Multi-modal imaging: simultaneous EEG-fMRI

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Outline

EEG overview

- § Why simultaneous EEG-fMRI?
- **How? Technical considerations**
- § When? Examples

EEG (electroencephalography)

measure of synchronous activity of population of neurons, primarily reflects postsynaptic potentials.

EEG measures

recording

de the set of the set o

Isolated amplifiers filters A/D converter

conductive media

Eyes closed

1 s

montage

Electrode configuration

- **Referential** $-$ (S_i vs. Ref; S_k vs. Ref)
- **Bipolar** $-$ (S_i vs.. S_k)

International 10-20 System of Electrode Placement

- F Frontal lobe T Temporal lobe
- C Central lobe P Parietal lobe
- O Occipital lobe

"Z" refers to an electrode placed on the mid-line.

- Odd: left
- Even: right

Data processing

- **Time domain**
	- Event Related Potentials (ERPs)

pre-processing:

detrend - filtering

epoch

baseline correction

ocular artifact reduction

(common grounded, artifact rejection)

time-locked averaging

Data processing

- **Filte Frequency domain**
	- § Power at different bands
	- Power spectra density (FFT)
	- Cross-spectra

(correlation among different electrodes)

■ Coherence

(measure of stability of the phase shift between electrodes)

■ Event related desynchronization

Clinical Applications

epilepsy, head trauma, drug overdose, brain infection, sleep disorder, coma, stroke, Alzheimer's disease, brain tumor, multiple sclerosis, surgical monitoring

Cognitive Science

sensory pathways, stimulus encoding, motor process, spatial task, verbal task, mathematics, short term memory, memory encoding, selective attention, task context, general intelligence, dynamic brain theory

PL Nunez, EEG, *Encyclopedia of the Brain*, 2003

Why do we want to measure EEG and fMRI simultaneously?

Neuroimaging

TRENDS in Neurosciences

EEG is the *gold standard* for sleep studies, epilepsy, some cognitive tasks, etc

HOW often measured together?

PUBMED SEARCH

PUBMED search on 8/14/2016, keywords

EEG setup

EEG-fMRI setup

Technical Issues

Electromagnetism 101

Maxwell's Laws.

•A changing magnetic field produces an electric field

BIG PROBLEM

•A changing electric field or current produces a magnetic field.
Luckily, the magnetic field change

Form the EEG does not affect the image quality!

THE not so good NEWS

¡ **MRI is noisy**

Electrical noise \rightarrow MRI and EEG were not meant for each other …

Remember Maxwell's Law?

Simultaneous EEG-fMRI - Technical issues

Simultaneous EEG-fMRI - Technical issues

Approximate values of different signals

- Gradient artifact : ± 10mV
- \blacksquare EEG: \pm 150µV
- BC artifact: ± 200µV
- \blacksquare Blink: \pm 150µV
- ¡ Movement: < 1mV
- \blacksquare ECG: \pm 20µ V
- EMG: ± 50µV
- Helium pump: 40-60Hz and

THE good NEWS

MRI compatible EEG equipment, leads and electrodes

Safe for the scanner Safe for the subject

More on safety later

- Careful setup:
	- Equipment
	- § Cables
	- § Subject head

DATA acquisition

- Sample EEG at 5 kHz (or more)
- Slice TR at a frequency that is not of interest (and a round number)
- Low Pass Filter at 250Hz
- ~0.01 Hz high pass to avoid saturation (use DC only if enough range)
- Volume (or slice) marker
- Resolution: 0.5µV (make sure dynamic range covers the signal, depends on scanner and configuration)
- Clock synchronization

EEG DATA acquisition

- **Make sure amplifiers do not saturate Adjust amplifier resolution**
- ¡ **Keep electrodes' impedance low (unless using high impedance equipment)**
- **Keep cabling safe and fixed**
- **Have a good cardiac signal**
- Adjust MR sequence
- ¡ **Adjust experiment (ISI <> TR)**

Gradient artifact removal

Norm

Scale

- 273

Dr Jen Evans

Ballistocardiogram artifact removal

Matching filter (BV Analyzer) (Allen et al, 2000):

Detect R

Create a template

Subtract (allows for amplitude adjustment)

Single Value Decomposition (Neuroscan)

Run classification Remove components Reconstruct time series

Optimal base set (EEGLAB Niazy, 2005)

PCA to create bases Fitting (adaptive algorithm) Subtraction

Combinations

i.e → Liu, 2012 use ICA, SVD & mutual information (based on Peng, IEEE 2005) software download: http://amri.ninds.nih.gov/cgi-bin/software

