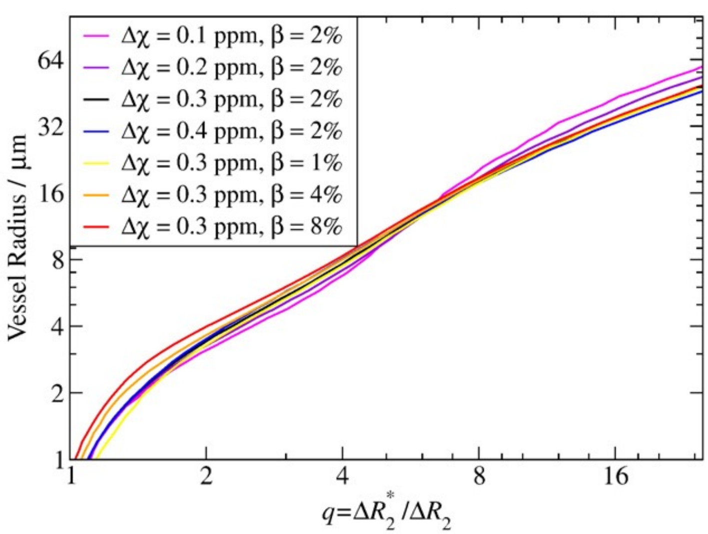
H. Lu, MRM, 60:357-363, 2008

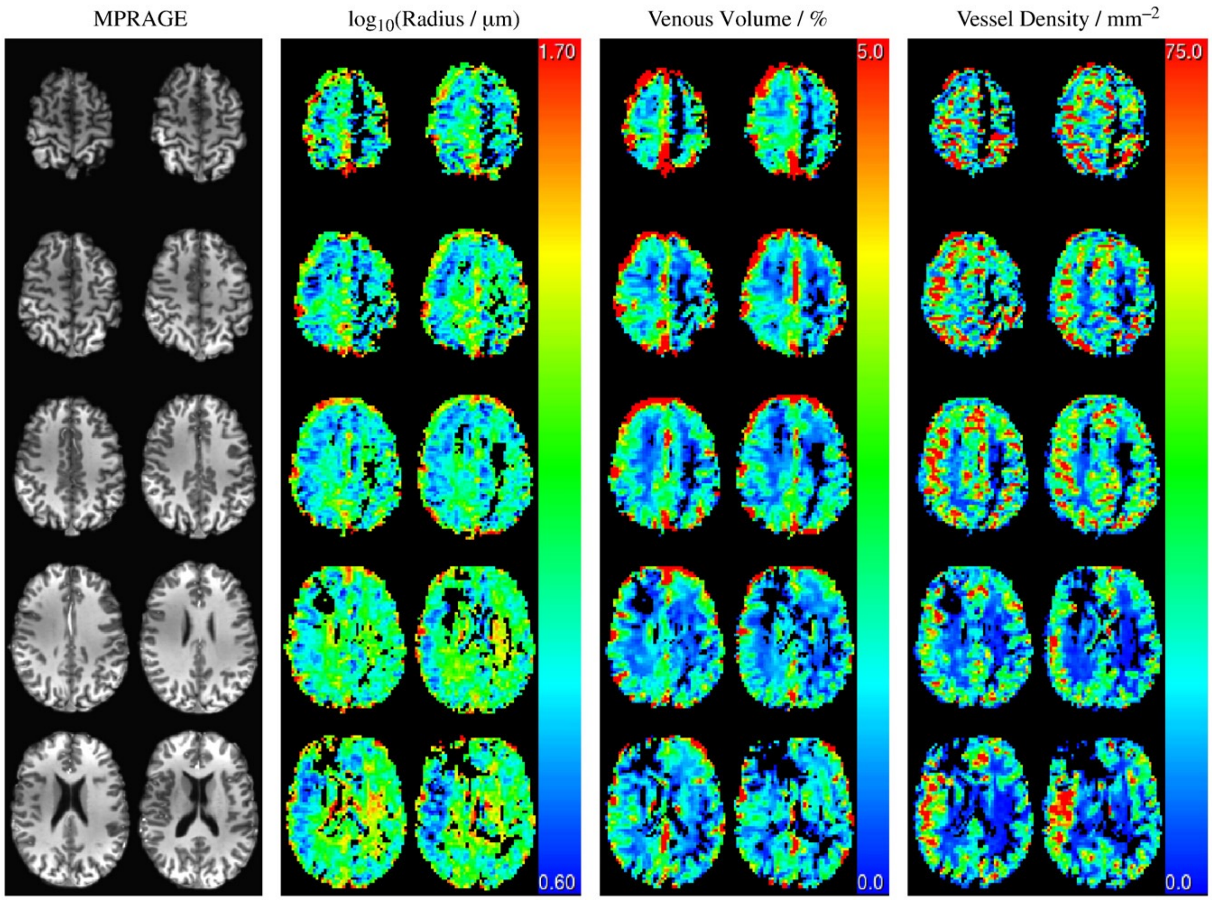
What information can we extract using MRI / fMRI?

*Ve*ssel Parameter Mapping

-SE/GE ratio -> vessel radius

-GE signal change with global stress
-> blood volume





T. H. Jochimsen, et al. NeuroImage, 51: 765-774 (2010)

Pros and Cons of Spin-Echo

- Increased specificity (esp at high fields where IV signal is low)
- Less sensitive to rapidly flowing blood
- Less signal dropout.

- Less slices per TR
- Lower fCNR by x 2 to 4.
- Acquisition window still T2*
- Very large IV signal still present at most field strengths.

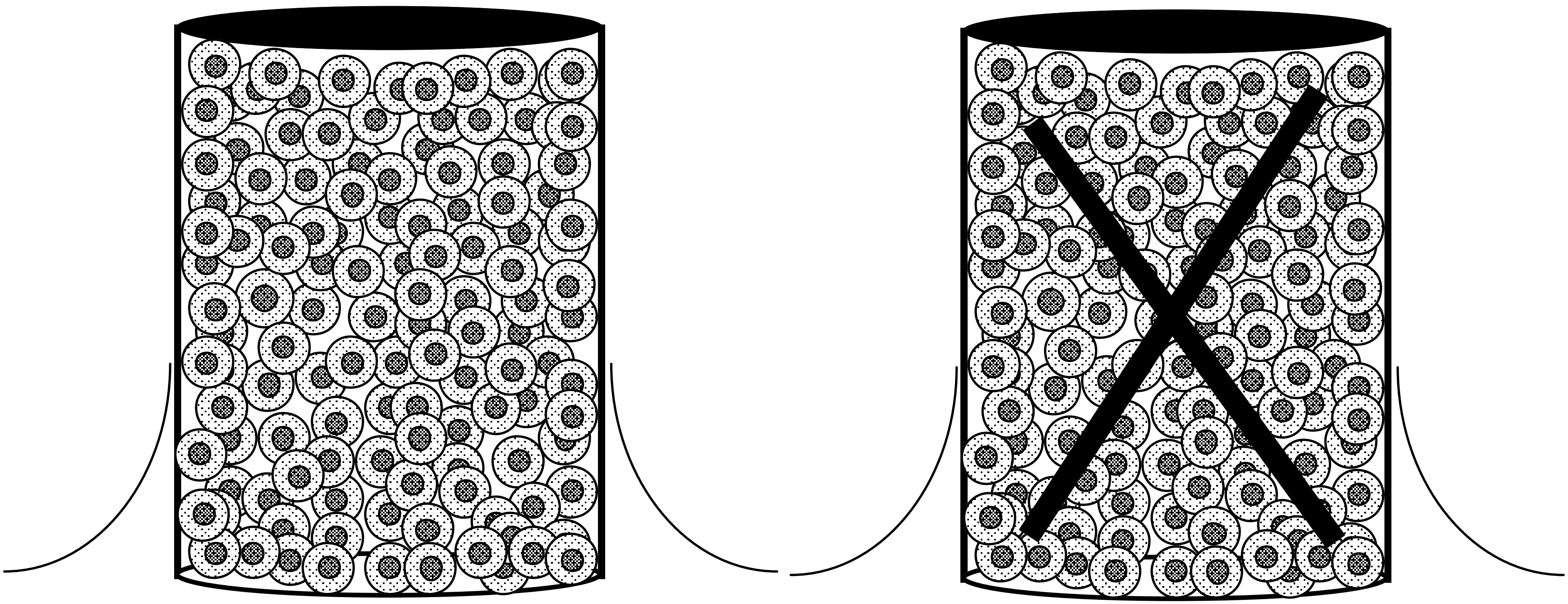
I would only use at 7T if also imaging at high ressolution and interested in something like columns or layers.

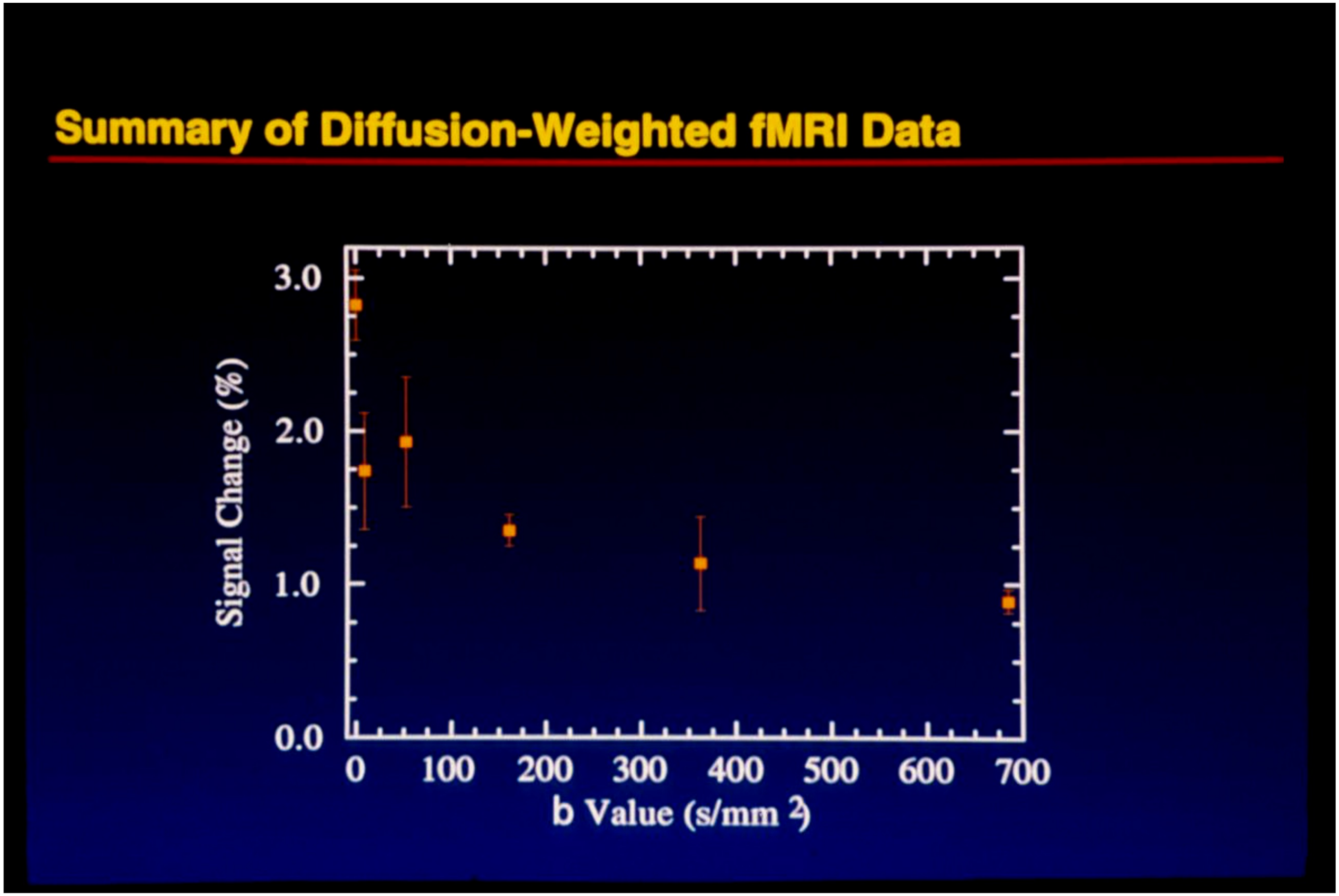
…so let’s remove the intravascular signal...

Velocity Nulled (or diffusion weighted) fMRI.

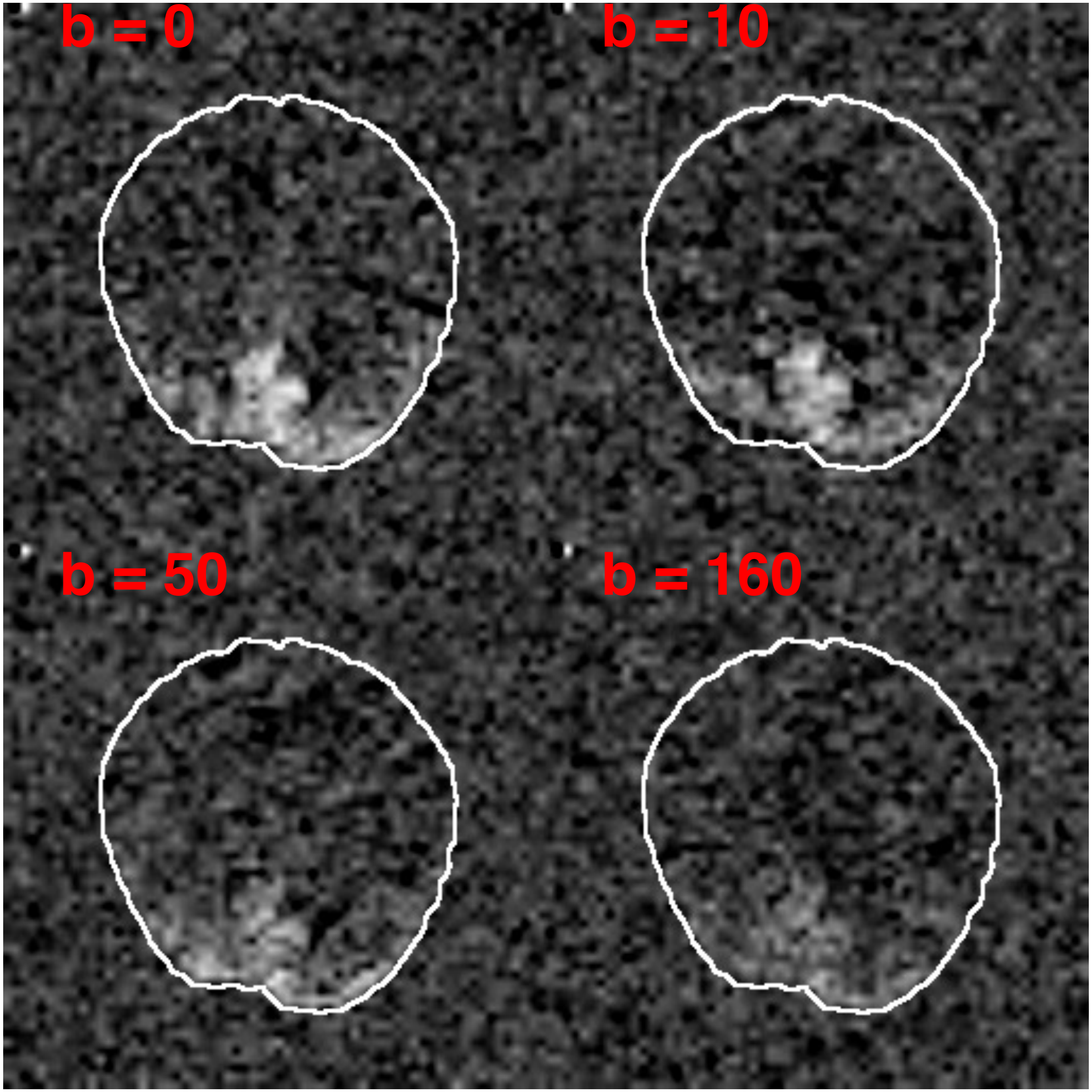
no diffusion weighting

diffusion weighting

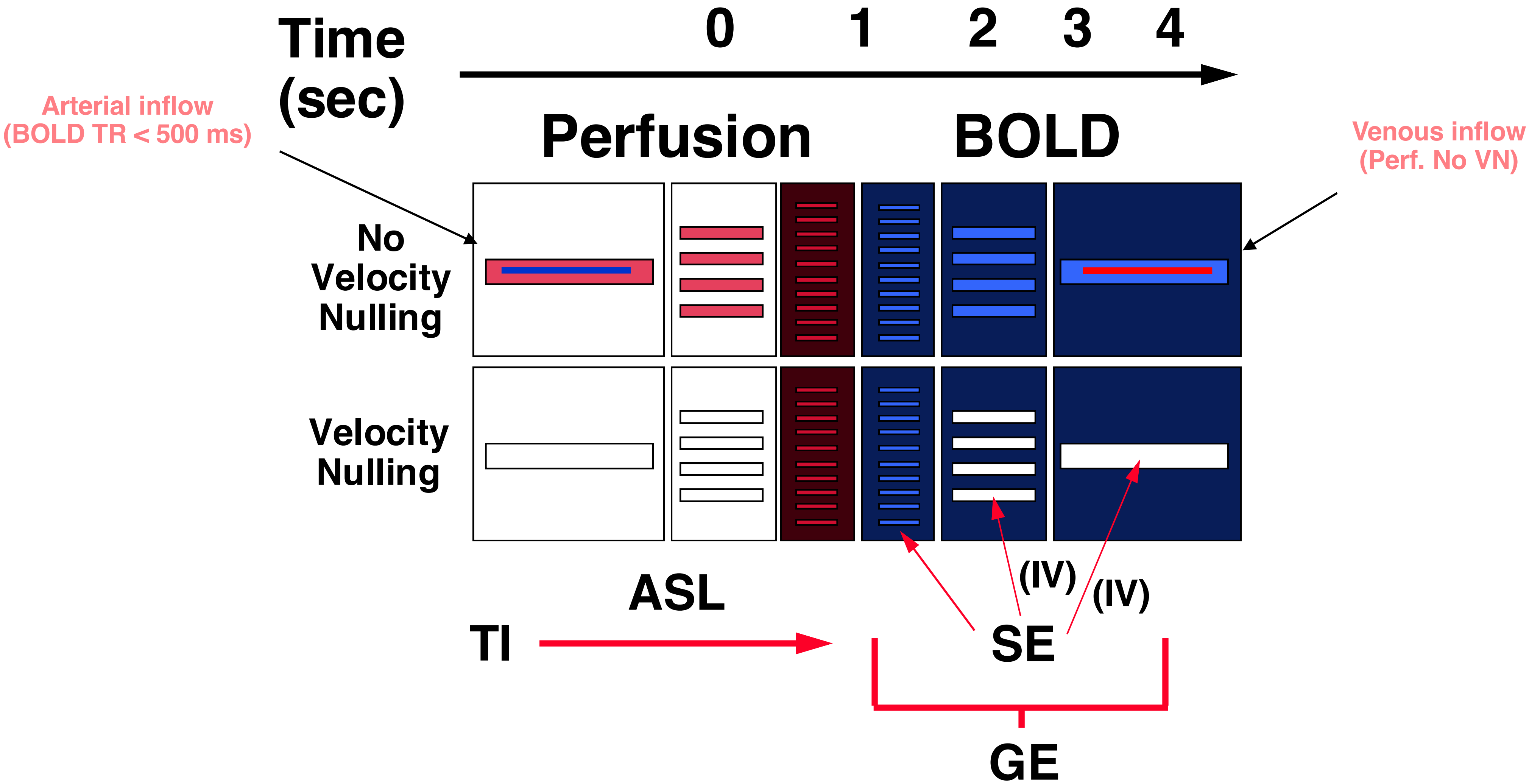




J. L. Boxerman, P. A. Bandettini, K. K. Kwong, J. R. Baker, T. L. Davis, B. R. Rosen, R. M. Weisskoff, The intravascular contribution to fMRI signal change: monte carlo modeling and diffusion - weighted studies in vivo. *Magn. Reson. Med.* 34, 4-10 (1995).


b = 0
b = 10
b = 50
b = 160

Hemodynamic Specificity



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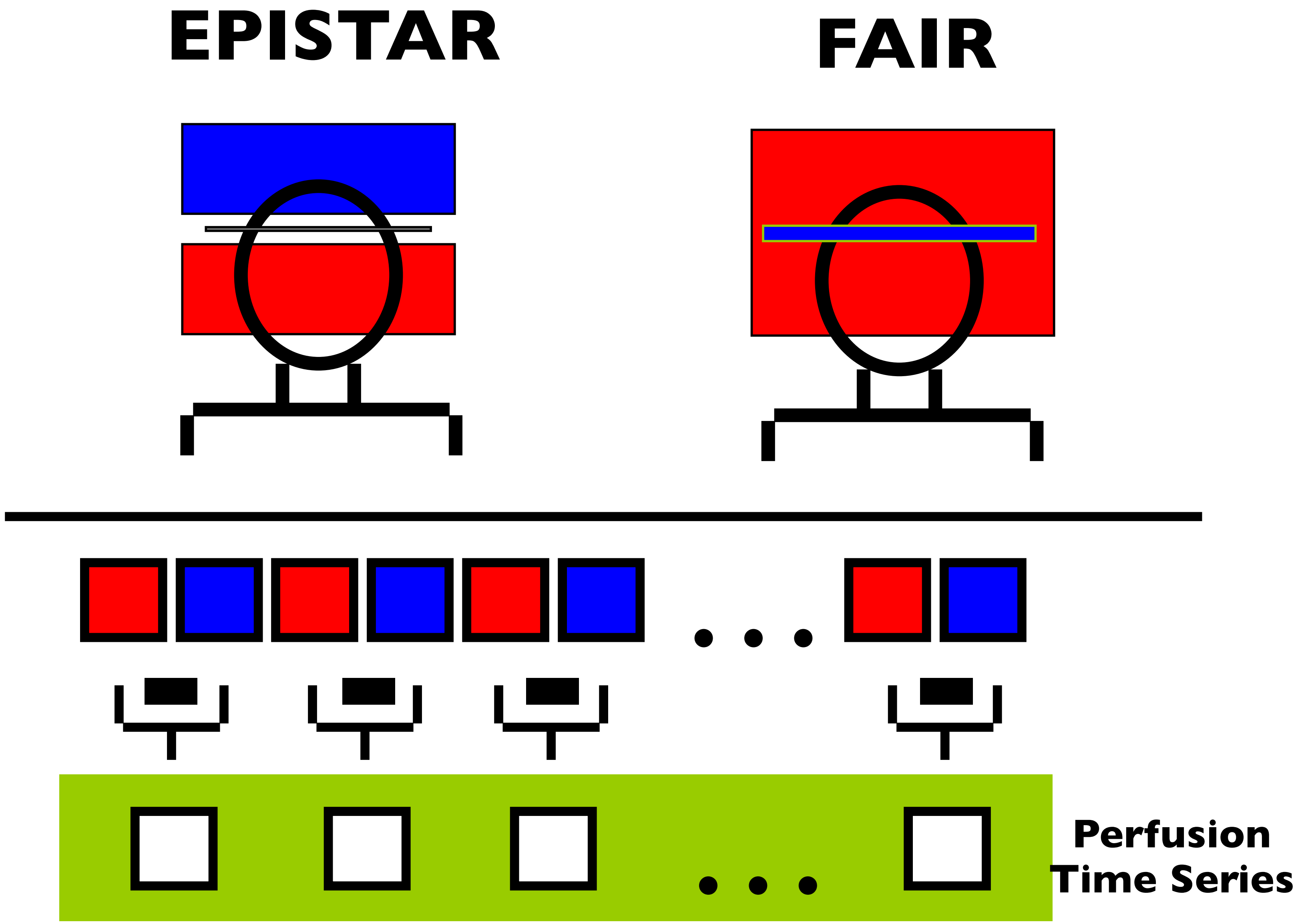
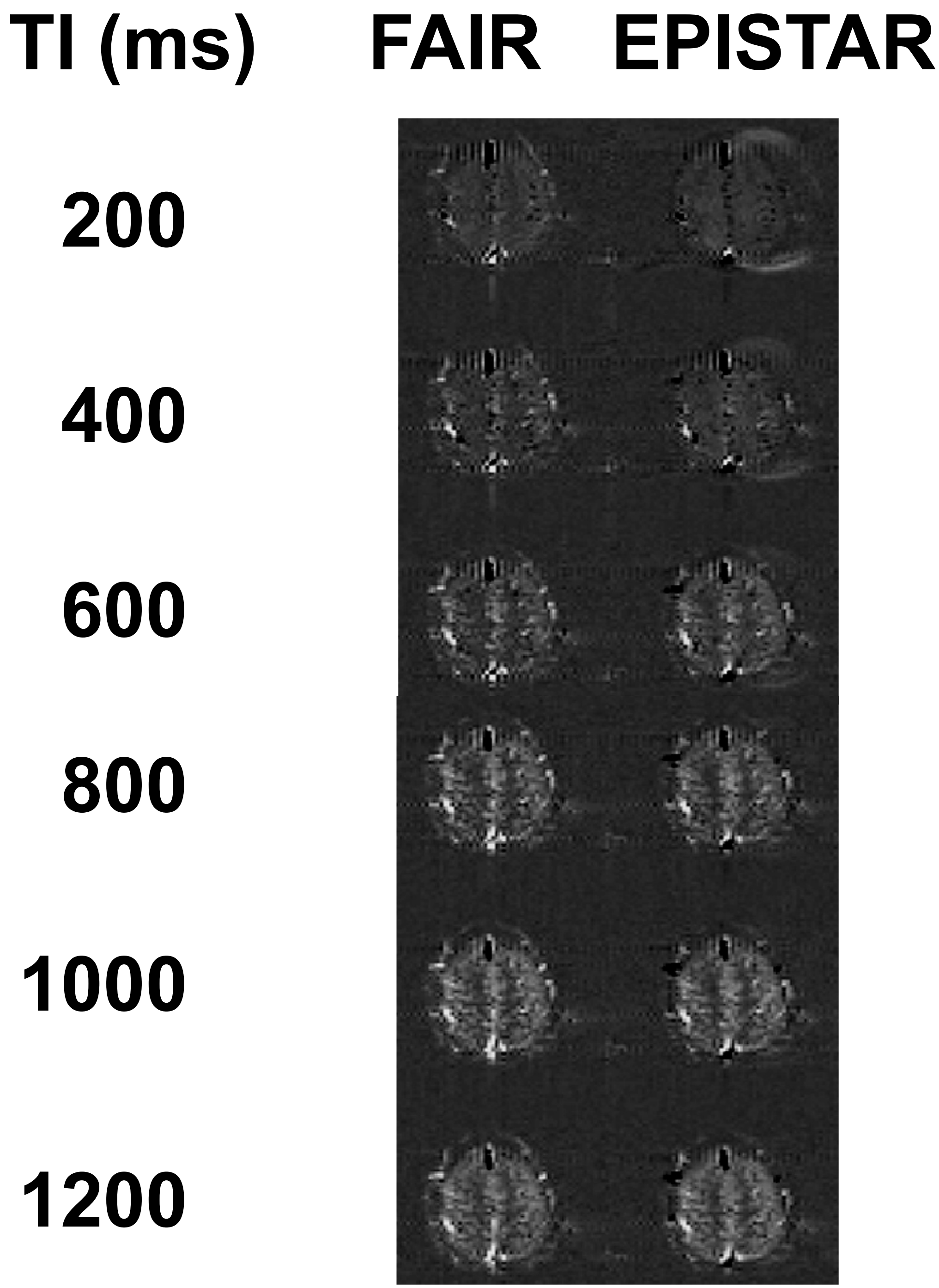
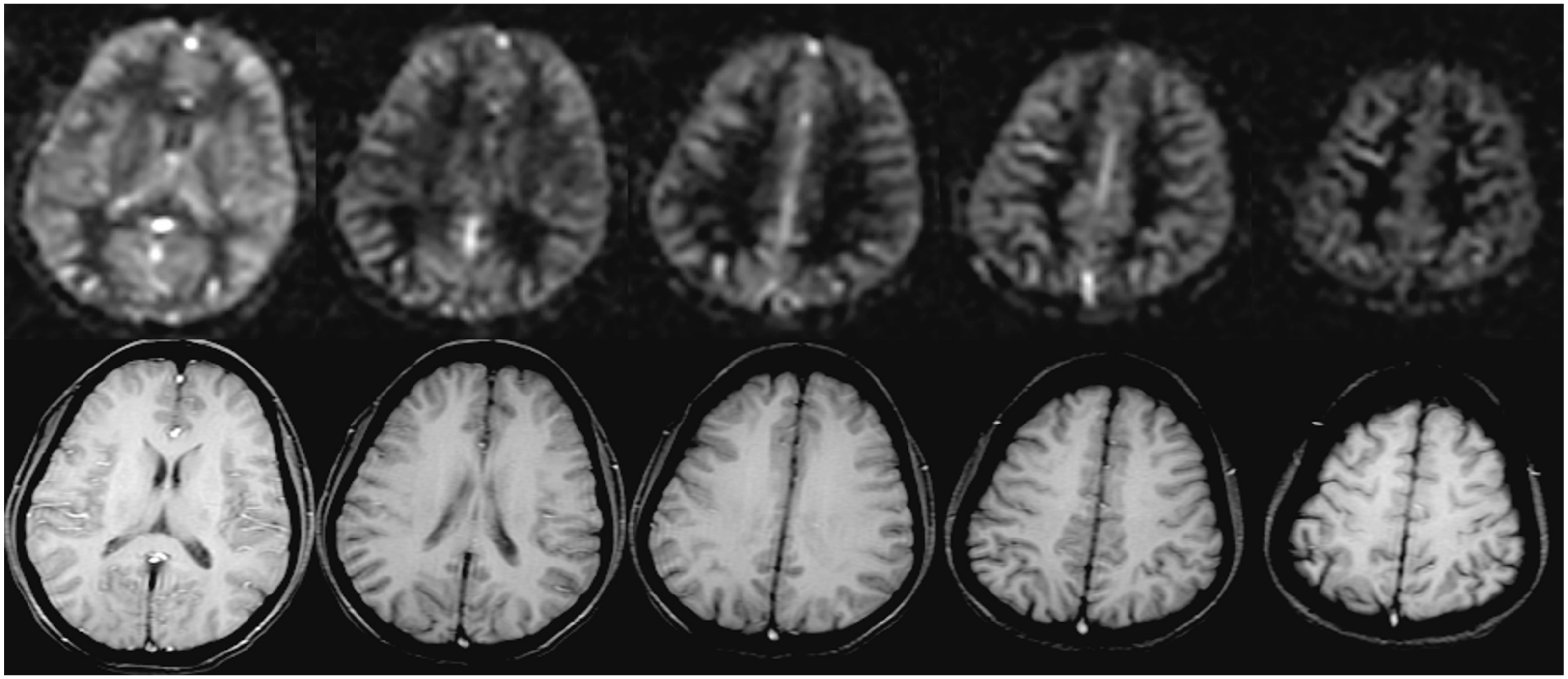
Perfusion Contrast




TI (ms)
FAIR
EPISTAR
200
400
600
800
1000
1200

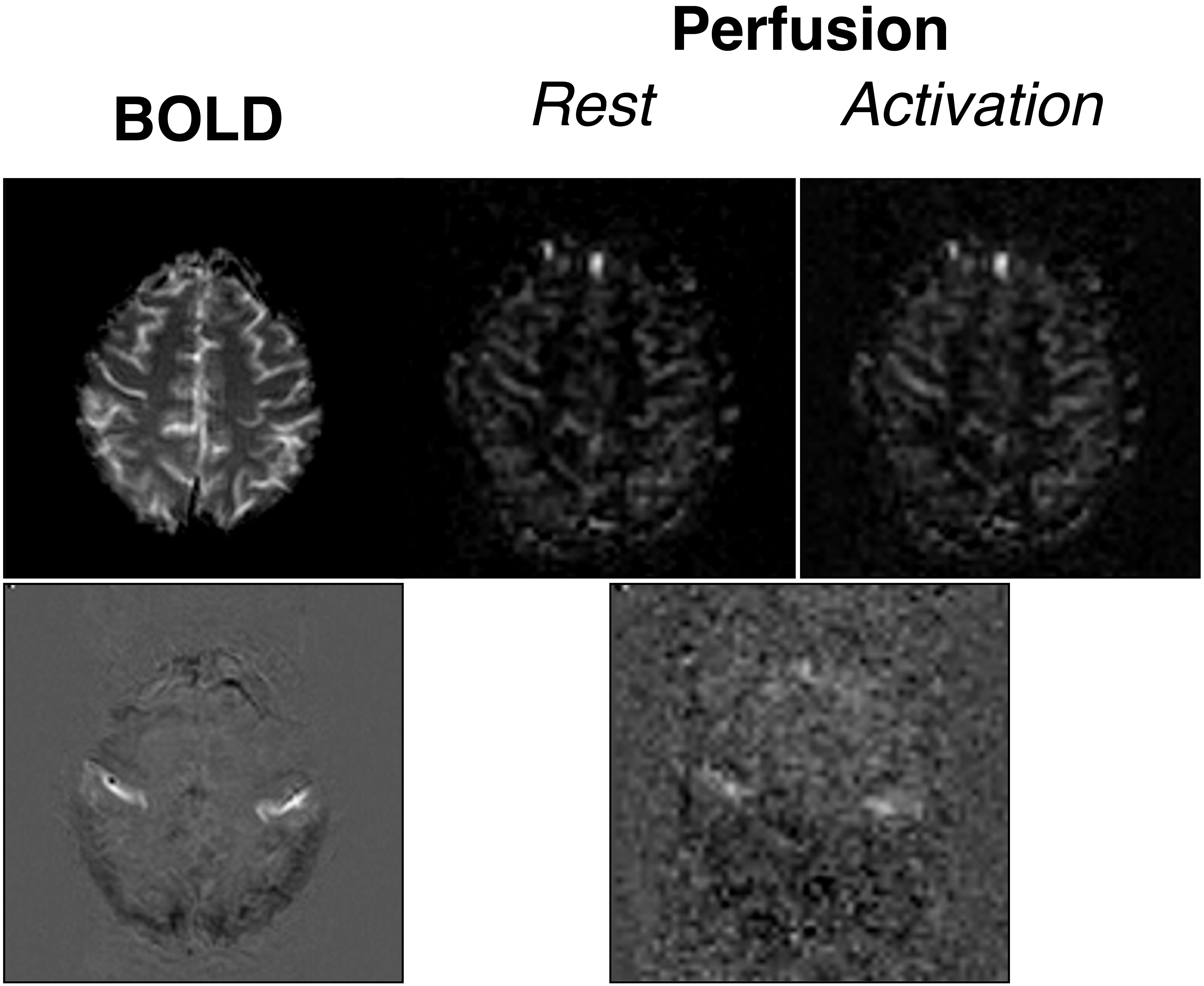


Williams, D. S., Detre, J. A., Leigh, J. S. & Koretsky, A. S. (1992) "Magnetic resonance imaging of perfusion using spin-inversion of arterial water." **Proc. Natl. Acad. Sci. USA 89, 212-216.**

Edelman, R., Siewert, B. & Darby, D. (1994) "Qualitative mapping of cerebral blood flow and functional localization with echo planar MR imaging ans signal targeting with alternating radiofrequency (EPISTAR)." **Radiology 192, 1-8.**

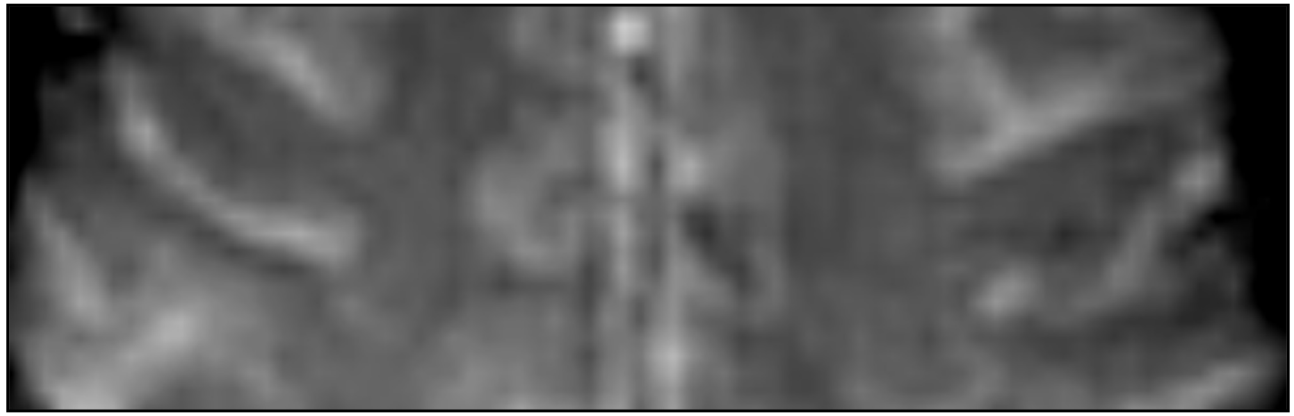
Kim, S.-G. (1995) "Quantification of relative cerebral blood flow change by flow-sensitive alternating inversion recovery (FAIR) technique: application to functional mapping." **Magn. Reson. Med. 34, 293-301**.

Kwong, K. K. et al. (1995) "MR perfusion studies with T1-weighted echo planar imaging."**Magn. Reson. Med. 34,878-887.**

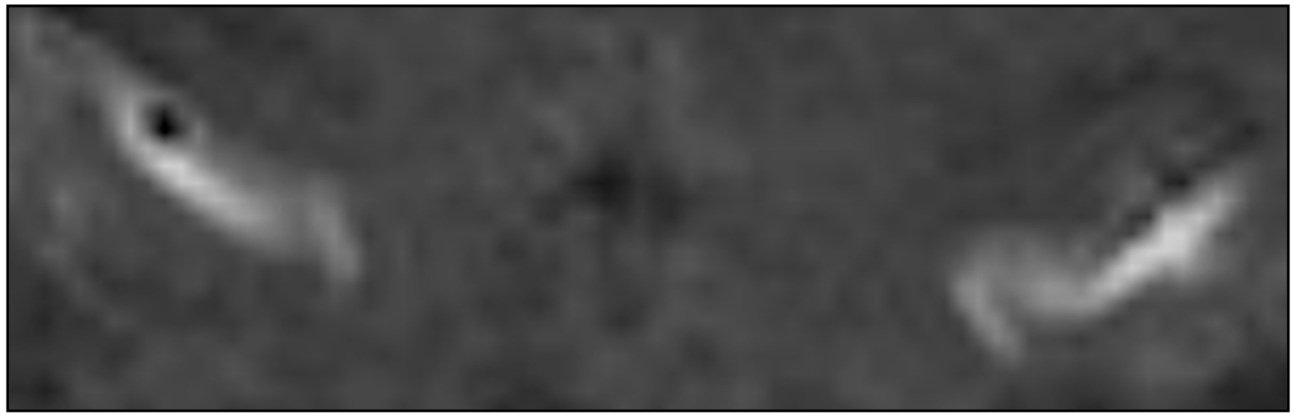


P. A. Bandettini, E. C. Wong, Magnetic resonance imaging of human brain function: principles, practicalities, and possibilities, *in* "Neurosurgery Clinics of North America: Functional Imaging" (M. Haglund, Ed.), p.345-371, W. B. Saunders Co., 1997.

Anatomy



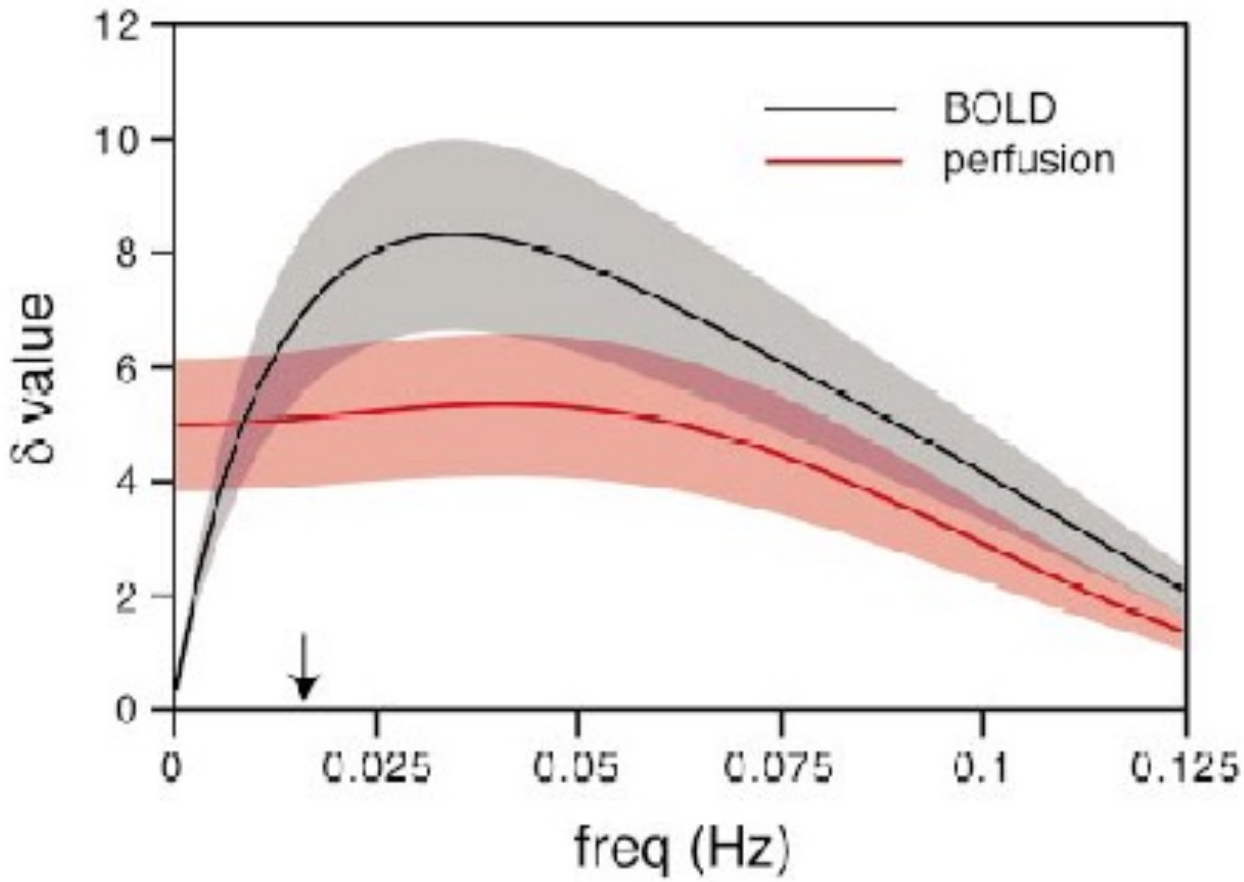
BOLD



Perfusion

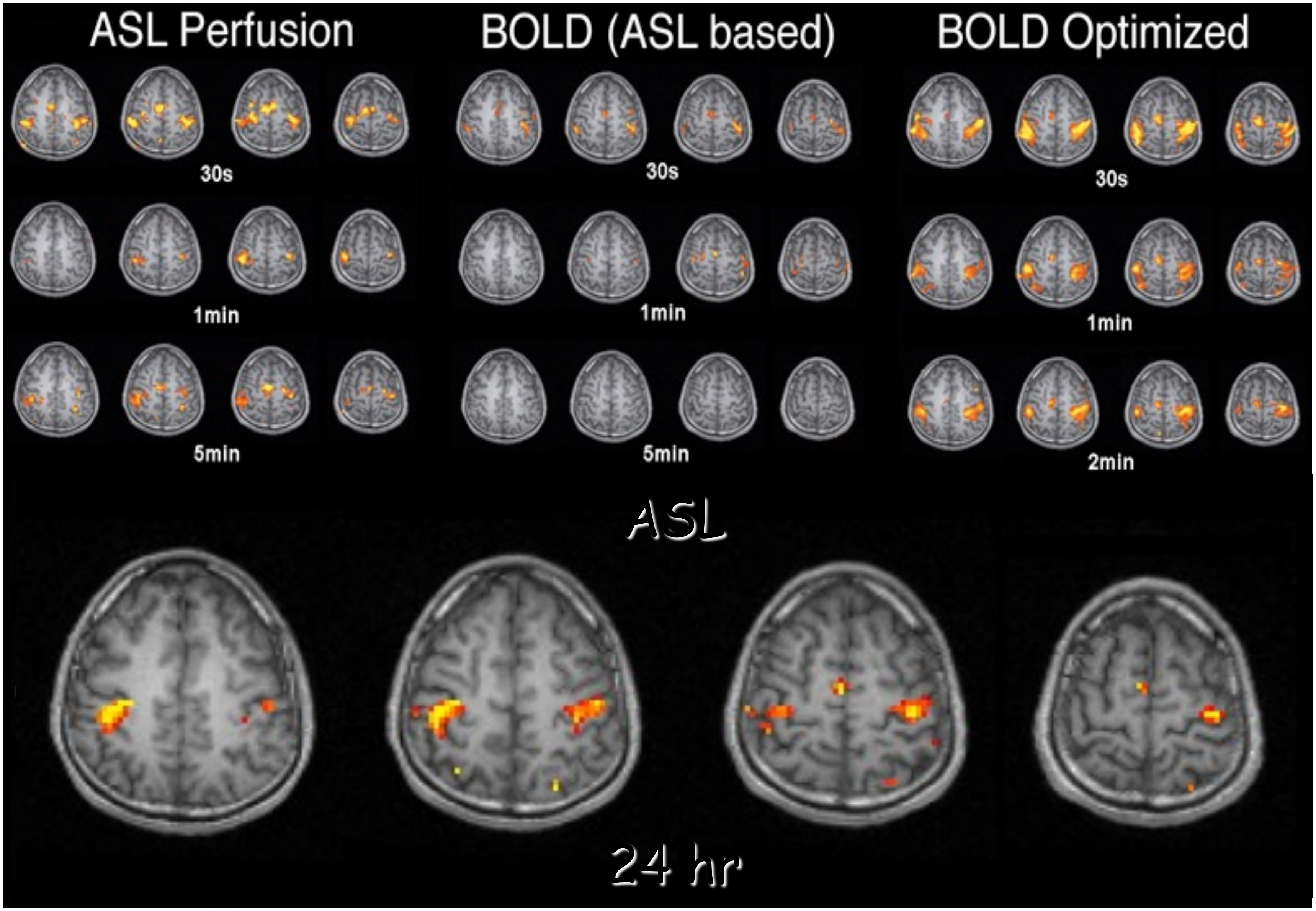
P. A. Bandettini, E. C. Wong, Magnetic resonance imaging of human brain function: principles, practicalities, and possibilities, *in* "Neurosurgery Clinics of North America: Functional Imaging" (M. Haglund, Ed.), p.345-371, W. B. Saunders Co., 1997.