Gradient artifact corrected

Cardioballistogram corrected

sequences. EPI 1 and FLASH are not shown for color clarity overlap with the strong overlap with the other low SAR sequences. Timepoint zero corresponds 0.089!C/% (or 2.8!C/(W/kg)) and 0.224!C/% (or \blacksquare in the head coil (at class coil \blacksquare coil (at T8), respectively. Please note that an SAR value of 100% corresponds to the maximum allowed \mathbb{C}^{∞} \mathbf{v} and body SAR, respectively. electrode through the RF transmission of the RF transmission of the RF transmission of the RF transmission of enhancing induction effects (9). These findings confirm the general warning given in the literature that scanner calculated SAR values can only be used as a 2.0 W/kg in parentheses. Data refer to subject m85 when where \mathbf{F} is an and fitted data (x) (–) approaching the equilibrium temperature are displayed, showing a clear increase of the equilibrium temperature with

 $\mathcal{F}_{\mathcal{A}}$, the T8 electrode as a function $\mathcal{F}_{\mathcal{A}}$ electrode as a function $\mathcal{F}_{\mathcal{A}}$

 $\mathcal{A} = \mathcal{A} \cup \mathcal{A}$ shows the heating of the $\mathcal{A} = \mathcal{A} \cup \mathcal{A}$

clarity, as the associated behind be a strong overlap with the associated with the strong overlap with the str

shows typical exponential temperature changes during MR \overline{a}

 $\mathcal{O}(10^{10})$ and $\mathcal{O}(10^{10})$ for the head coil (at class $\mathcal{O}(10^{10})$ for the head coil (at class $\mathcal{O}(10^{10})$

ably due to a different analog due to a different analog α

11.2!C/(W/kg)) for the head coil (at clavicle) and body

Figure 5. Relation between scanner-calculated average figure of relation between scanner calculated average head (a) and body (b) SAR and fitted equilibrium temperatures for subject m90, clavicle electrode (a) and subject m85, **Figure 5.** Relation between scanner-calculated average T8 electrode (b) when using the head (a) and body (b) coil, respectively. The least-squares inical in (son clear linear increase of the equilibrium temperature with average head (a) and body (b) SAR. respectively. The least-squares linear fit (solid line) shows a

Simultanoous Electroensephalogra Simultaneous Electroencephalography-Functional MRI at 3 T: An Analysis of Safety Risks Imposed by Performing Anatomical Reference Scans With the FEC Equipment in E **Scans With the EEG Equipment in Place**

sible temperature for equipment in continuous con-

The in vivo study was repeated with the same subjects using the inbuilt body coil for RF transmission and signal reception in order to investigate to what degree the choice of the RF transmit coil influences heating Temperature measurements were performed at the same electrode positions as in the head coil study with the following exceptions: since the risk of RF heating has been reported to be higher for body coil transmission due to the larger spatial extension of the exciting RF field (18), the electrode at the clavicle was not applied for the subject where a temperature increase of more than 4!C had been measured at this site in the previous experiment based on head coil transmission. Furthermore, the T8 electrode (position 8, see above) was used in all subjects.

tact with the skin is 41!C (10). Body Coil Transmission

Data Analysis

Ulrike Nöth, Laufs, Stoermer, and Deichmann JMRI 2012

although there was no major difference in SAR values. **SAR**: Specific Absorption Rate (or the energy deposited in the body by the radio frequency transmission)

SAFETY considerations

Sequences

§ EPIs (in most cases ok to run an MPRAGE for localization) be aware of high res short TR EPIs (**pay attention to SAR**) Special sequences require special safety testing

Set up

- Cables straight and in the center. Avoid loops
- Equipment as far back from iso-center as possible (far front for EMG) All scanners are **not** equal; gradients and coils affect electrodes' temperature

Be aware different body shapes and weight load coil differently

Interim Summary

- ¡ EEG measurements have:
	- § Good temporal resolution
	- Poor spatial resolution

(when measure non invasively)

- Electrical and hemodynamic responses are related
- **Simultaneous EEG-fMRI requires special equipment**
- ¡ **SAFETY PROCEDURES ARE KEY**
- Dimensionality reduction is needed for data integration

When do we want to measure EEG and fMRI simultaneously?

When is it important to measure simultaneously?

¡ **State dependent analysis**

- § Alertness
- State vs Trait
- Understanding origin of signals (BOLD; EEG)

¡ **Physiological markers defined by EEG**

- Seizures
- § Sleep stages

Type of studies

■ Correlations of EEG and fMRI

- § In time domain
- **In frequency domain**
- ¡ Multivariate methods
	- \blacksquare ICA
- **Informing one with the other**
	- Sorting data and perform analysis in one modality
- Mix analysis

EEG parameter as regressor

BOLD-EEG band-power correlations

$$
\frac{1}{2}
$$

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∕µ

Goldman et al. 2002 Simultaneous **EEG** and **fMRI** [of the alpha rhythm](http://www.ncbi.nlm.nih.gov/pubmed/12499854).