Better than BOLD for long duration activation…

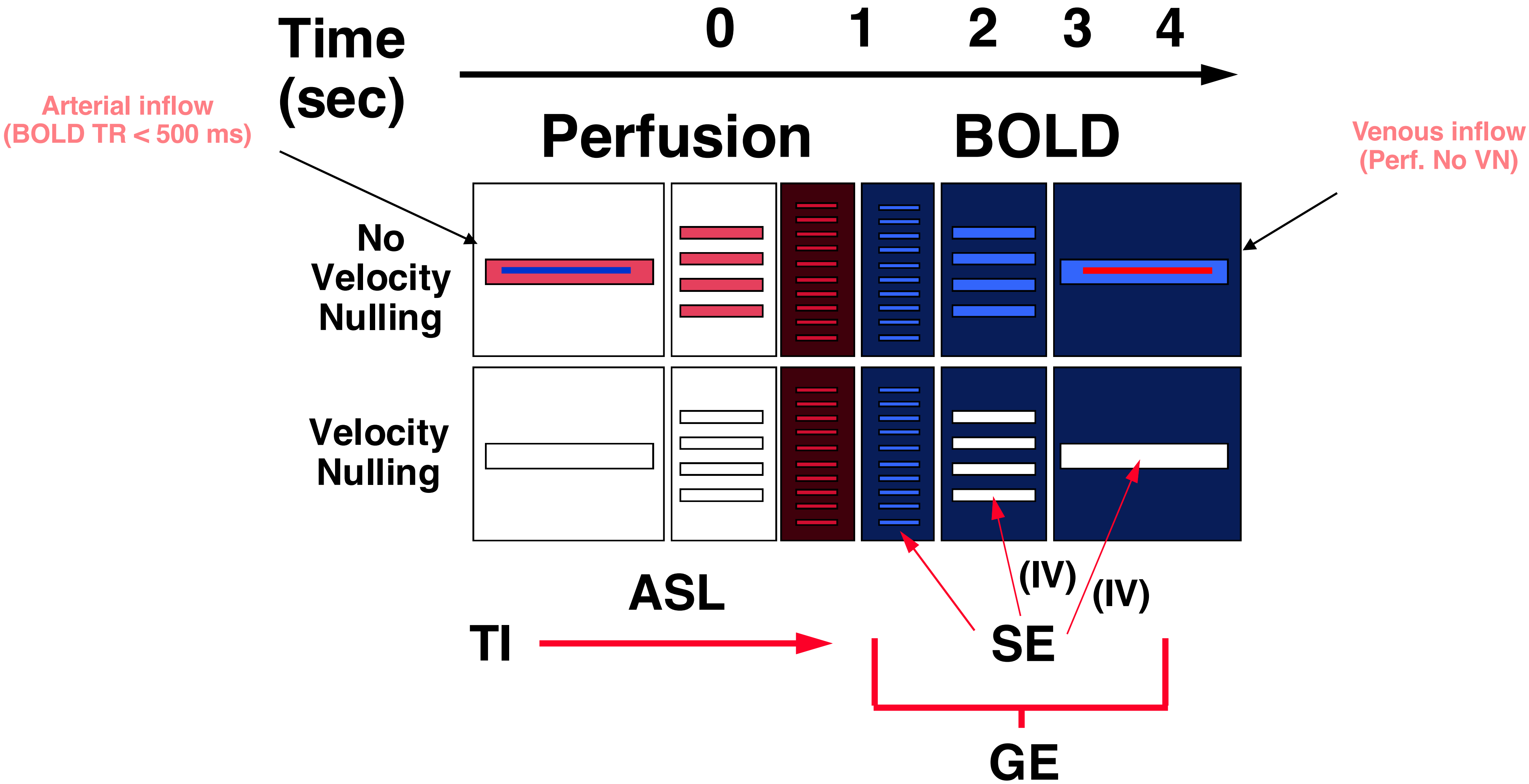


GK Aguirre et al, (2002) NeuroImage 15 (3): 488-500

Perfusion vs. BOLD: Low Task Frequency



Hemodynamic Specificity



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- Volume (gadolinium)
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- $\Delta CMRO_2$
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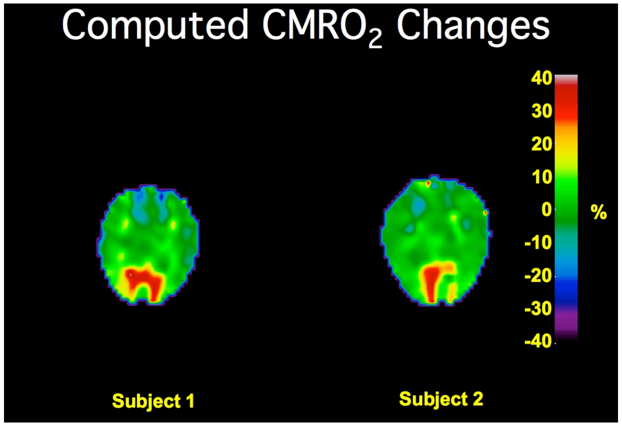
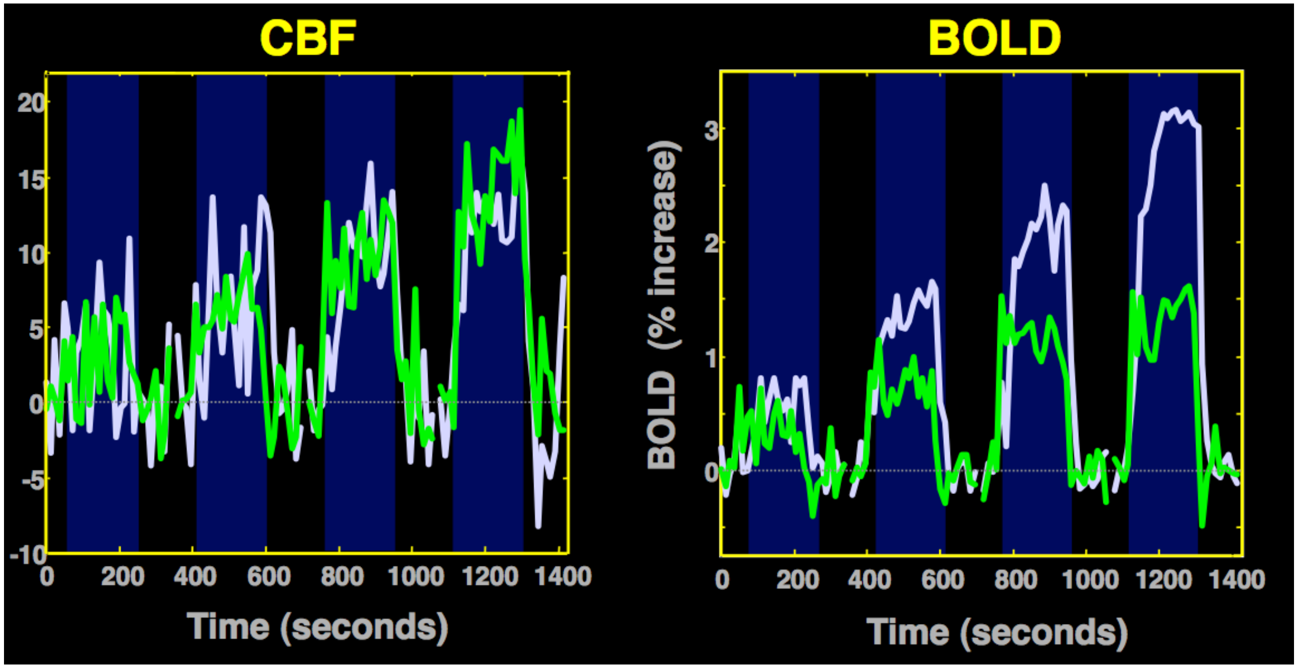
Activation-induced $CMRO_2$ changes



-requires a global hemodynamic stress
-assumption is that $CMRO_2$ unchanged with global stress
-requires simultaneous flow and BOLD collection

R. D. Hoge, et al, PNAS 96: 9403-9408, 1999



Visual = green
Hypercapnia = white

Functional Contrast

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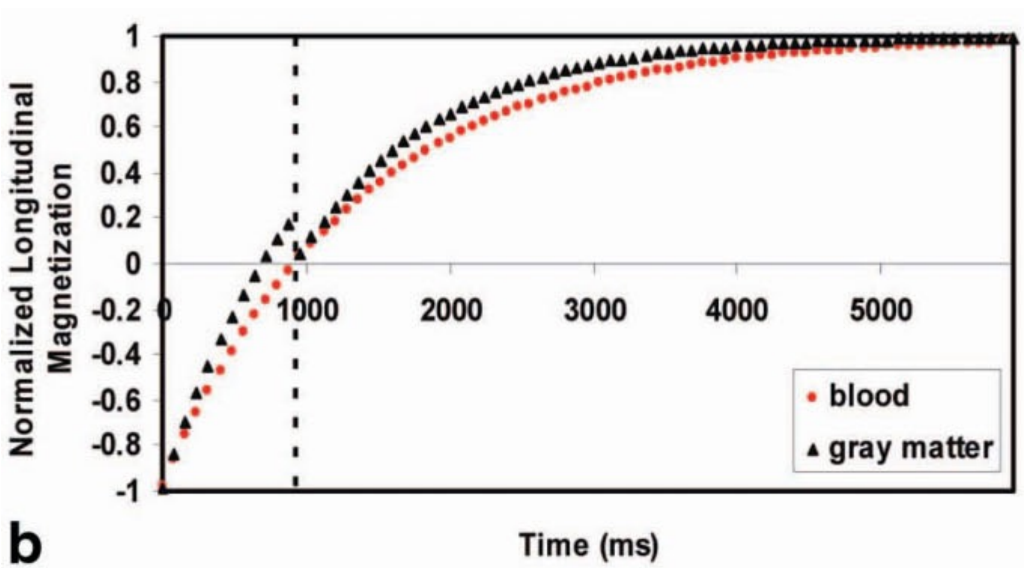
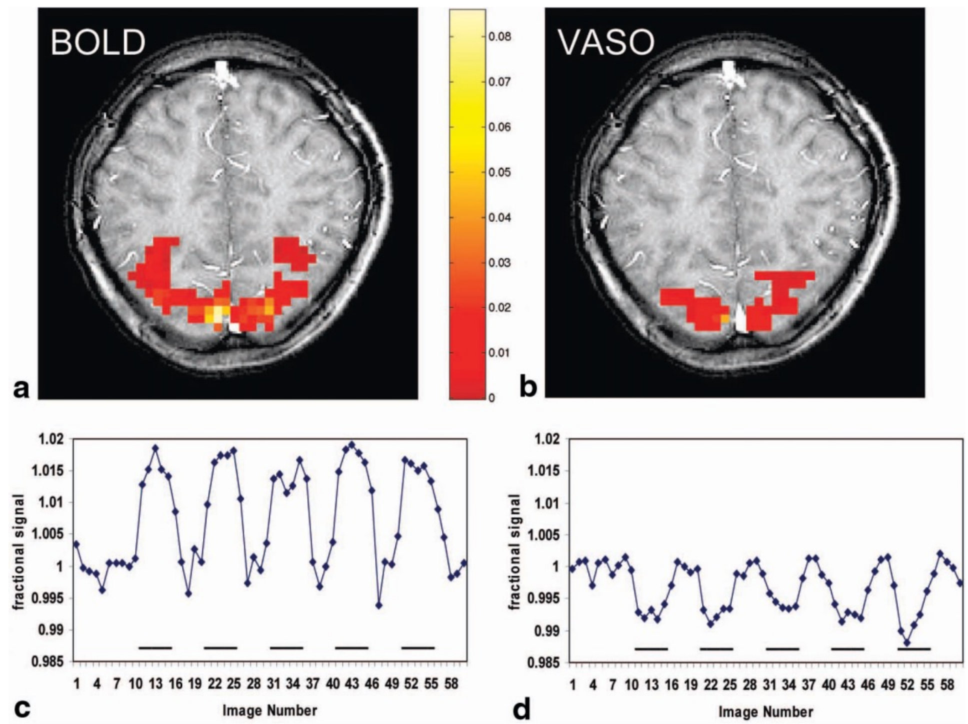
- **Temperature**

Activation-induced Blood Volume Changes: “VASO”

H. Lu, et al, MRM 50: 263-274, 2003



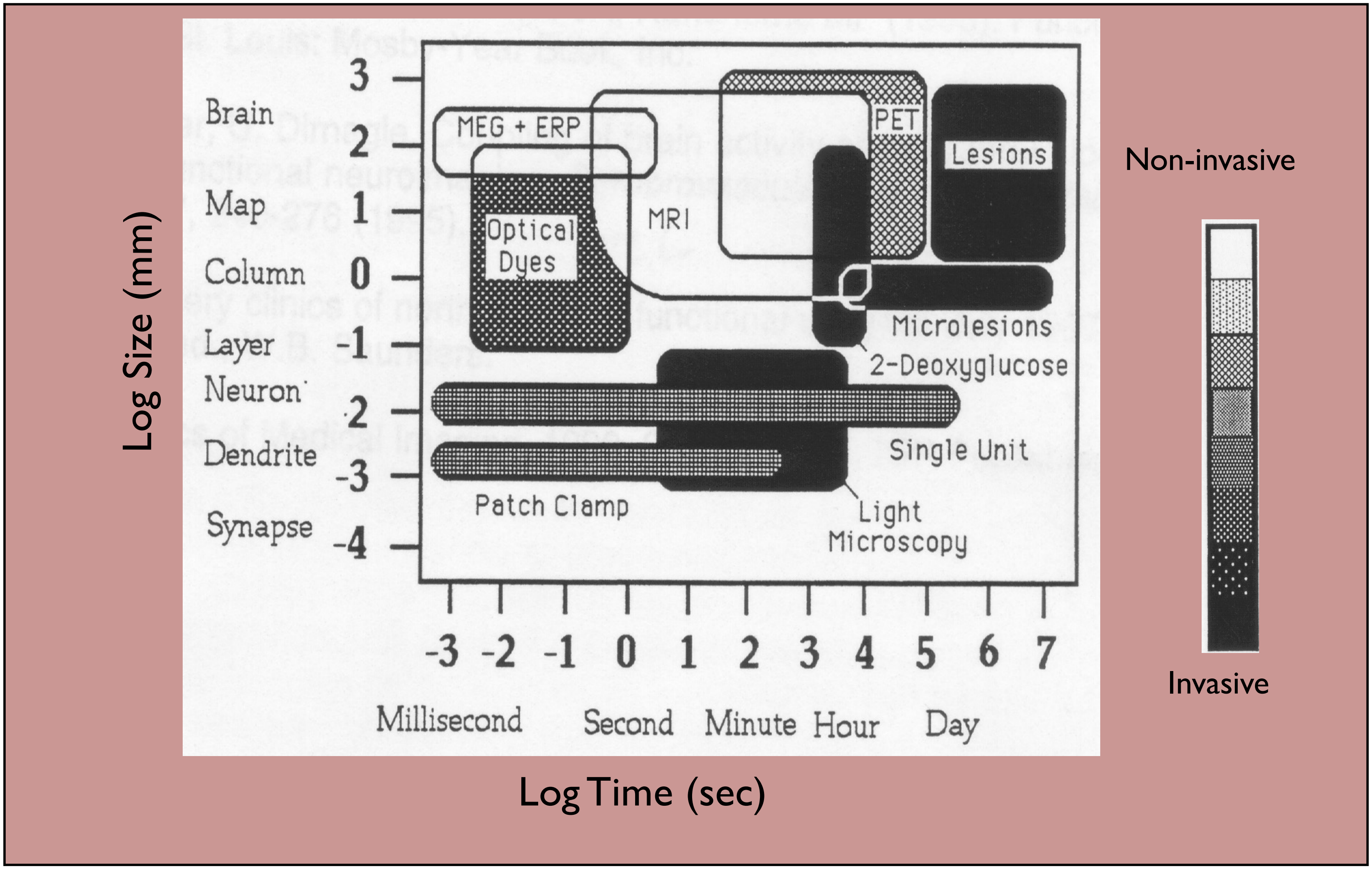


Null blood based on T1 difference between blood and tissue
..more blood -> less signal.

Extracting Information from the fMRI Signal:

- **Spatial Resolution**
- **Temporal Resolution**
- **Sensitivity**

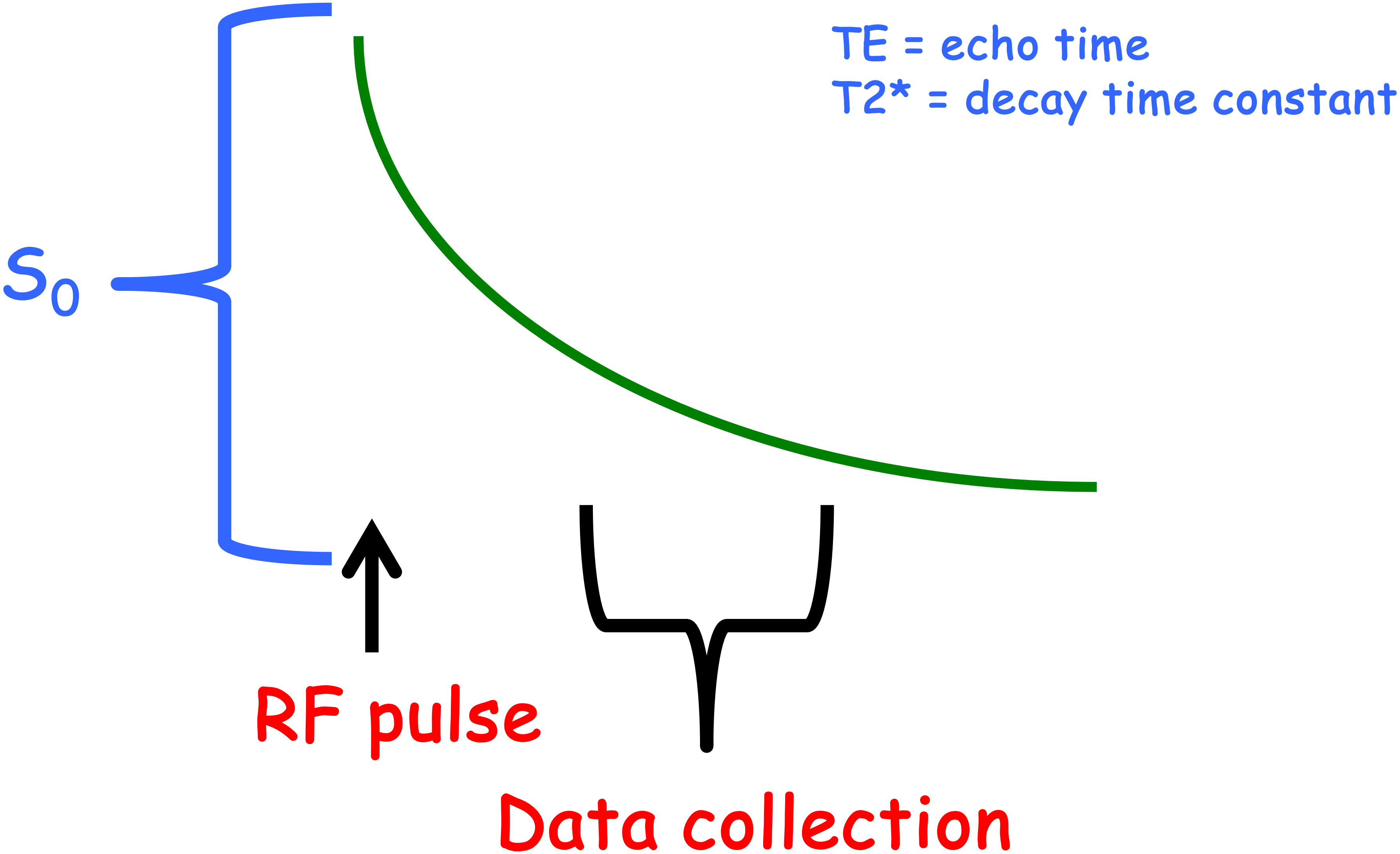
Functional Neuroimaging Techniques

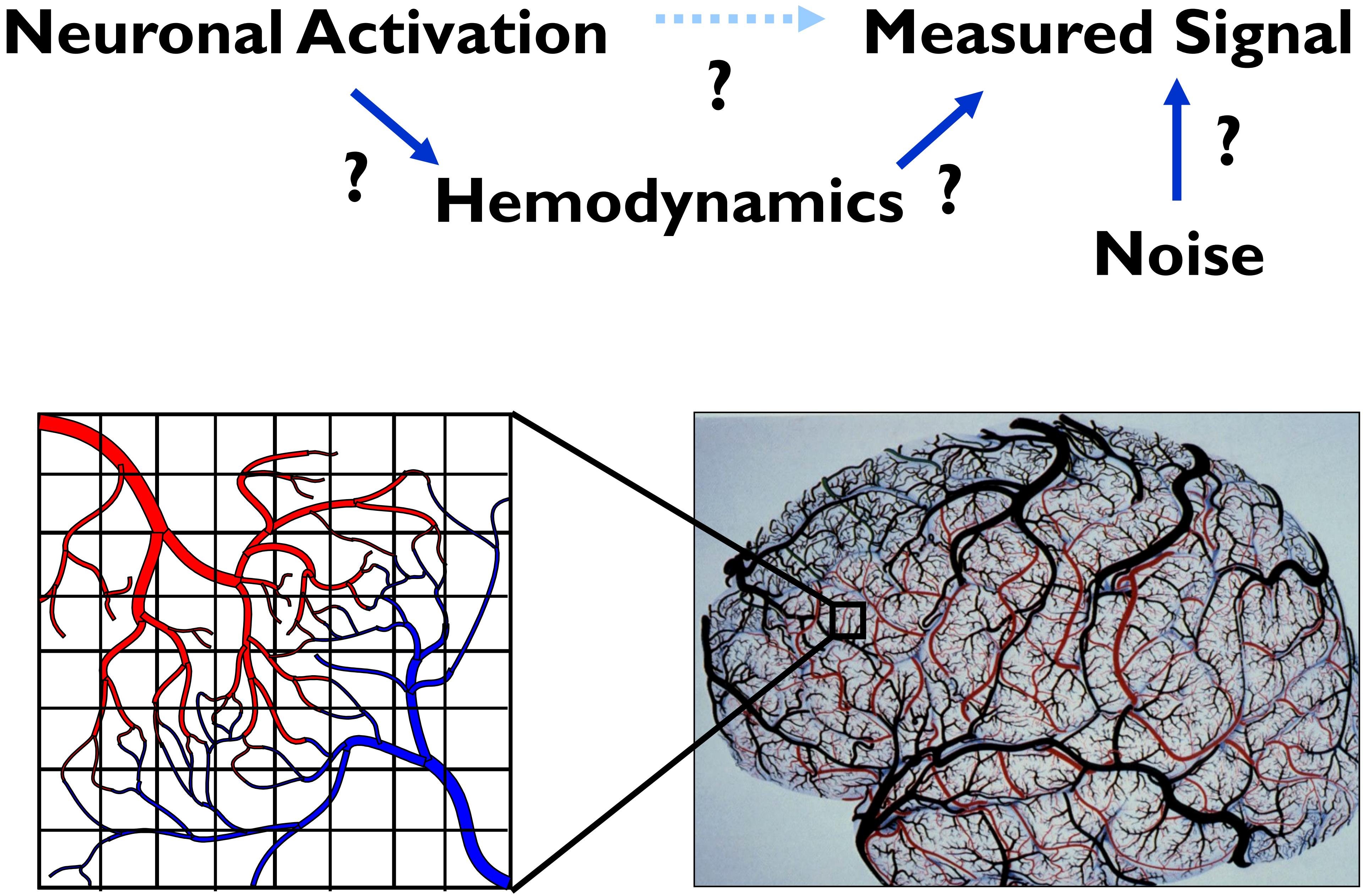


Extracting Information from the fMRI Signal:

- Spatial Resolution
- Temporal Resolution
- Sensitivity

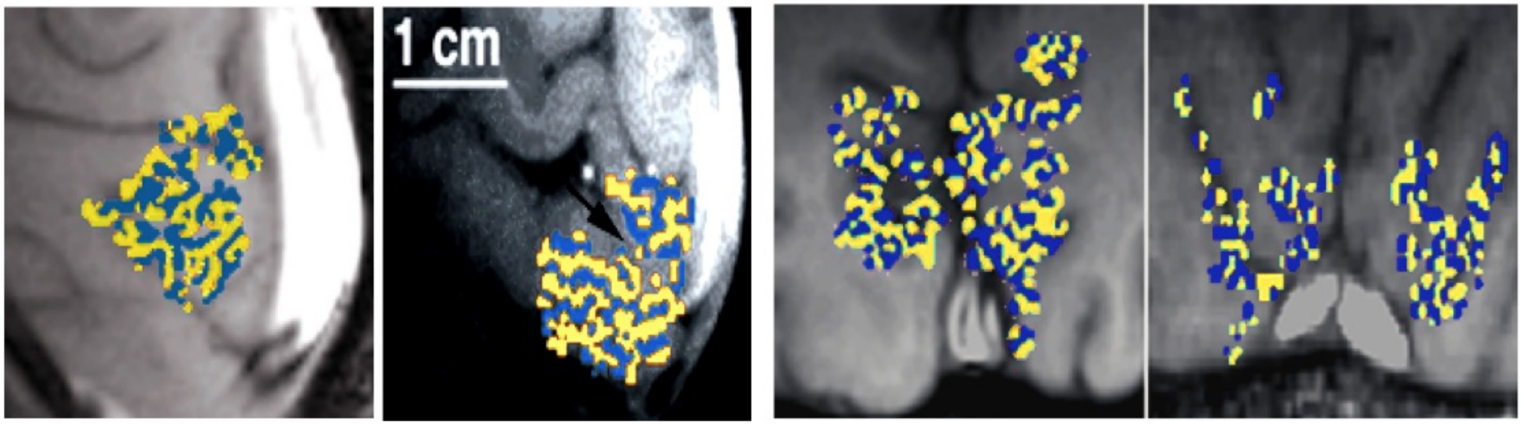
$$\text{Signal} = S_0\, e^{-TE/T2^*}$$





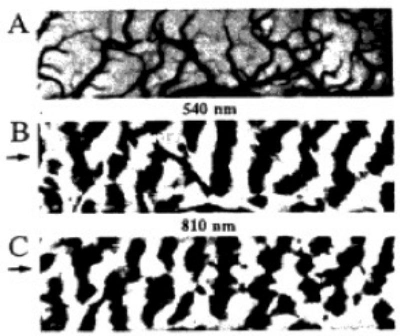
Neuronal Activation
Measured Signal
?
?
Hemodynamics
?
?
Noise

Ocular Dominance Column Mapping

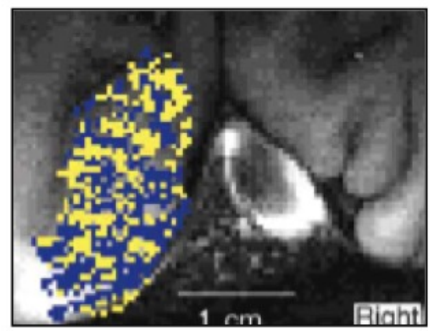


Menon, R. S., S. Ogawa, et al. (1997). J Neurophysiol 77(5): 2780-7.
0.54 x 0.54 in plane resolution

Optical Imaging



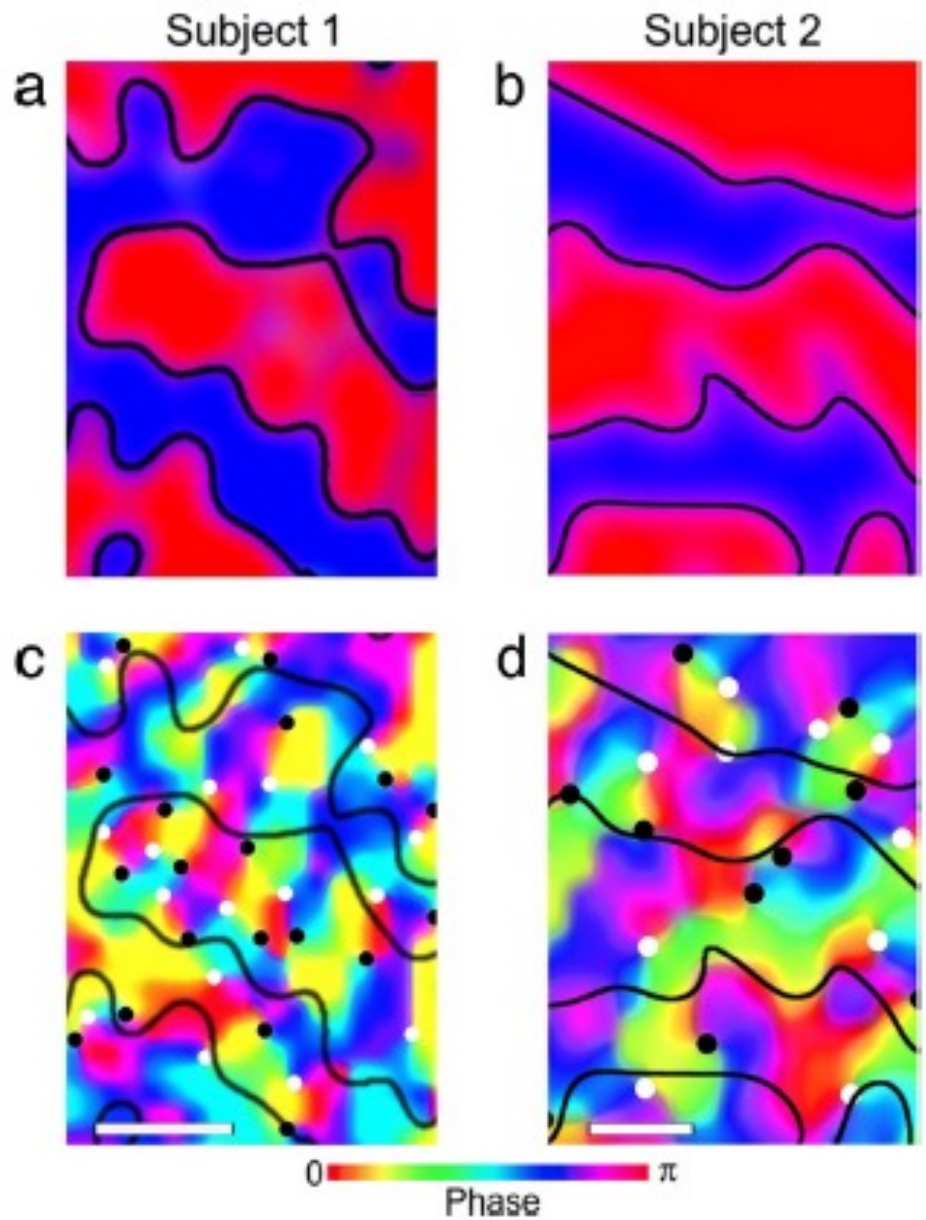
R. D. Frostig et. al, PNAS
87: 6082-6086, (1990).



Cheng, et al. (2001)
Neuron,32:359-374

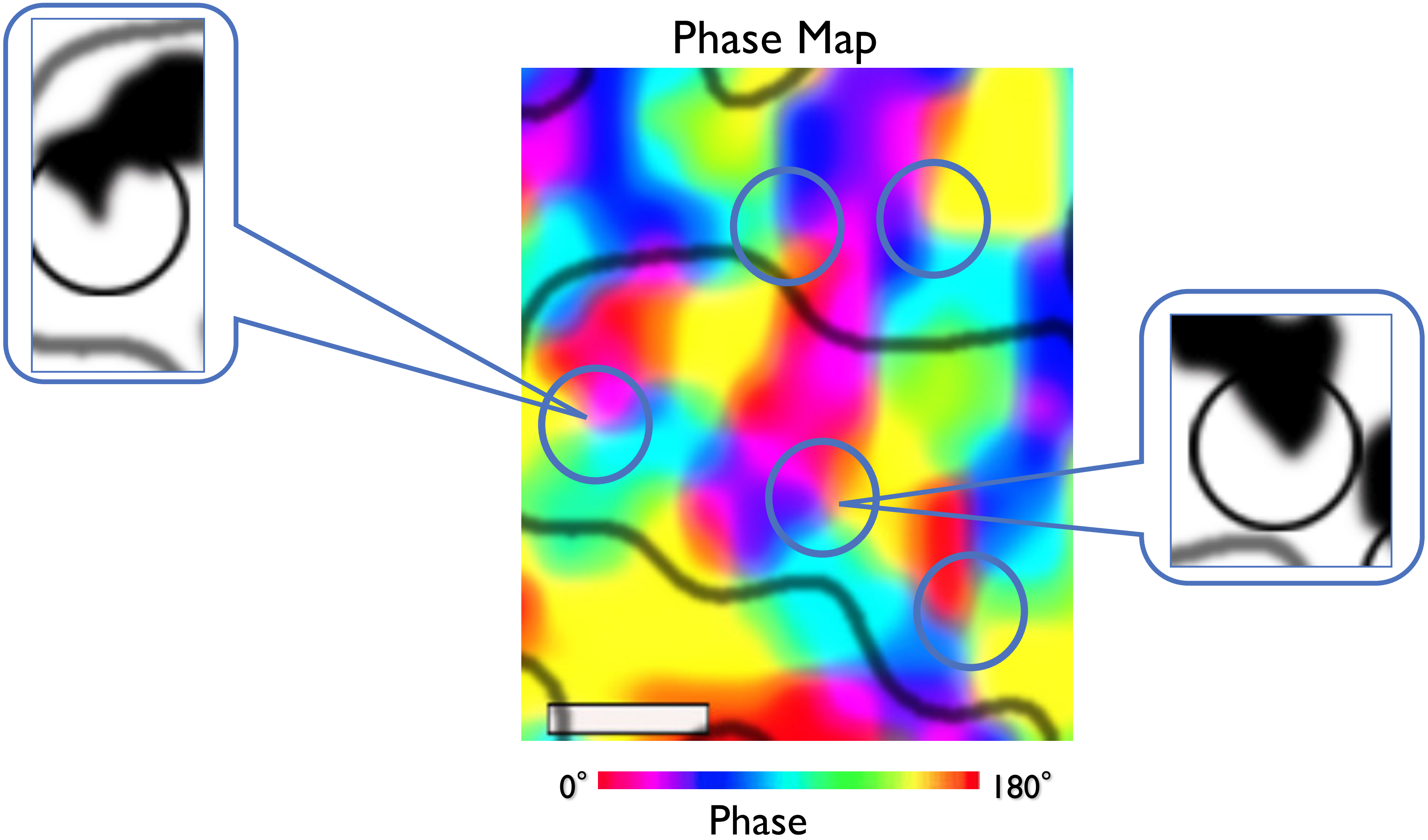
0.47 x 0.47 in plane resolution

3.5mm at 1.5T (S. Engel et al - 1994)
3.9mm (GE), 3.4mm (SE) at 3T (L. Parkes et al - 2005)
2.3 mm at 7T (A. Schmuel et al - 2007)



Yacoub et al. PNAS 2008

Orientation Columns in Human V1 as Revealed by fMRI at 7T

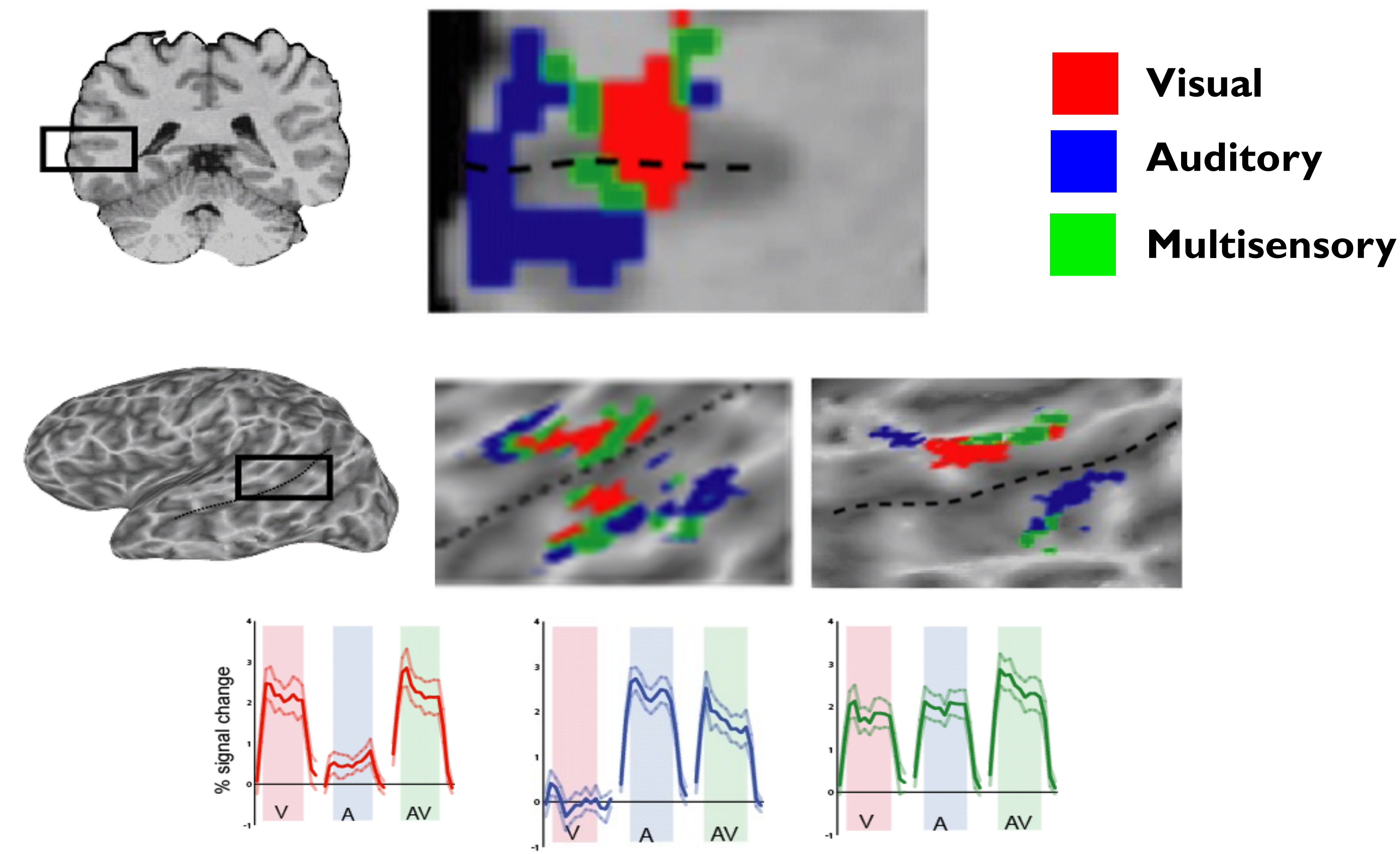


Scalebar = 0.5 mm

Yacoub et al. PNAS 2008

Multi-sensory integration

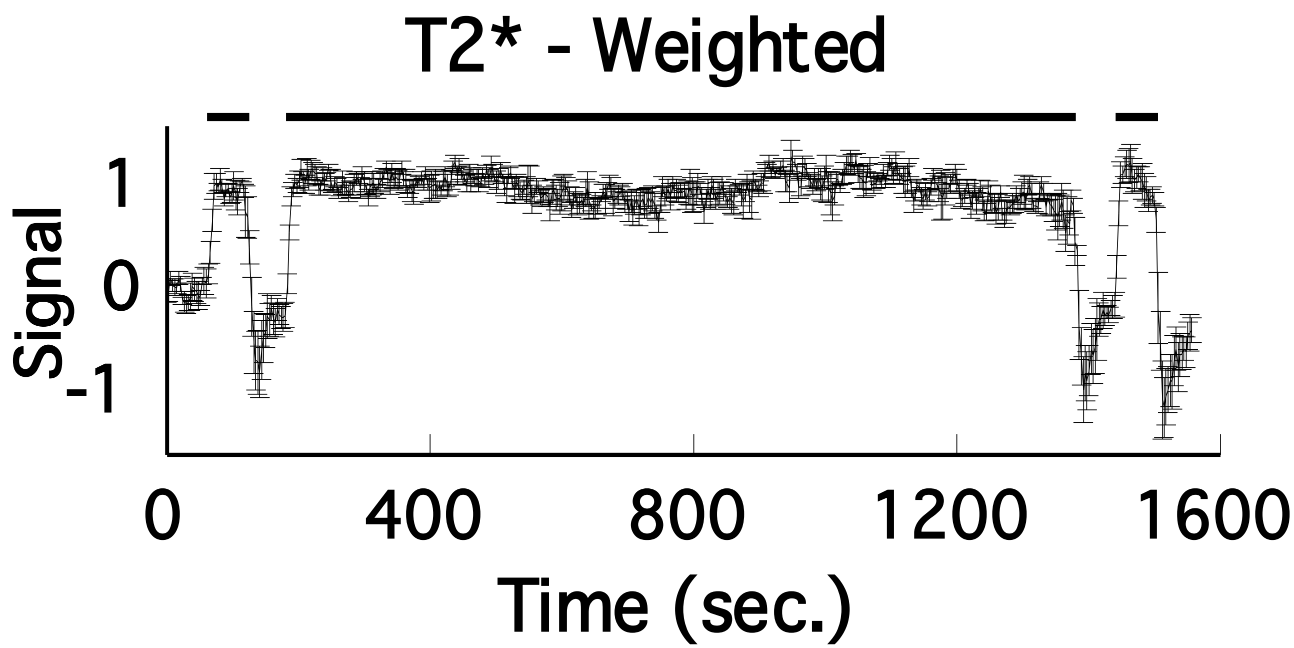
M.S. Beauchamp et al.,



Extracting Information from the fMRI Signal:

- Spatial Resolution
- Temporal Resolution
- Sensitivity

20 minutes continuous activation



P. A. Bandettini, K. K. Kwong, T. L. Davis, R. B. H. Tootell, E. C. Wong, P. T. Fox, J. W. Belliveau, R. M. Weisskoff, B. R. Rosen, (1997). "Characterization of cerebral blood oxygenation and flow changes during prolonged brain activation." ***Human Brain Mapping*** **5, 93-109.**

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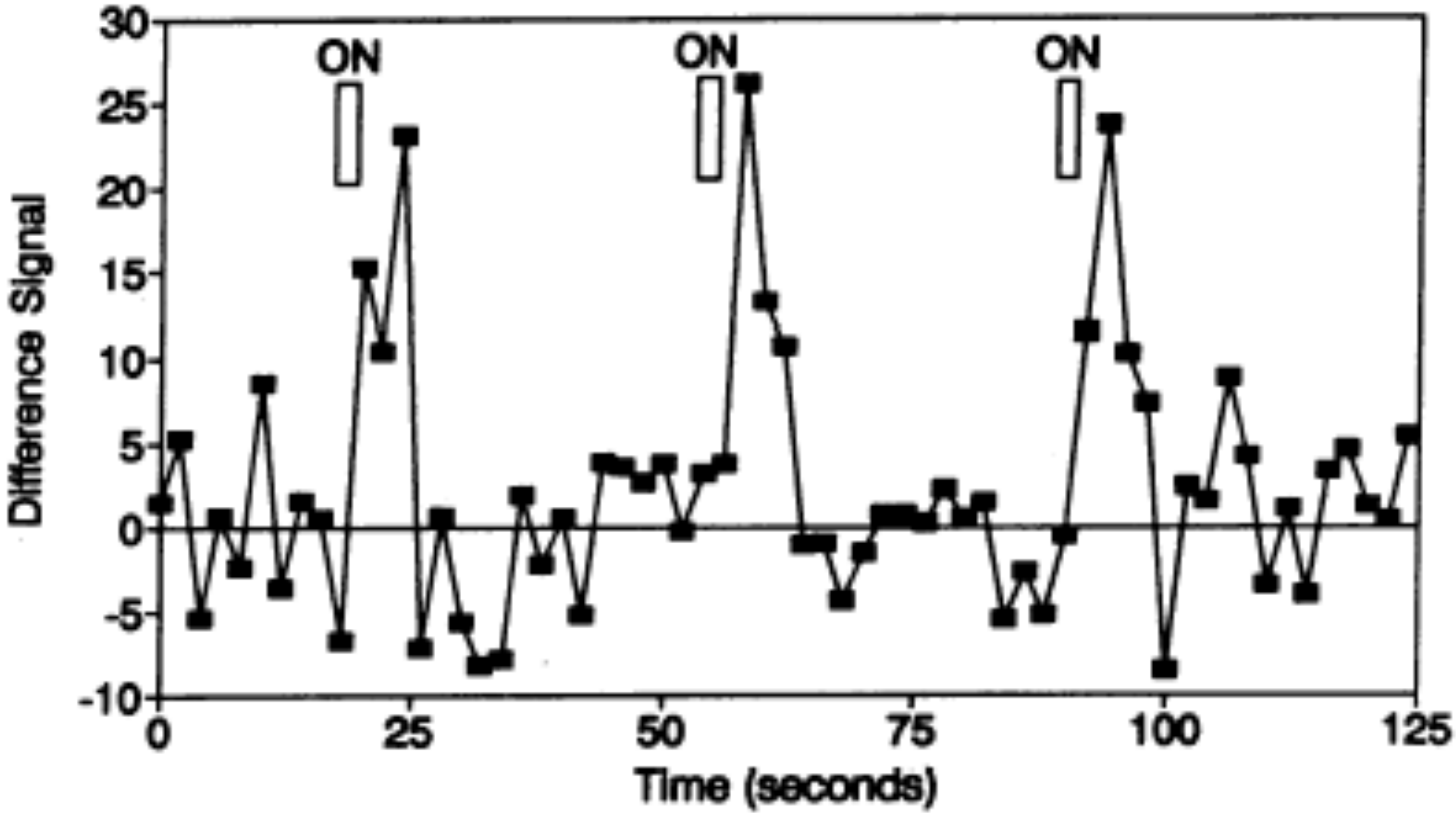
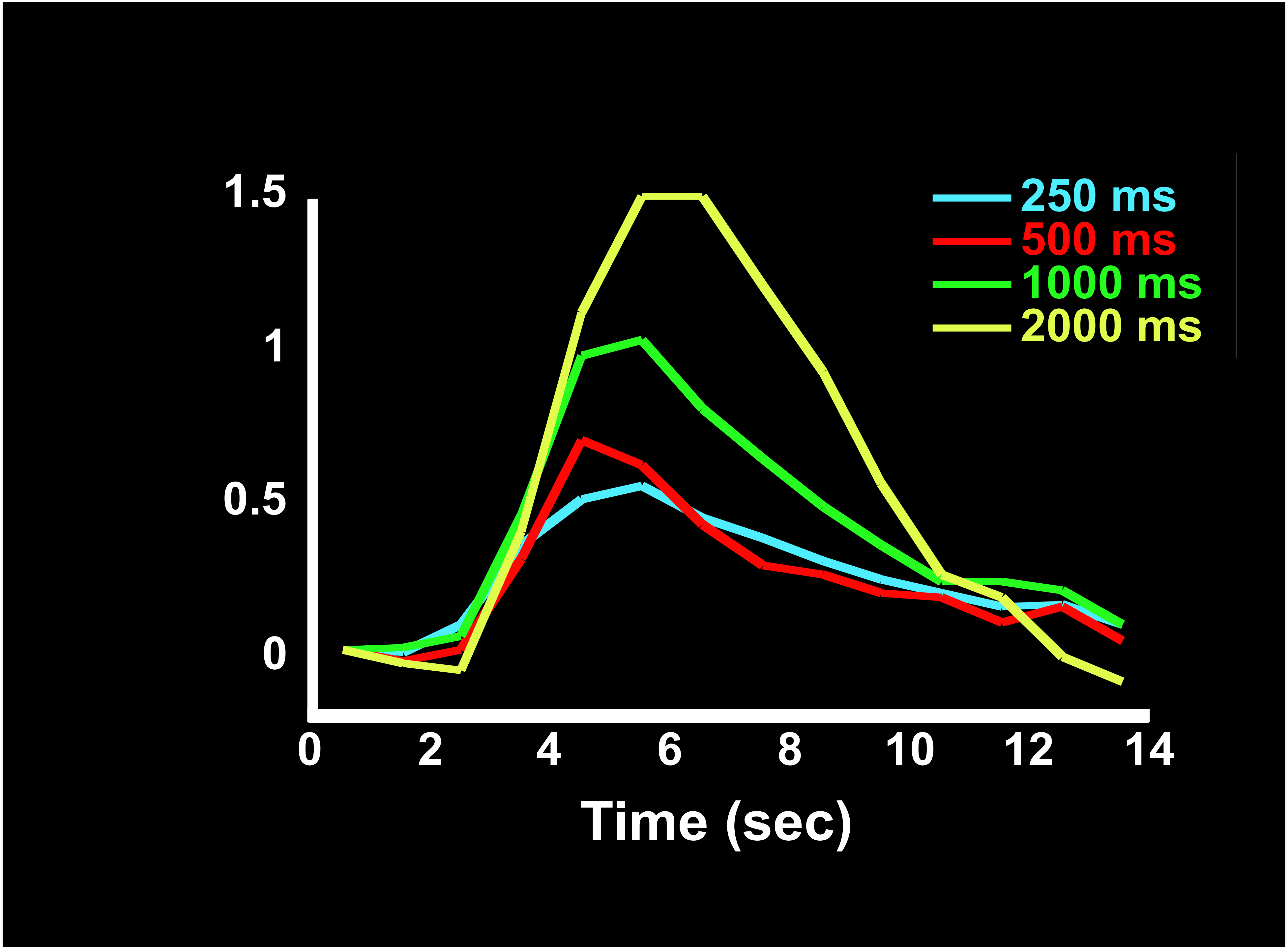
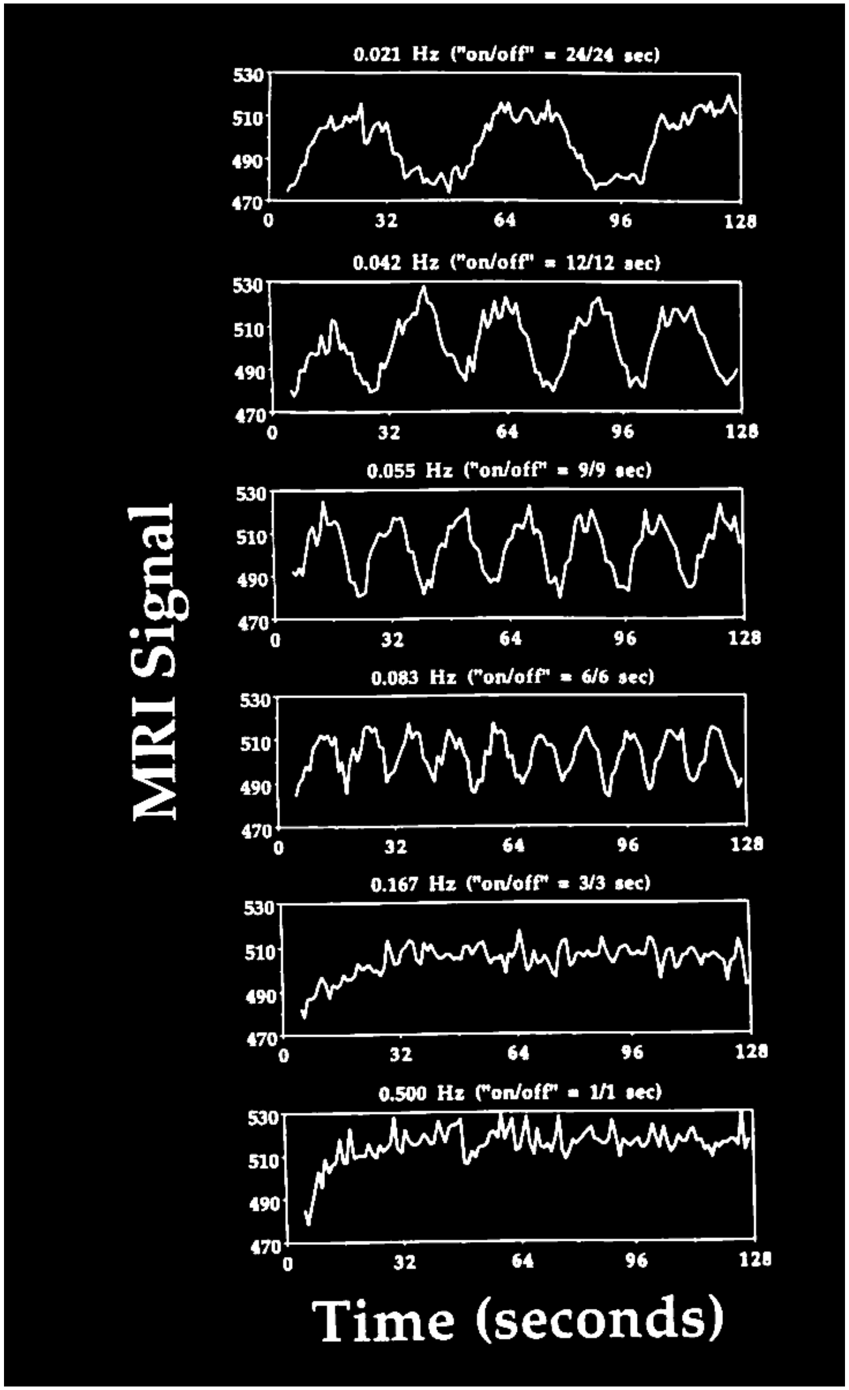
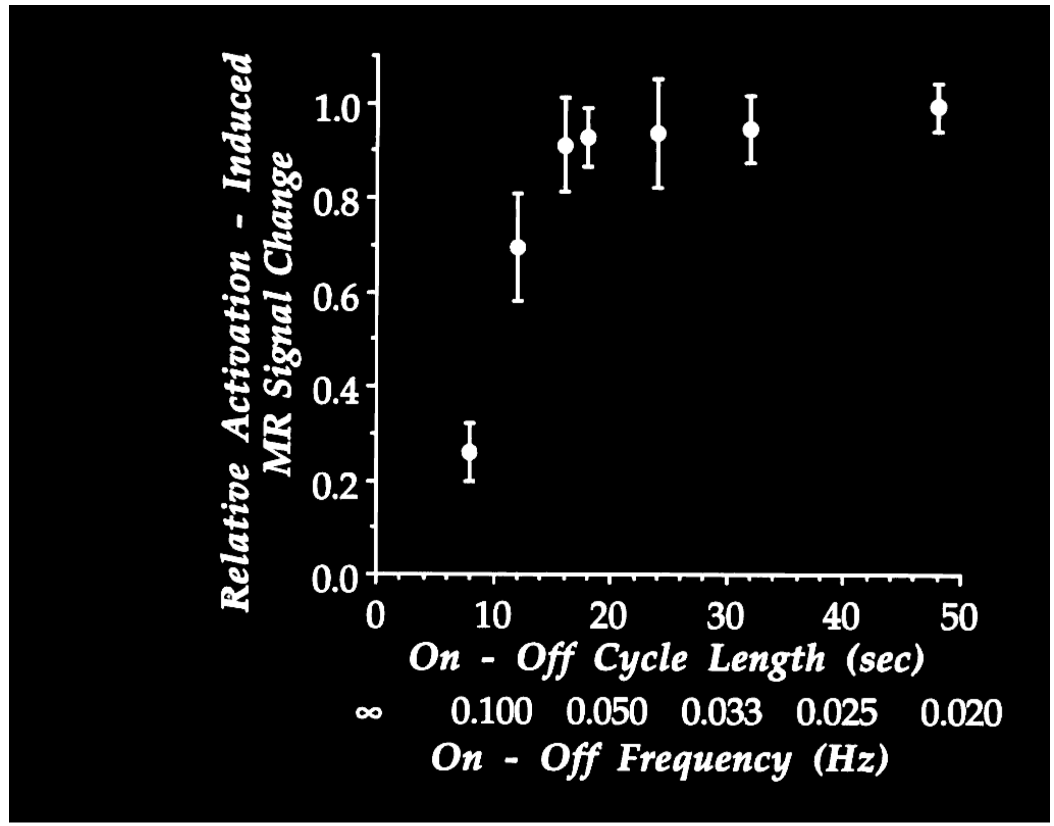