Correlation between Amplitude of BOLD fluctuations and alertness Index derived from EEG

Horovitz et al HBM, 2008

How to link time and space information? Parametric studies and correlational analysis

Correlation maps between fMRI signal change and P300 amplitude. Composite of 7 subjects. Horovitz et al MRI, 2002

OLD DAYS: SAME SUBJECTS, EEG AND FMRI ON SEPARATE SESSONS

Single-Trial Analysis of Oddball Event-Related Potentials in Simultaneous EEG-fMRI

a) Outside MR scanner

Benar et al. Human Brain Mapping 28:602–613 (2007)

Time (ms)

Assessing the spatiotemporal evolution of neuronal activation with singletrial event-related potentials and functional MRI

Tom Eichele PNAS 2005 vol. 102 no. 49

EEG to define states

Use EEG to sort fMRI data

Changes in the level of consciousness

Decoupling of the brain's default mode network during deep sleep

11276-11201 | FMAS | Arty 7, 2009 | vol. 106 | no. 27

Silvina G. Horovitz^{a, b, 1}, Allen R. Braun^c, Walter S. Carr^d, Dante Picchioni^e, Thomas J. Balkin^e, Masaki Fukunaga^b, and Jeff H. Duynb

Do changes in connectivity over time have a physiological origin?

EEG-vigilance and BOLD effect during simultaneous EEG/fMRI measurement

S. Olbrich et al. / NeuroImage 45 (2009) 319–

neg. BOLD

Spatiotemporal dynamics of the brain at rest exploring EEG microstates as electrophysiological signatures of BOLD resting

state networks.

EEG to understand BOLD signal

Correlations of simultaneously acquired SSVEPs with BOLD fMRI response

The graphs to the left show the group average MR (blue) and EEG (green) timeseries signals for each task. Excellent agreement is found between modalities. However, the amplitude of the last flanking blocks seems decreased in the SSVEP signal.

J.W Evans et al OHBM 2015

EEG & fMRI to study disease

intracranial recordings - fMRI

D.W. Camsichael et al. / NeuroImage 63 (2012) 301-309

Rg. 3. Simultareously acquired MRI and IcEEG data quality; visual comparison. The same three orthogonal views are displayed of MRI structural (top left) and fMRI data (bottom middle left) in patient #1. The crosshalts indicate the displayed slices through the volume and are centred near the implanted electrode contacts. These are displayed overlaid on the reconstructed brain surface from the T1-weighted volumetric MRL The fMRI datavolume (bottom left) is also surface reconstructed to visualise image artefact levels. As in 'a' for patient #2. A segment of MRI scanner artefact corrected icEEG for patient #1. As in 'c' for patient #2. The results of the left vs. right hand finger tap task in patient #1 with the fMRI response visible immediately beneath the electrode contacts on the contical surface.

305

A study of the electro-haemodynamic coupling using simultaneously acquired intracranial EEG and fMRI data in humans

T. Murta, L. Hu, T. Tierney, U.J. Chaudhary, M.C. Walker, D.W. Carmichael, P. Figueiredo, L. Lemieux NEUROIMAGE, 2016 (accepted Aug 3)

Highlights

- First study of EEG morphology using simultaneous intracranial EEG-fMRI in humans.
- **The duration of sharp waves is** significantly correlated with the BOLD signal amplitude.
- **BOLD** amplitude reflects more field potential duration than neuronal synchrony.
- Sharp wave duration should be included in BOLD models of epileptic discharges.

Use EEG to understand **fMRI neurofeedback**

Zotev et al. NeuroImage: Clinical 11 (2016) 224–238

Automatic EEG-assisted retrospective motion correction for fMRI (aE-REMCOR).

Chung-Ki Wong, Vadim Zotev, Masaya Misaki, Raquel Phillips, Qingfei Luo, Jerzy Bodurka. Neuroimage 2016

Highlights

- **EXEMEDA is capable to automatically** detect rapid head and cardioballistic motions.
- **EXECT:** Motion effects can be corrected by aE-REMCOR on slice-by-slice basis in fMRI data.
- **E** improve accuracy of the rs-fMRI connectivity analysis.
- **E** aE-REMCOR provides incentive for conducting simultaneous EEG & fMRI.

Selection algorithm for motion ICs

Resting state functional connectivity of default mode network

For the resting scan shown in Fig. 6

Resting state connectivity of the default mode network (DMN).

Top: Individual subject. (a)–(b): Correlation map without and with aE-REMCOR for the scan with significant rapid head movements (c) difference.

(g-h-i) Group results

Simultaneous EEG-fMRI summary

- § Safety first!
- Quality control at experiment setup & data collection Equipment setup Pulse sequence Task design
- § EEG pre-processing Gradient & ballistocardiogram artifacts

■ Data integration

Dimensionality reduction Spatial correlations Regressions Sorting data based on state

§ Some applications

Understanding BOLD signal Understanding Disease Origins of EEG signals State dependent studies