ON
ON
ON
Difference Signal
30
25
20
15
10
5
0
-5
-10
0
25
50
75
100
125
Time (seconds)


250 ms
500 ms
1000 ms
2000 ms
1.5
1
0.5
0
0
2
4
6
8
10
12
14
Time (sec)



How rapidly can one switch on and off?

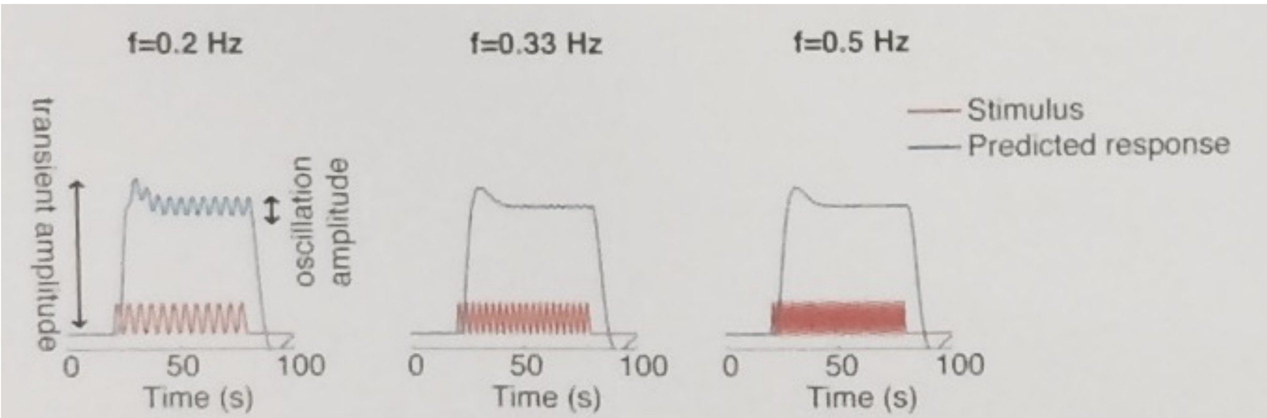


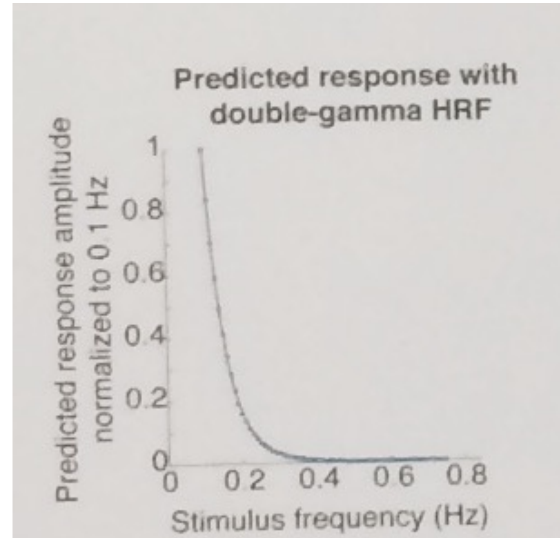
P. A. Bandettini,, Functional MRI using the BOLD approach: dynamic characteristics and data analysis methods, in "Diffusion and Perfusion: Magnetic Resonance Imaging" (D. L. Bihan, Ed.), p.351-362, Raven Press, New York, 1995.

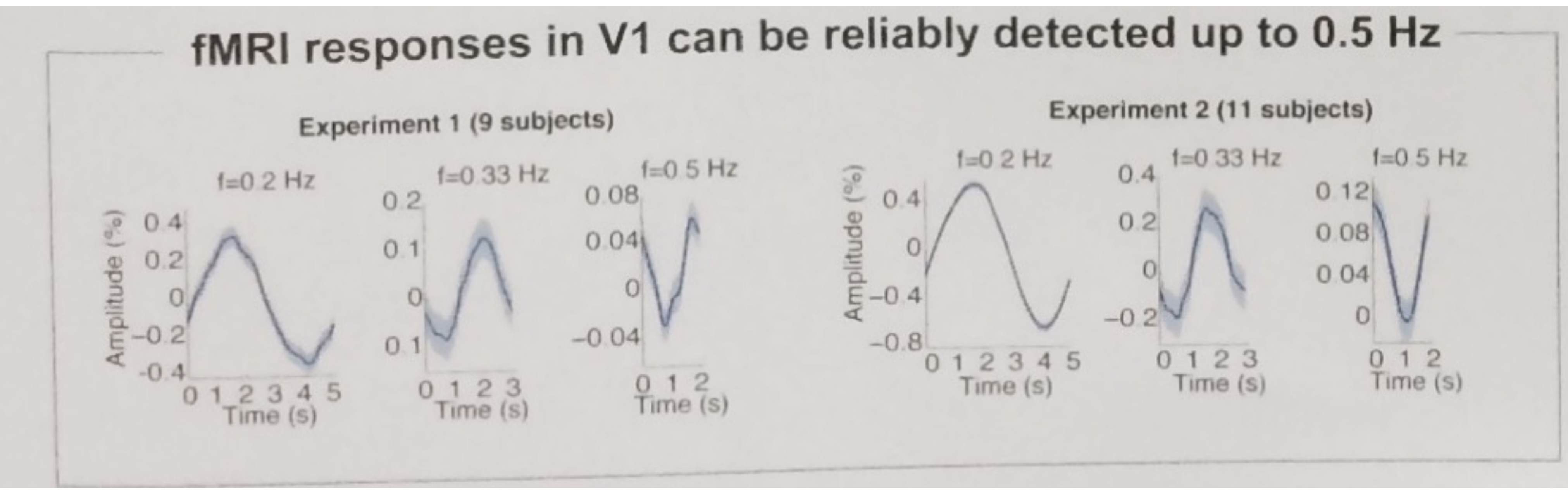
Detection of delta-band oscillations in visual cortex using fast fMRI and simultaneous EEG-fMRI

Laura D. Lewis, Kawin Setsompop, Bruce R. Rosen, Jonathan R. Polimeni

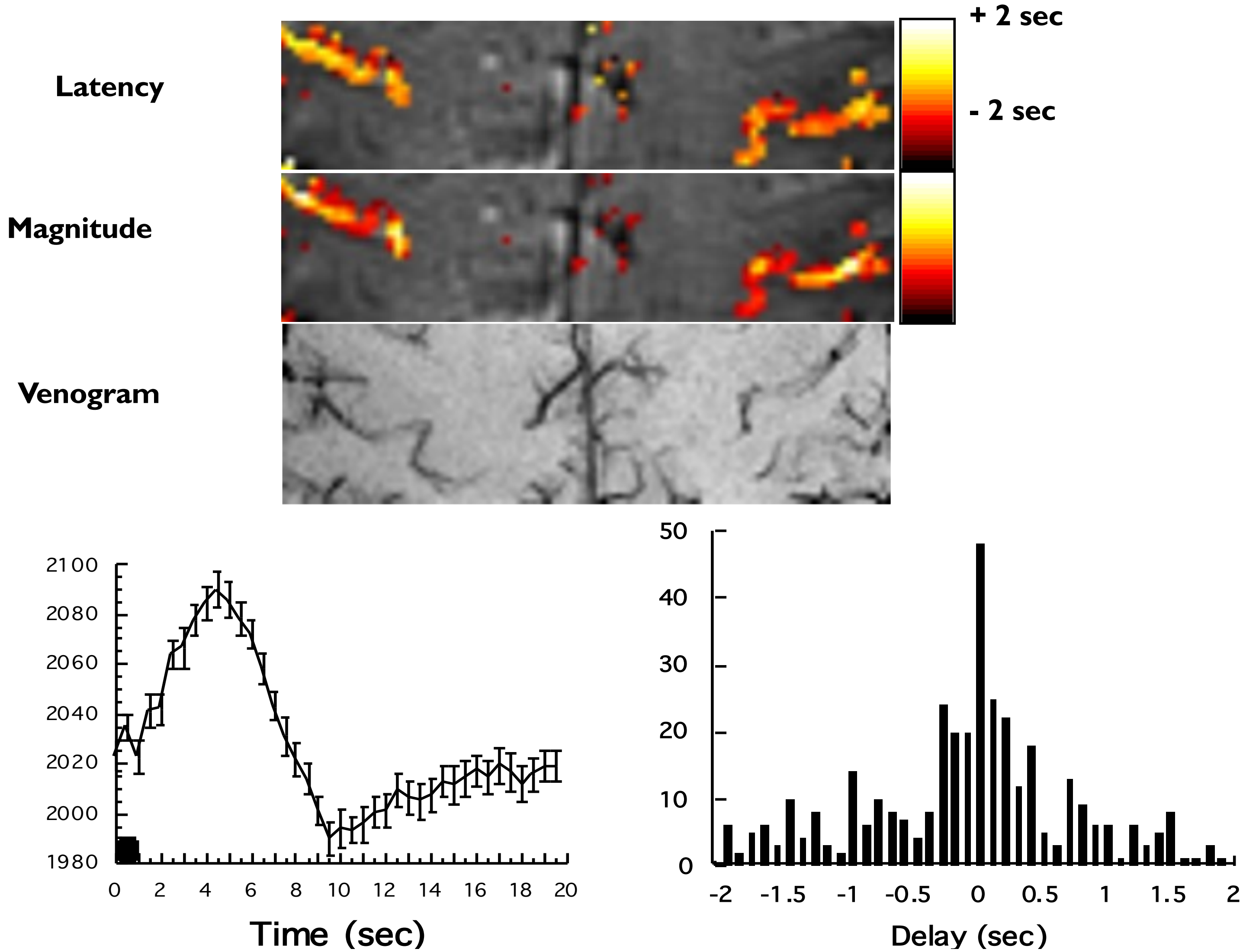
OHBM 2015







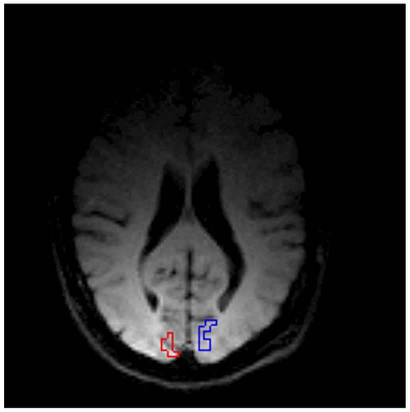
Latency Variation…



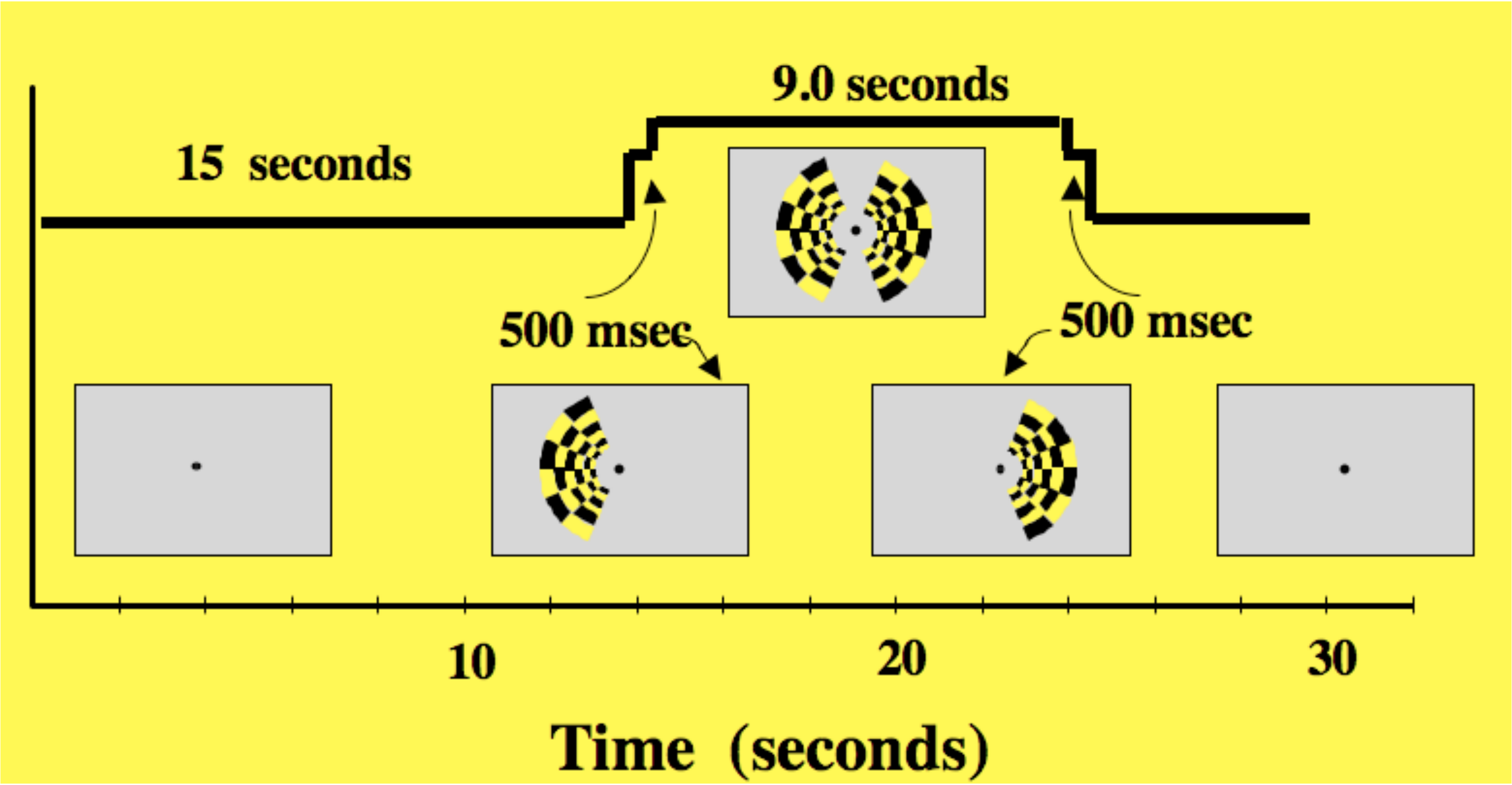
P.A. Bandettini, (1999) "Functional MRI" 205-220.

Hemi-Field Experiment

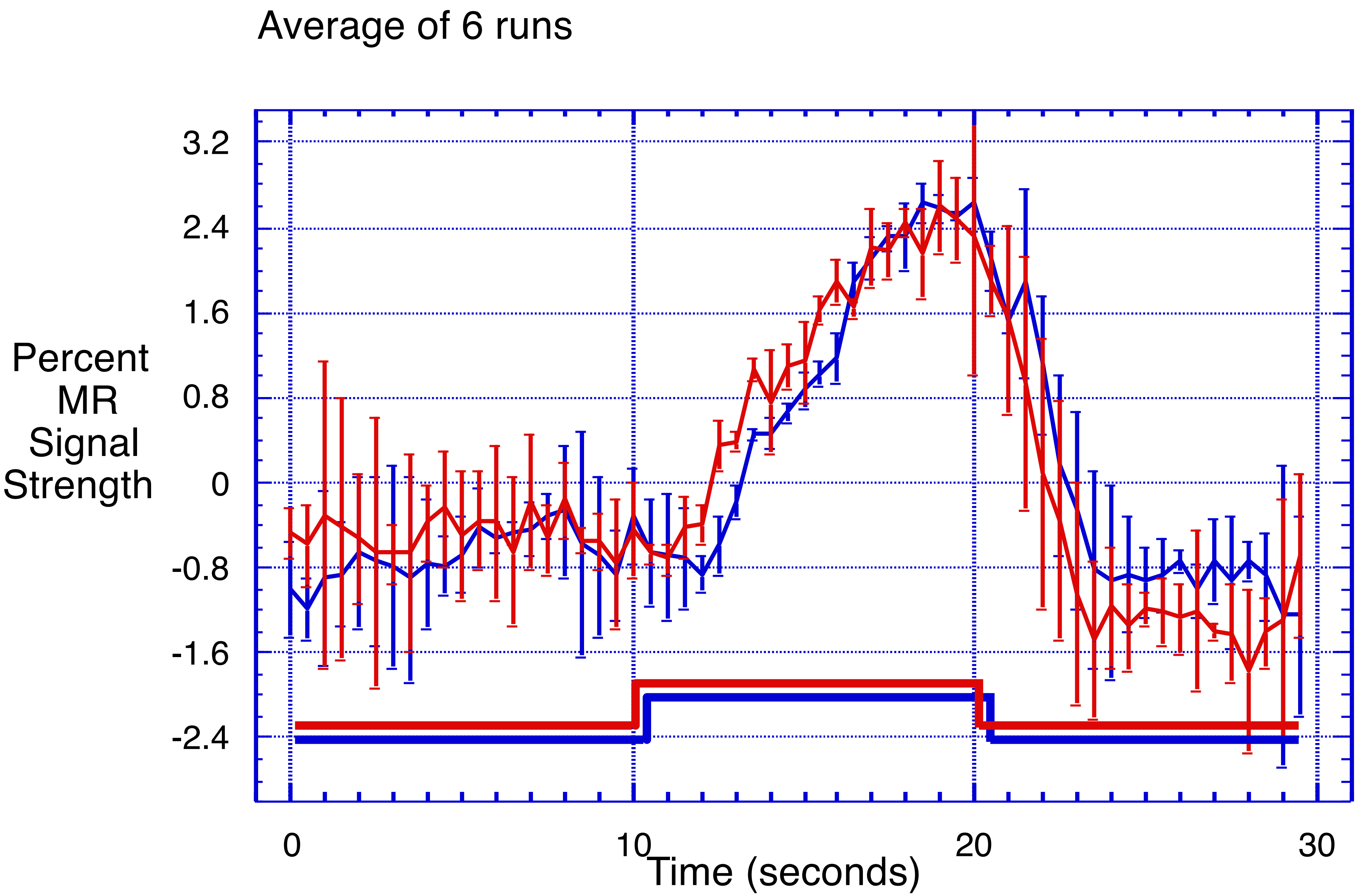
Right Hemisphere



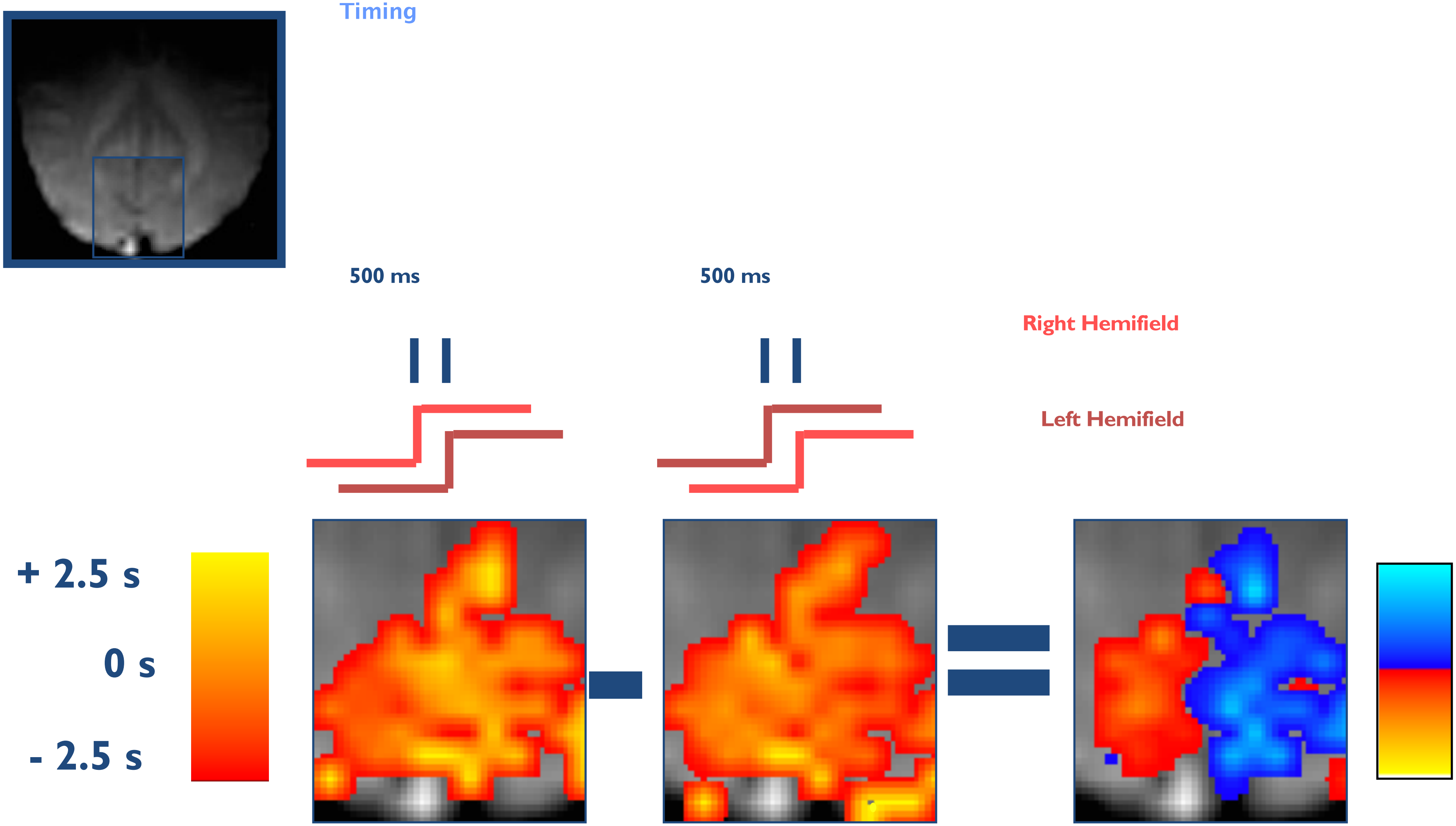
Left Hemisphere



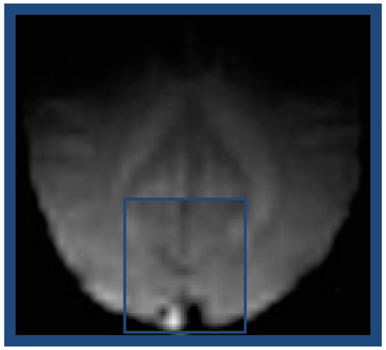
Hemi-field with 500 msec asynchrony

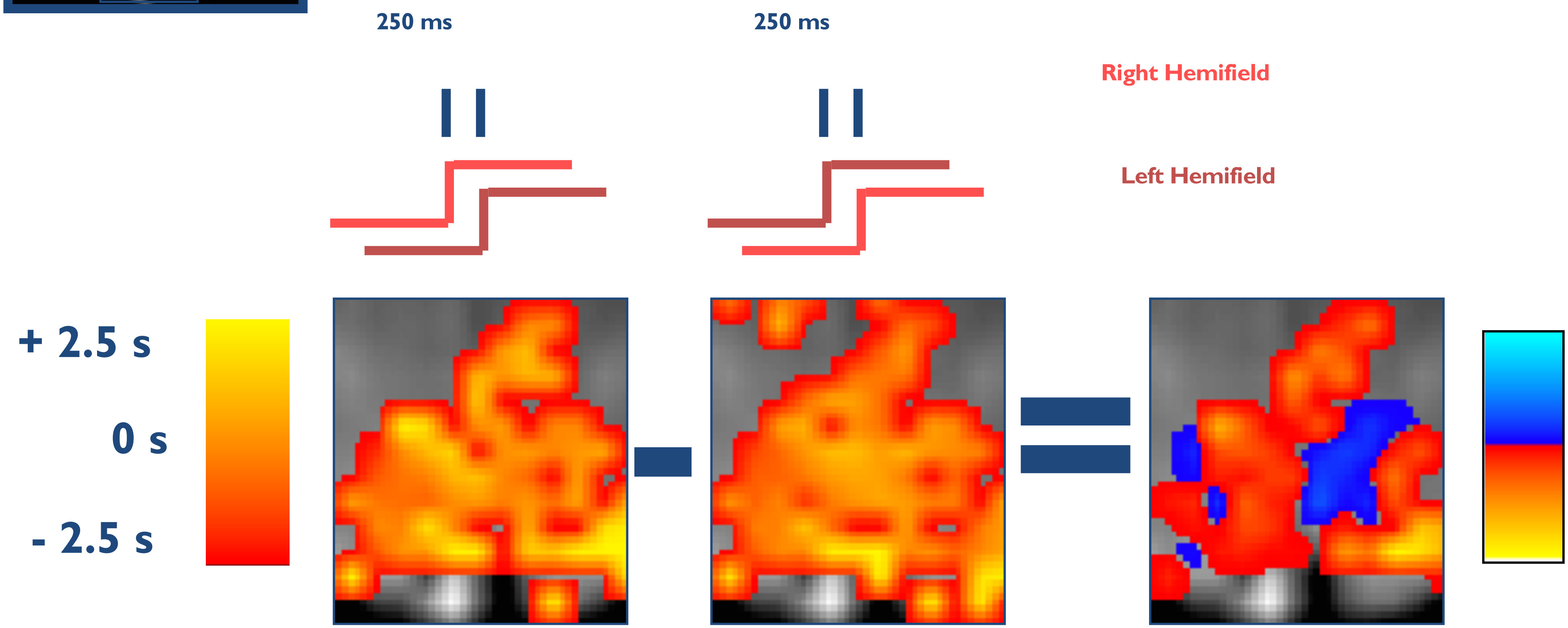


Timing

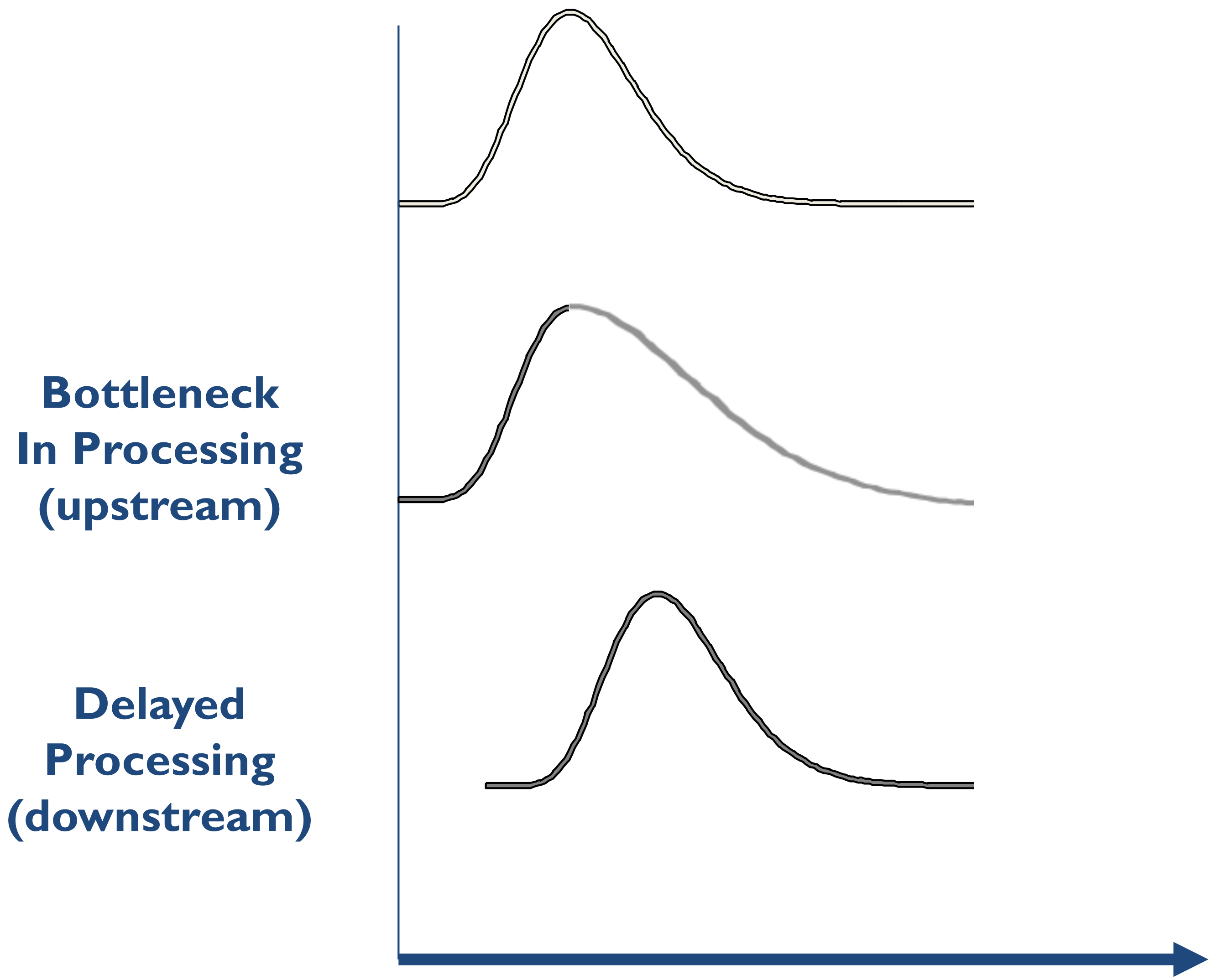


Timing



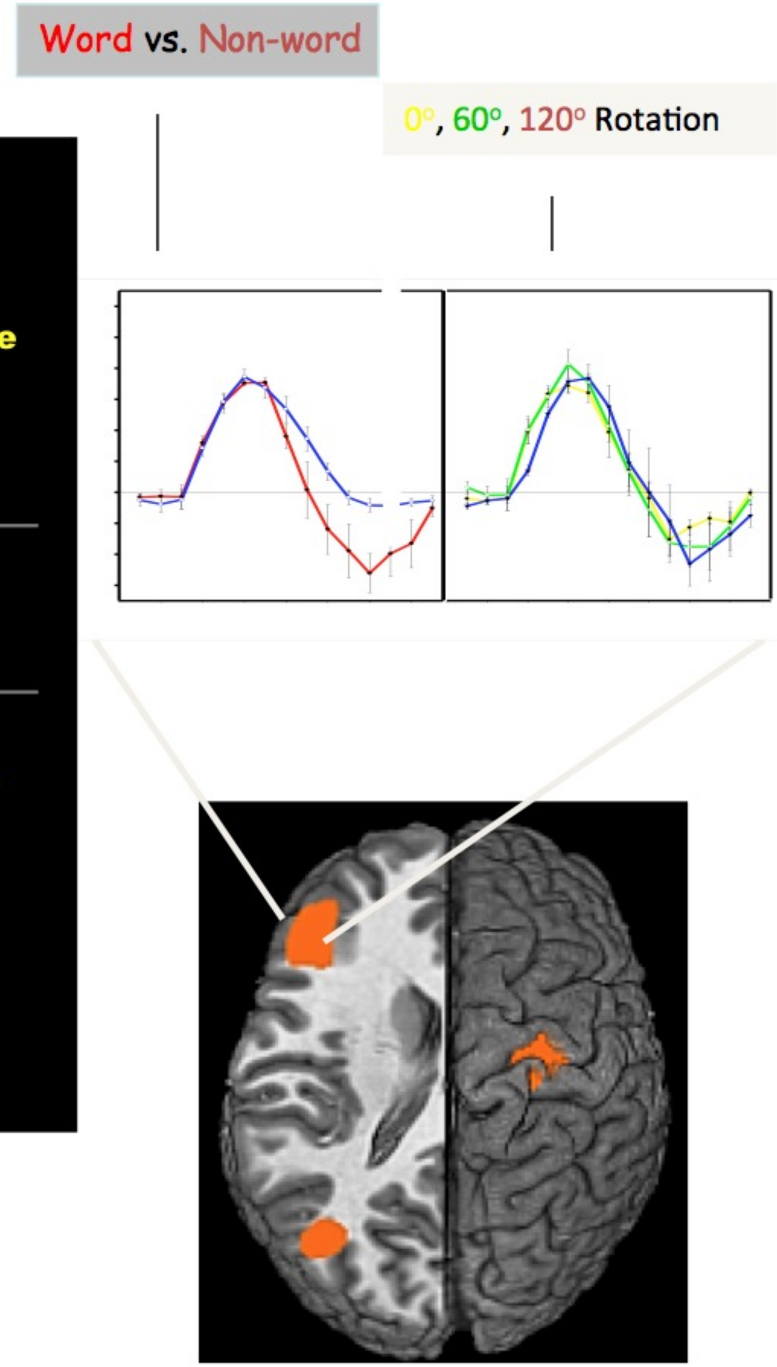


Hemodynamic Response Modulation



Lexical Delay

Rotational Delay	Words	Non-Words	Mean Reaction Time
0°	smudge	dierts	823 ms
60°	frolic	cuhlos	891 ms
120°	slouch	gedmus	1446 ms
Mean Reaction Time	986 ms	1219 ms	

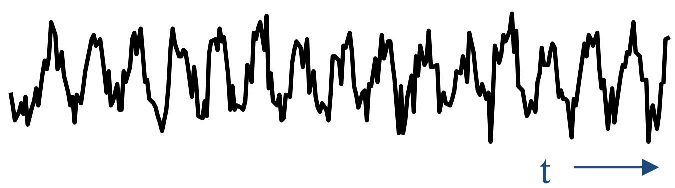


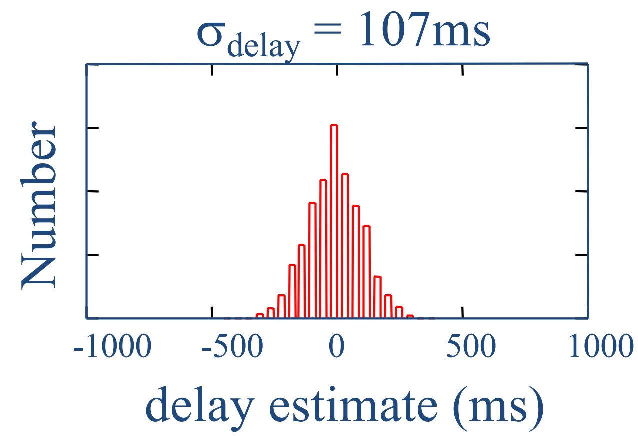
Bellgowan, et al (2003), PNAS 100, 15820–15283

Even if no hemodynamic variability exists…

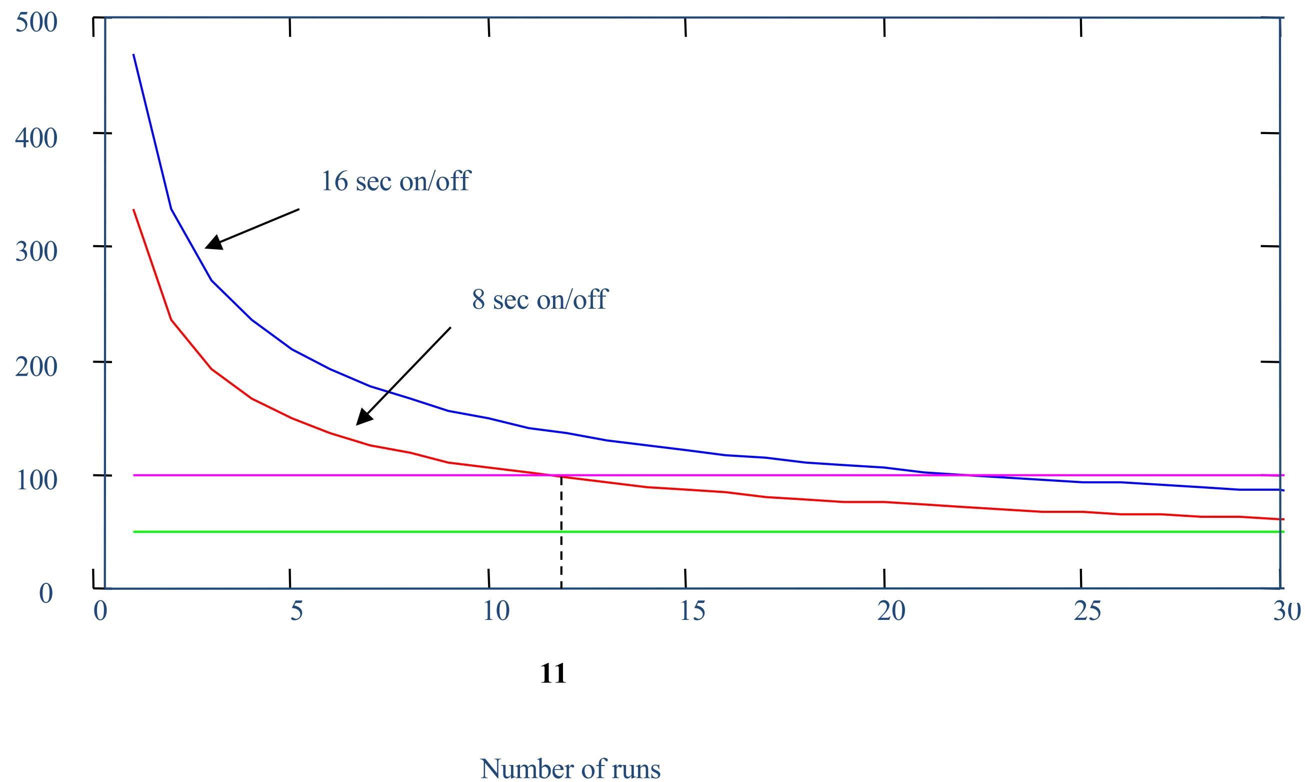
1 run:

1% Noise
4% BOLD
256 time pts /run
1 second TR



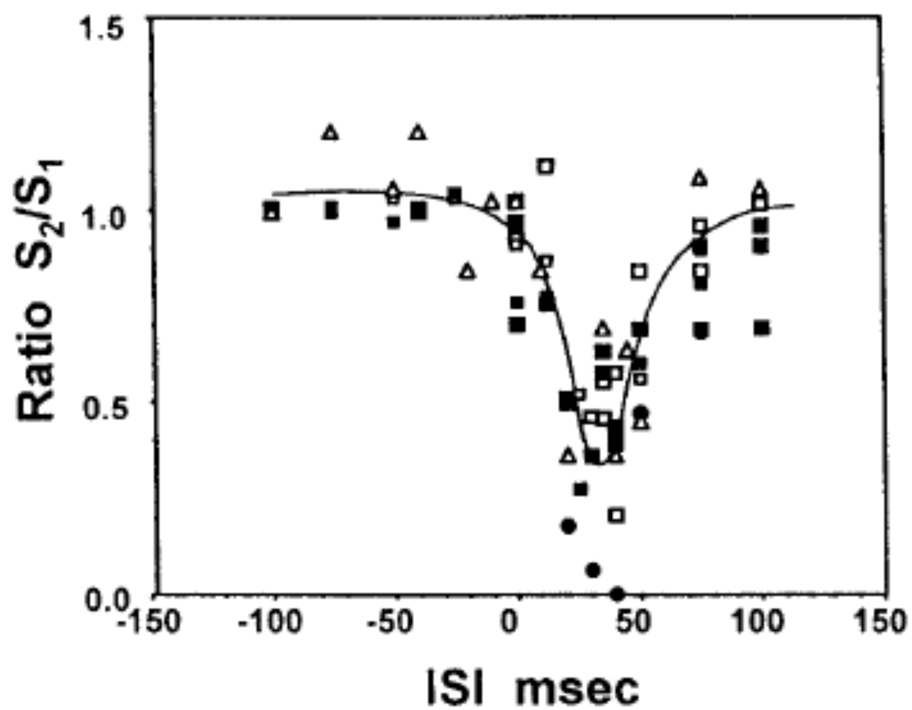


Smallest latency
Variation Detectable
(ms) ($p < 0.001$)



An approach to probe some neural systems interaction by functional MRI at neural time scale down to milliseconds

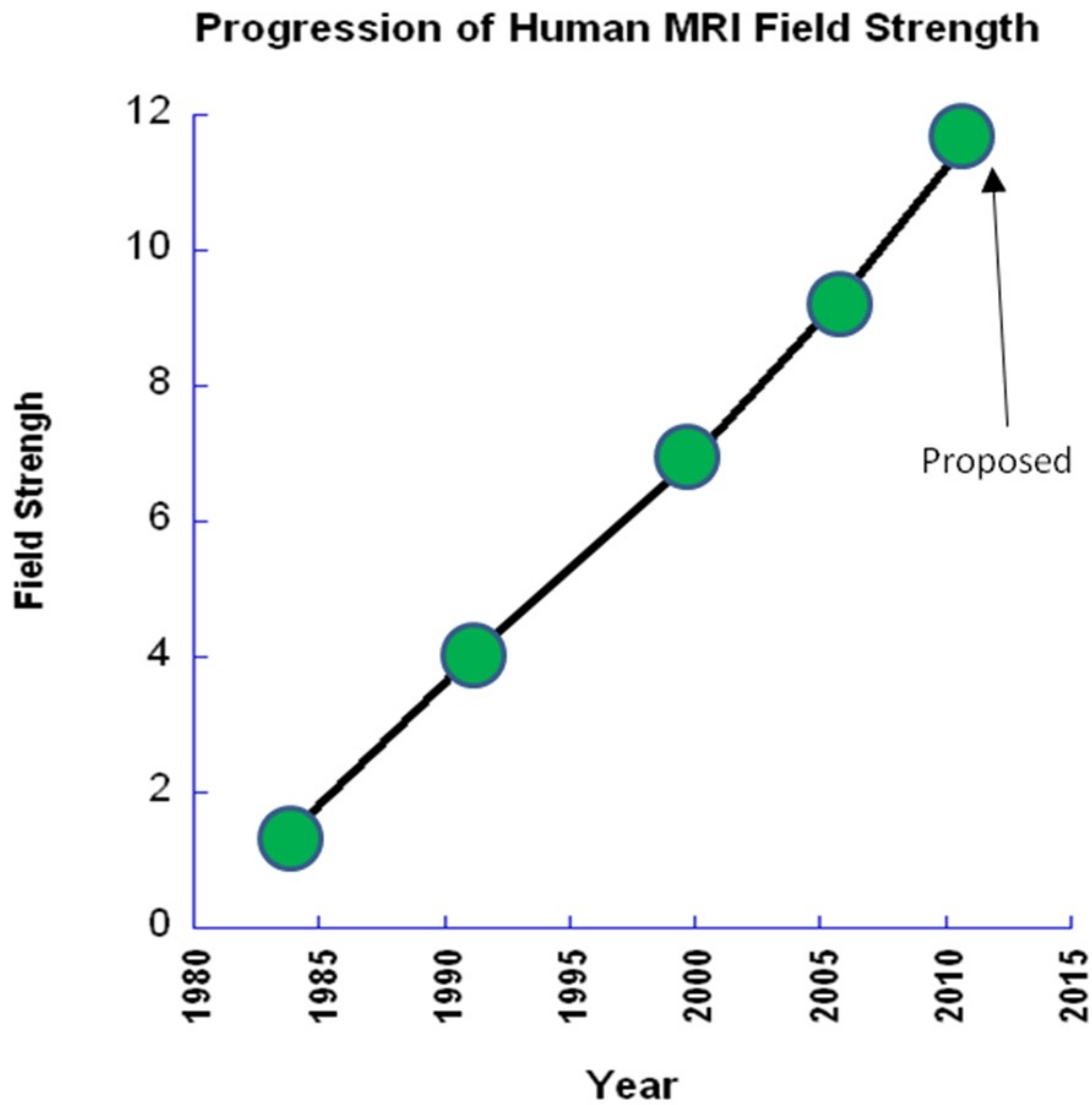
Seiji Ogawa[†‡], Tso-Ming Lee[†], Ray Stepnoski[†], Wei Chen[§], Xiao-Hong Zhu[§], and Kamil Ugurbil[§]



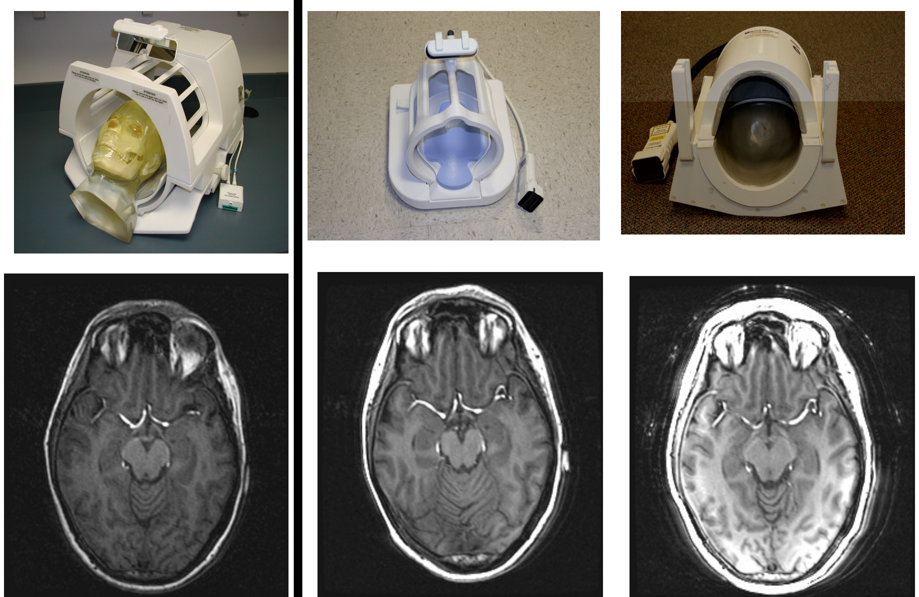
11026–11031 PNAS **September 26, 2000** vol. 97 no. 20

Extracting Information from the fMRI Signal:

- **Spatial Resolution**
- **Temporal Resolution**
- **Sensitivity**

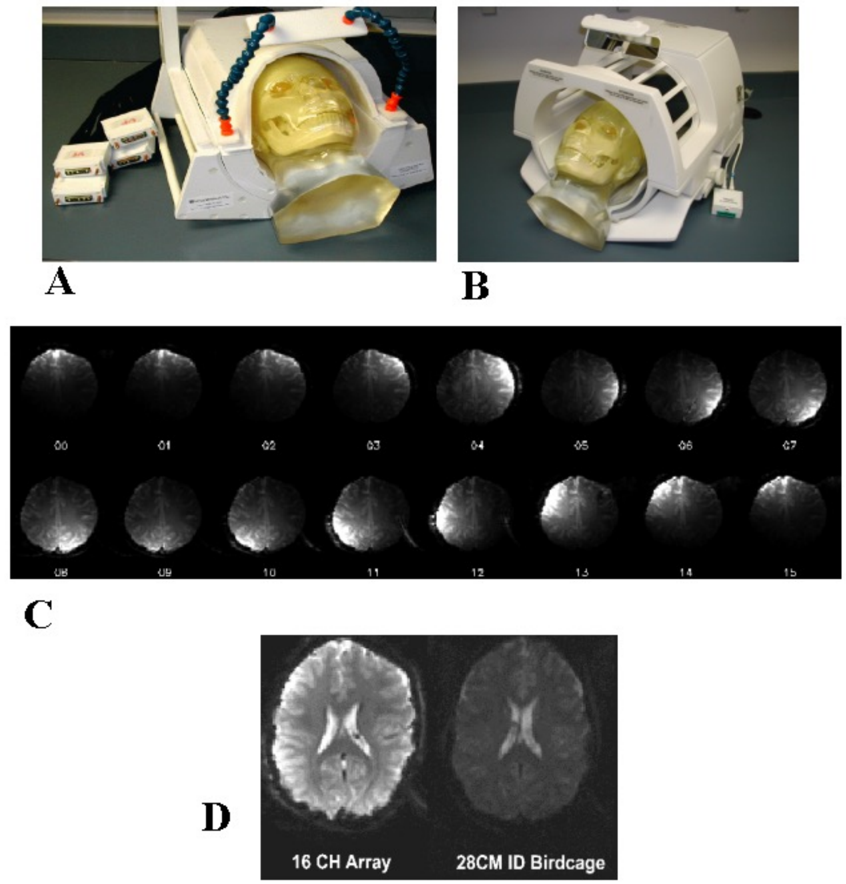

Progression of Human MRI Field Strength
Field Strengh
Year
0
2
4
6
8
10
12
1980
1985
1990
1995
2000
2005
2010
2015
Proposed

8 channel parallel receiver coil



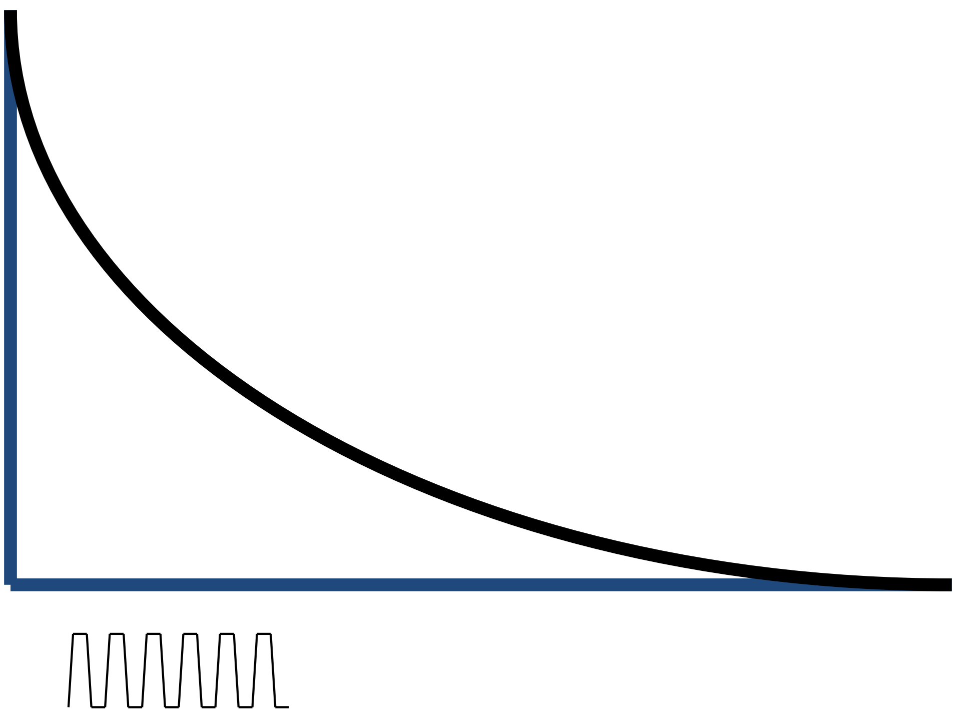
GE birdcage | GE 8 channel coil | Nova 8 channel coil

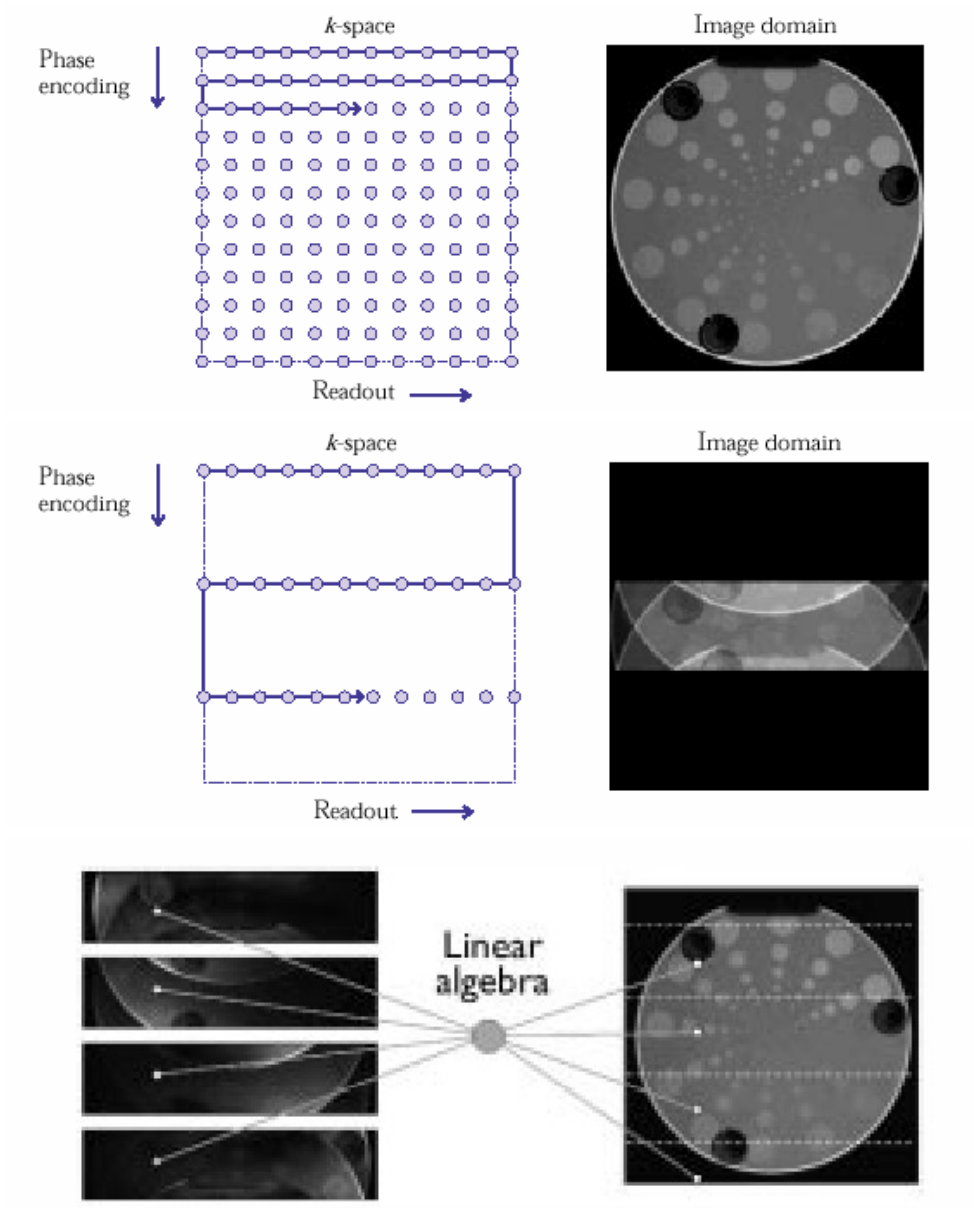
16 channel parallel receiver coil



J. Bodurka, et al, Magnetic Resonance in Medicine 51 (2004) 165-171.

SENSE Imaging

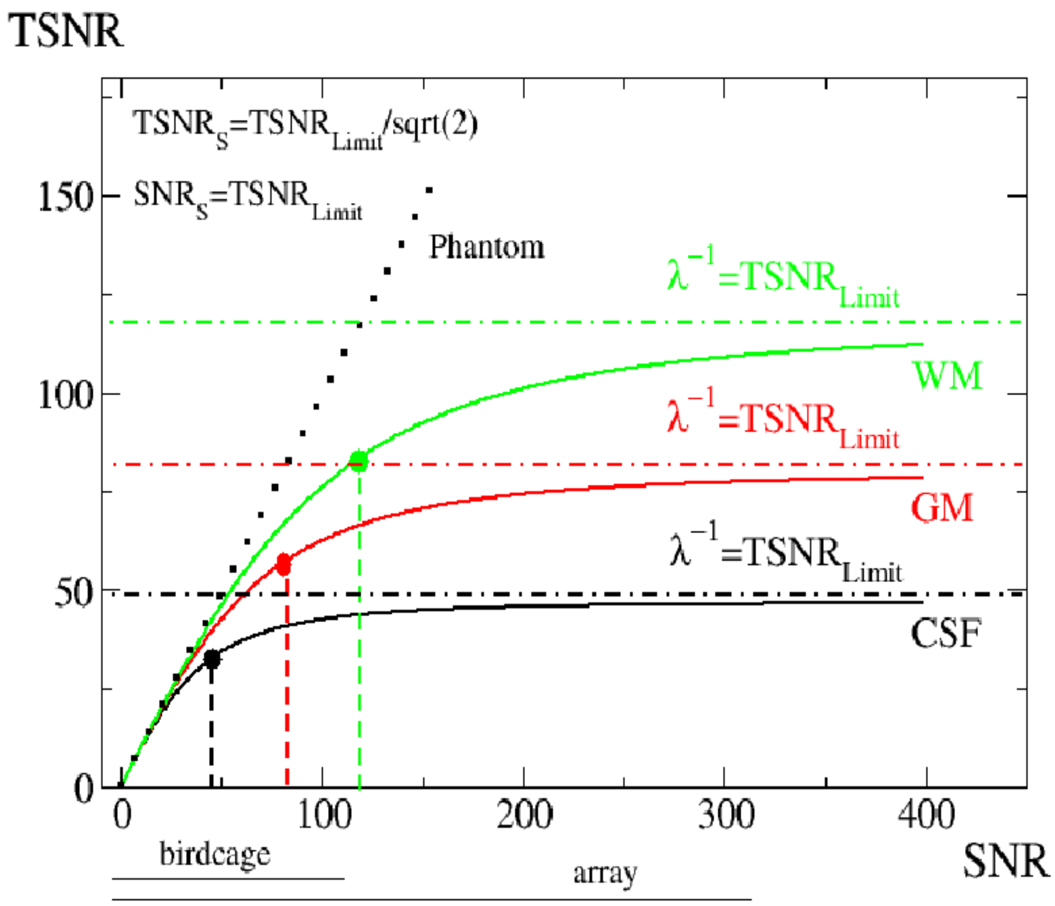




≈ 5 to 30 ms

Pruessmann, et al.

Temporal Signal to Noise Ratio (TSNR) vs. Signal to Noise Ratio (SNR)



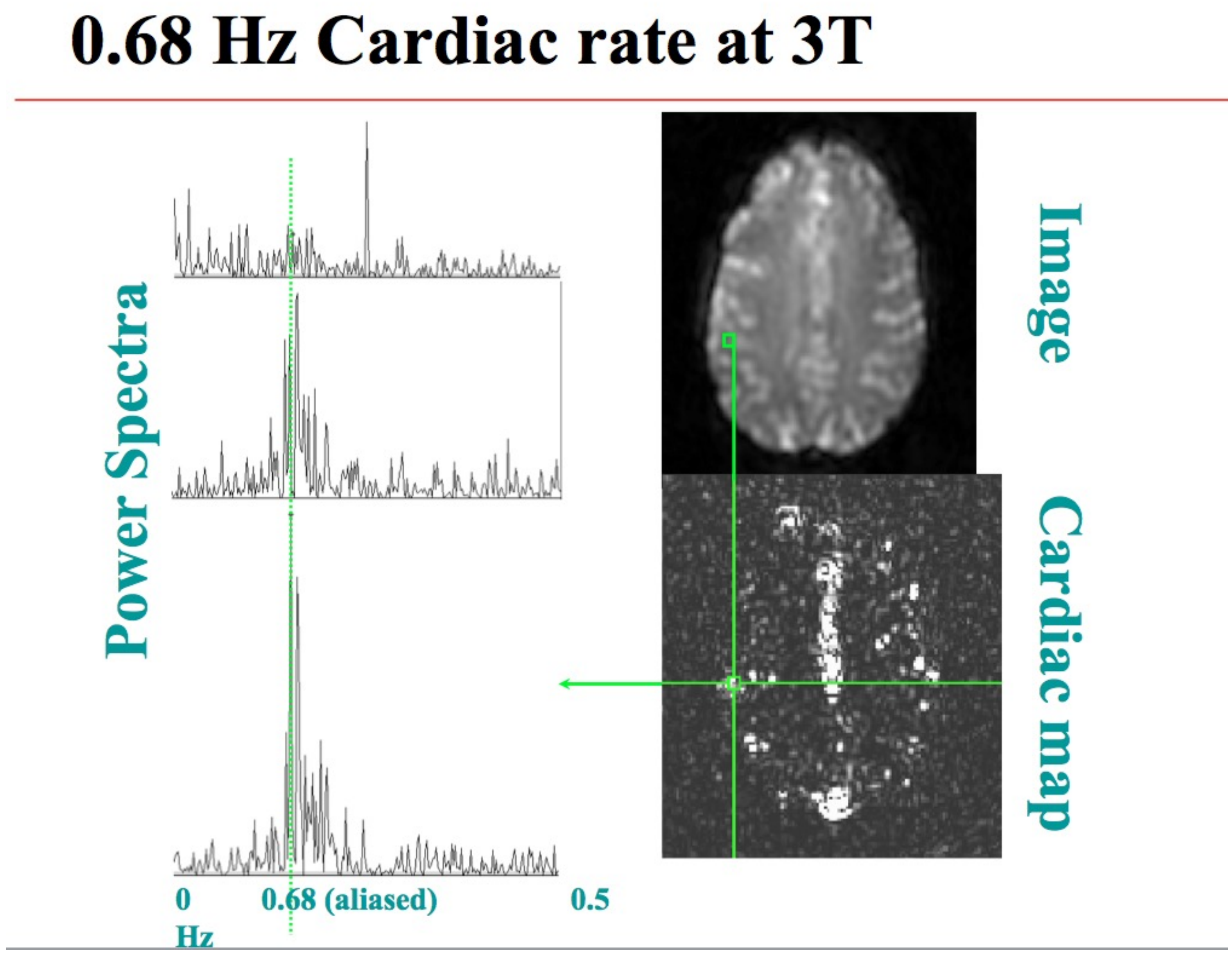
J. Bodurka, F. Ye, N Petridou, K. Murphy, P. A. Bandettini, *NeuroImage,* 34, 542-549 (2007)

Sources of time series fluctuations:

- Blood, brain and CSF pulsation
- Vasomotion
- Breathing cycle (B_0 shifts with lung expansion)
- Bulk motion
- Scanner instabilities
- Changes in blood CO_2 (changes in breathing)
- Spontaneous neuronal activity

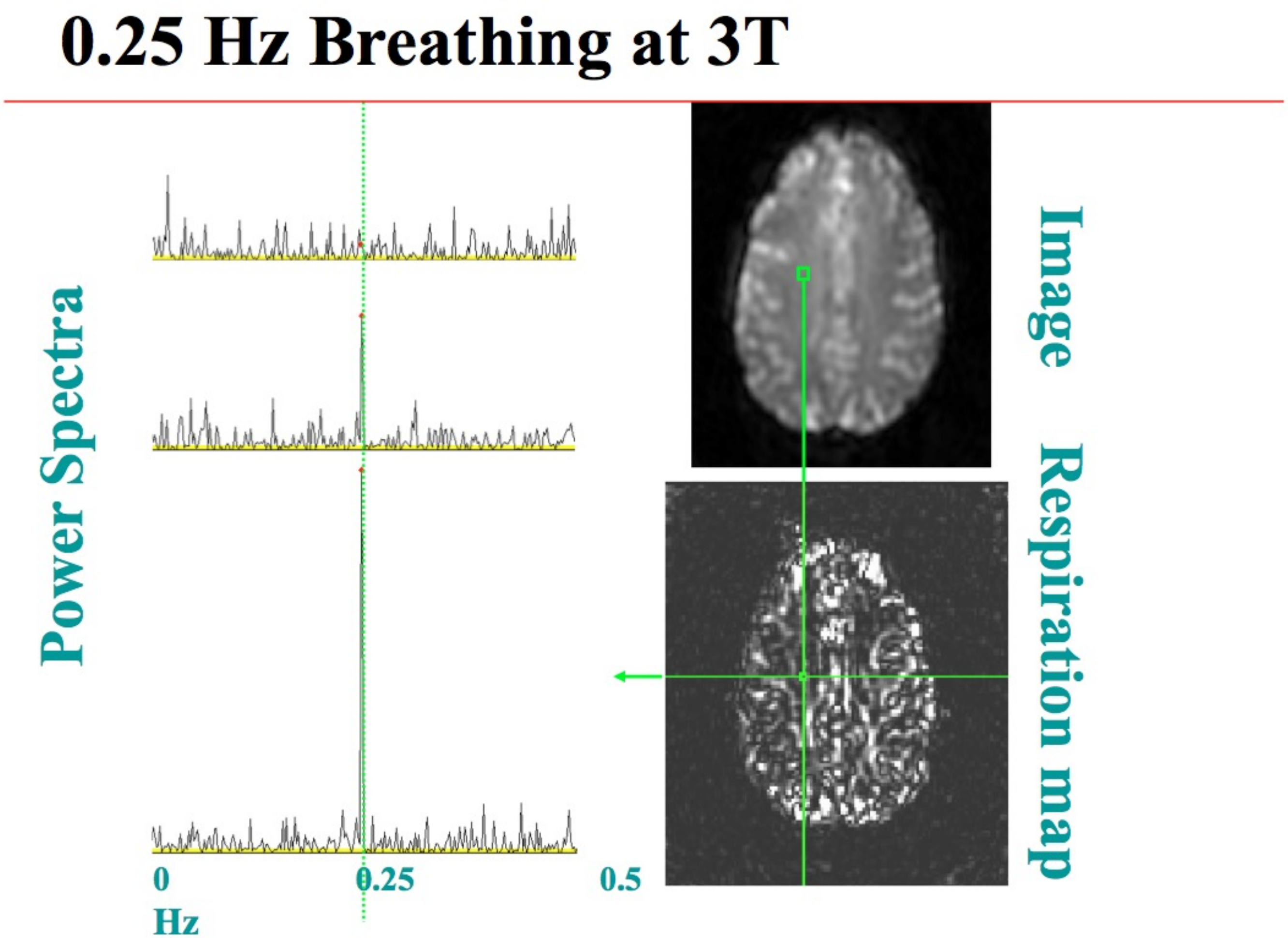
What information can we extract using MRI / fMRI?

Heart Rate

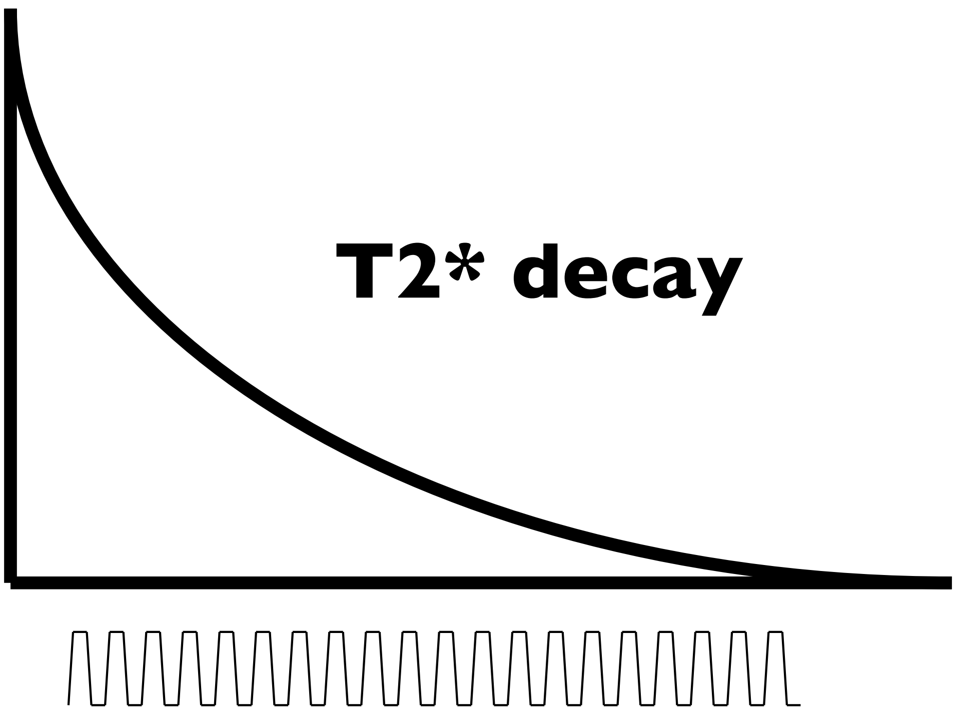


What information can we extract using MRI / fMRI?

Respiration Rate

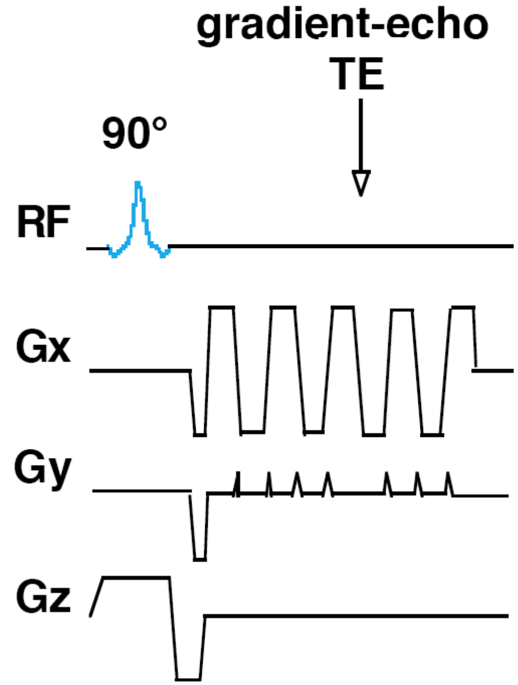


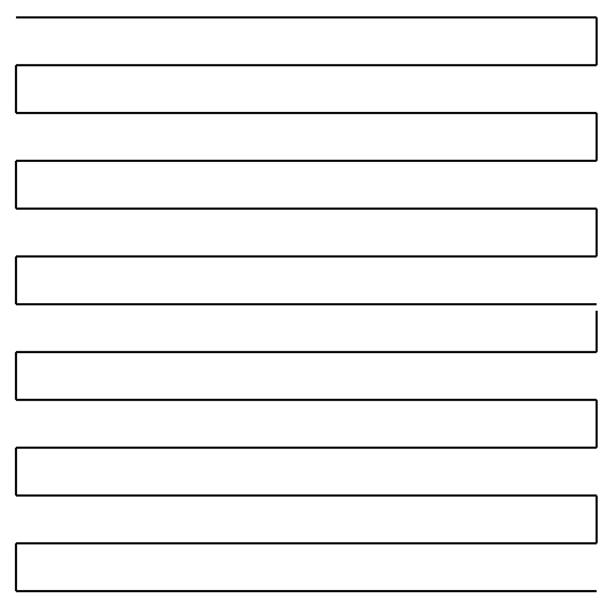
Single Shot Echo Planar Imaging (EPI)

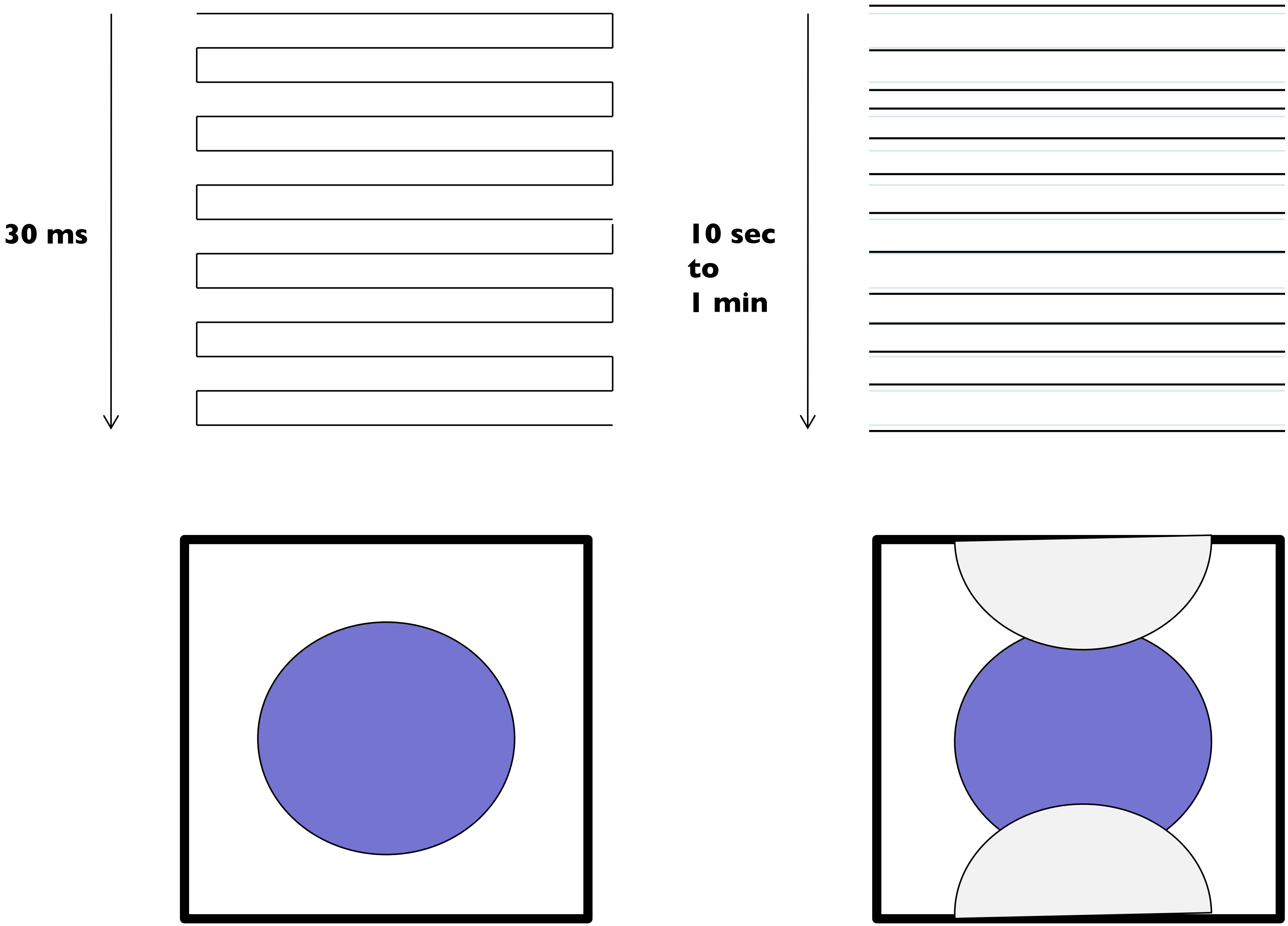


EPI Readout Window

≈ 20 to 40 ms

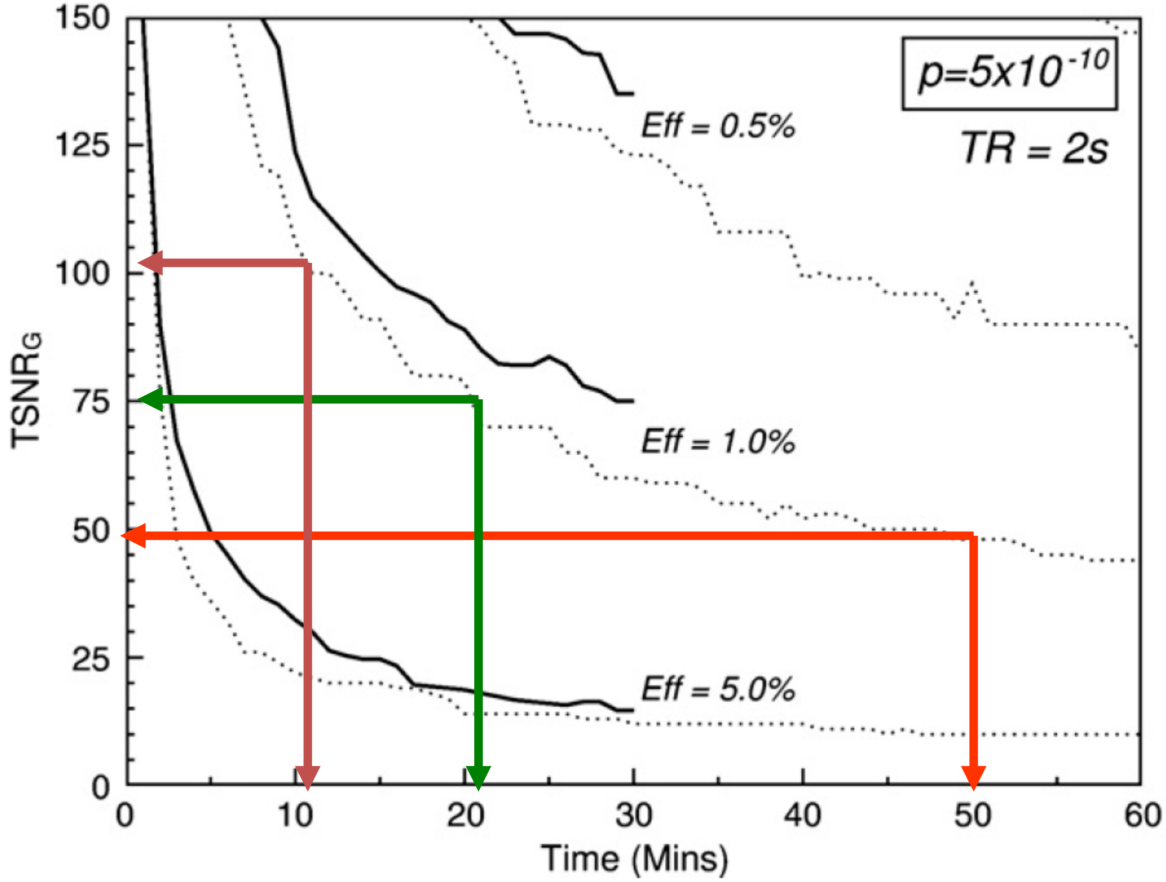






30 ms
10 sec
to
1 min

Sensitivity, Scan Time, and Temporal Signal to Noise

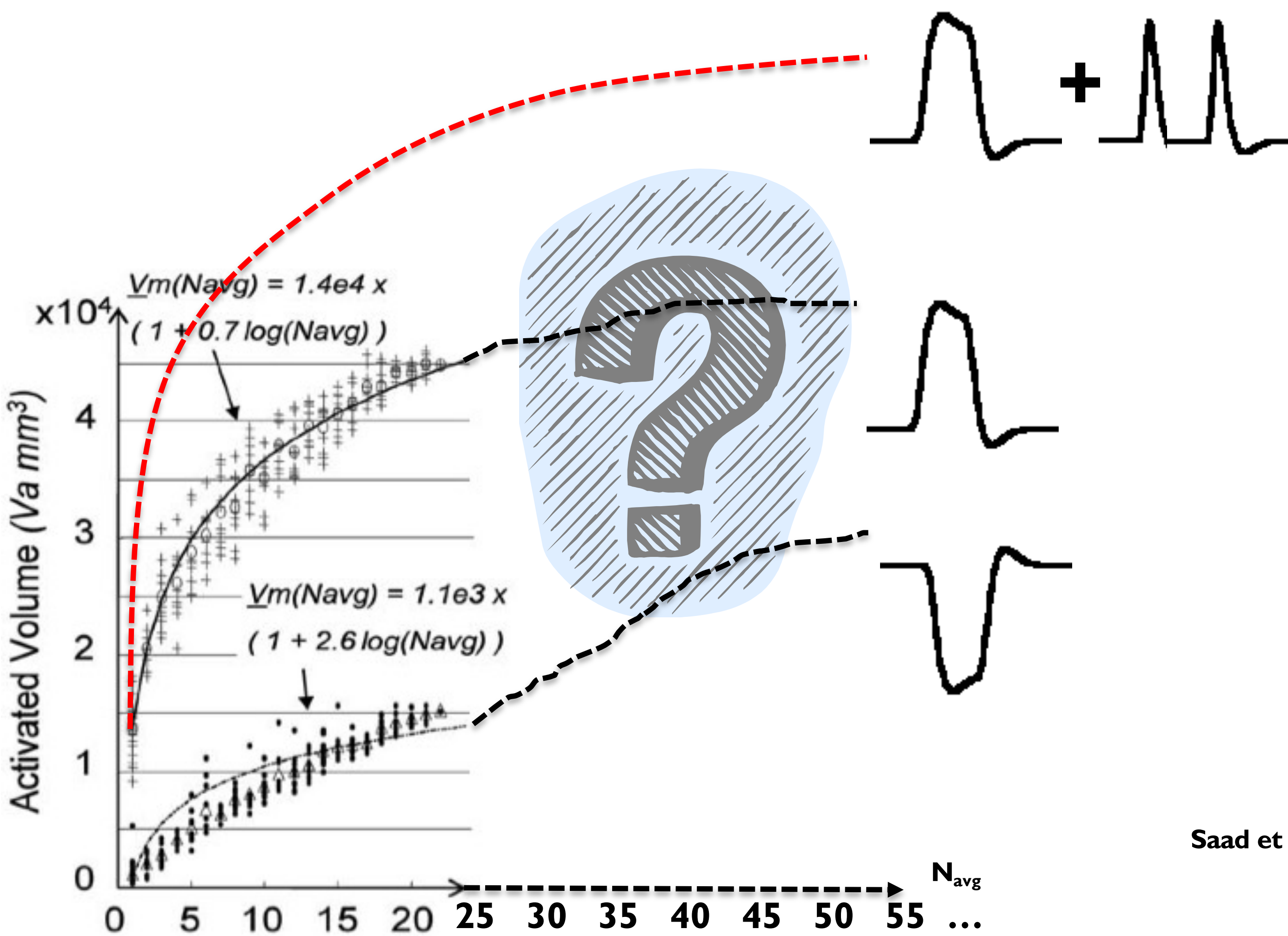


K. Murphy, J. Bodurka, P.A. Bandettini, *NeuroImage*, 34, 565-574 (2007)

IS THE SPARSENESS OF FMRI ACTIVATIONS REAL?

OR

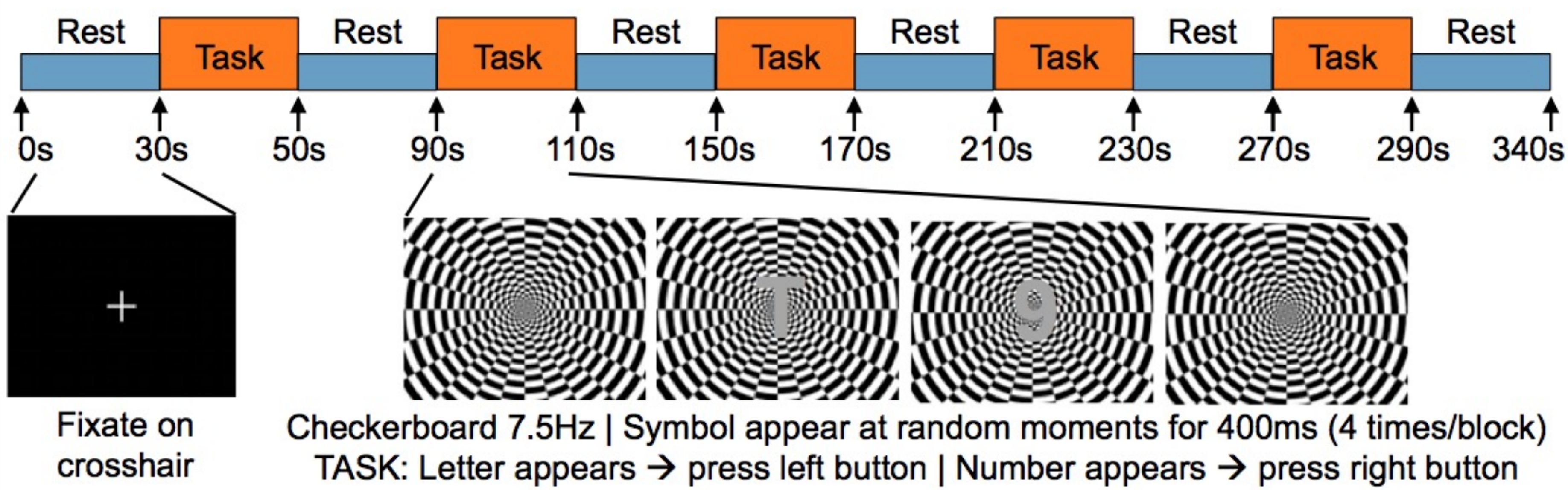
IS IT THE RESULT OF INSUFFICIENT TSNR + OVERLY STRICT RESPO



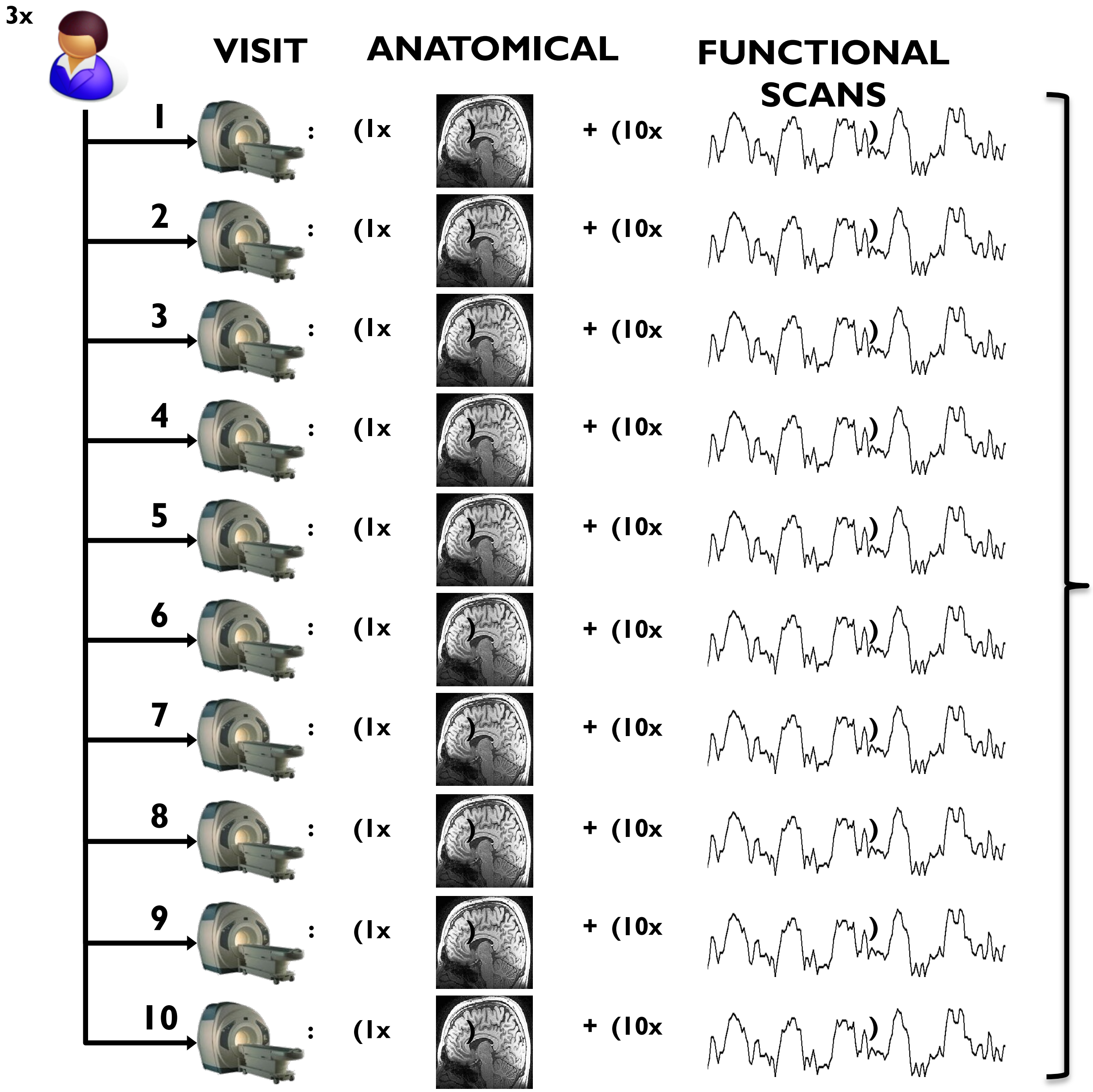
Saad et al

Experimental Methods (I)

- 3 Healthy Volunteers: 1M/2F; Age = 27 ± 2.5
- 3T GE Signa HDx
- Anatomical Scan: MPRAGE | .9x.9x1.2 mm^3 | 192 Slices
- Functional Scans: GRE-EPI
  - TR/TE = 2s/30ms
  - In-Plane Res = 64x64
  - #Slices = 32 Oblique
  - **FOV = 240mm**
  - **Slice Thickness = 3.8 mm**
  - **Flip Angle = 75°**



Experimental Methods (II)



100 FUNCTIONAL RUNS/SUBJECT

||

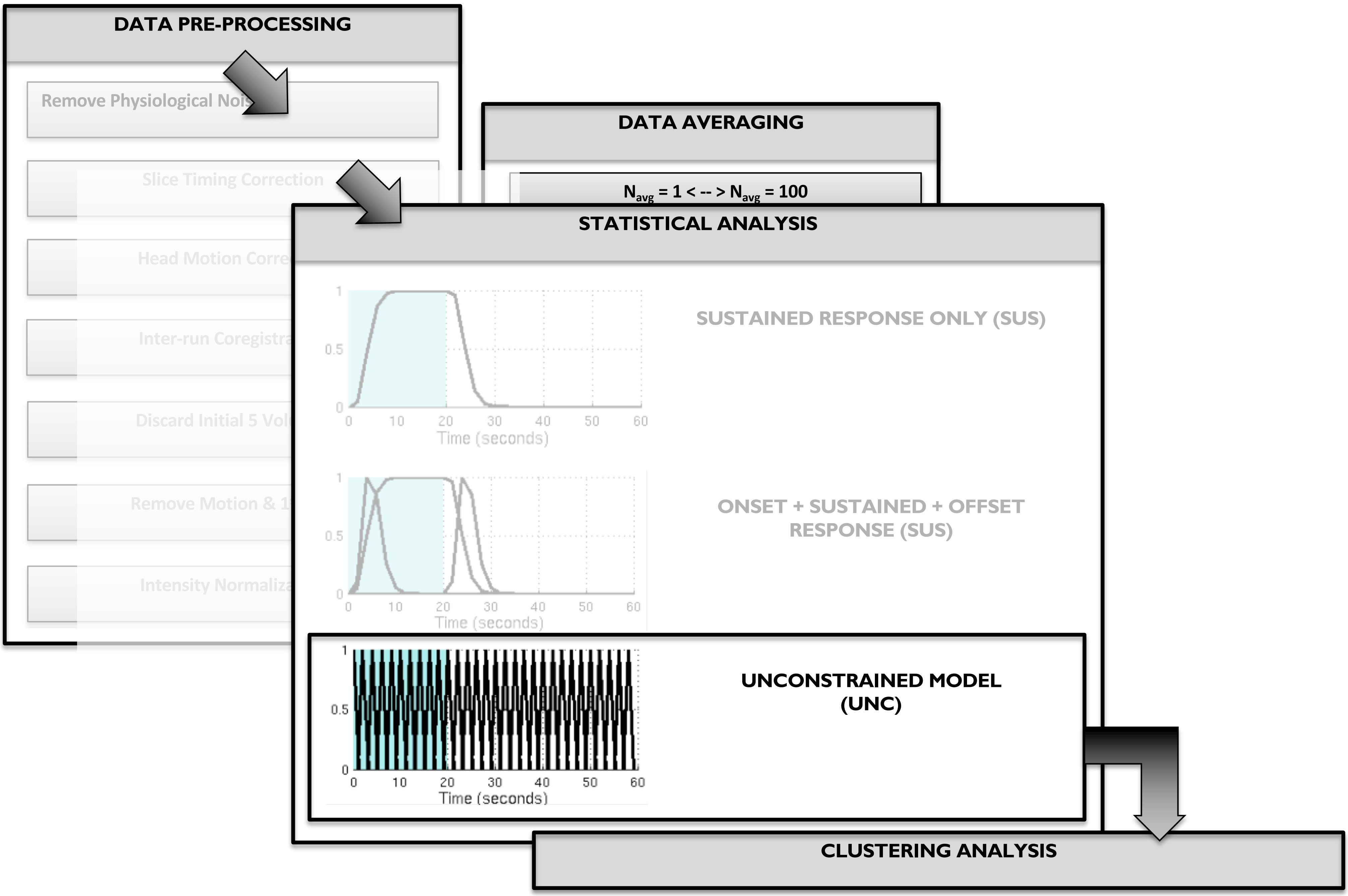
500 TRIALS/SUBJECT

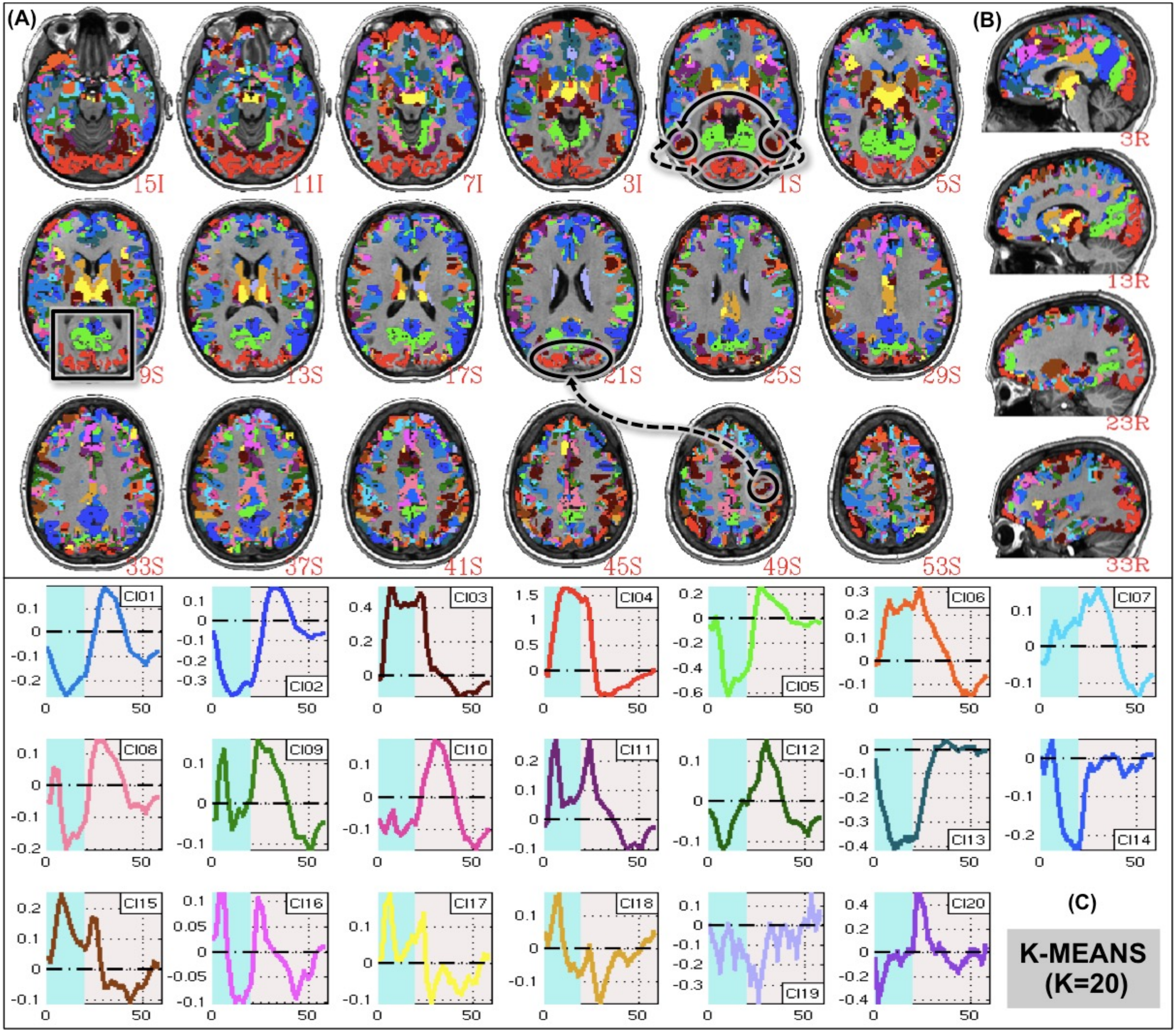
||

9 HOURS OF DATA/SUBJECT

X 100
(QA Axial EPIs)

Data Analysis




(A)
15I
11I
7I
3I
1S
5S
9S
13S
17S
21S
25S
29S
33S
37S
41S
45S
49S
53S
(B)
3R
13R
23R
33R
CI01
CI02
CI03
CI04
CI05
CI06
CI07
CI08
CI09
CI10
CI11
CI12
CI13
CI14
CI15
CI16
CI17
CI18
CI19
CI20
(C)
K-MEANS
(K=20)