

# Nuts and Bolts of MRI and fMRI

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National Institute  
of Mental Health



# Outline

- System overview
- Components of the acronym
  - What's the Magnet for?
  - Where does Resonance come in?
  - How is Imaging accomplished?
- Some basic types of MR contrast
- Re-cap of System overview

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# System overview

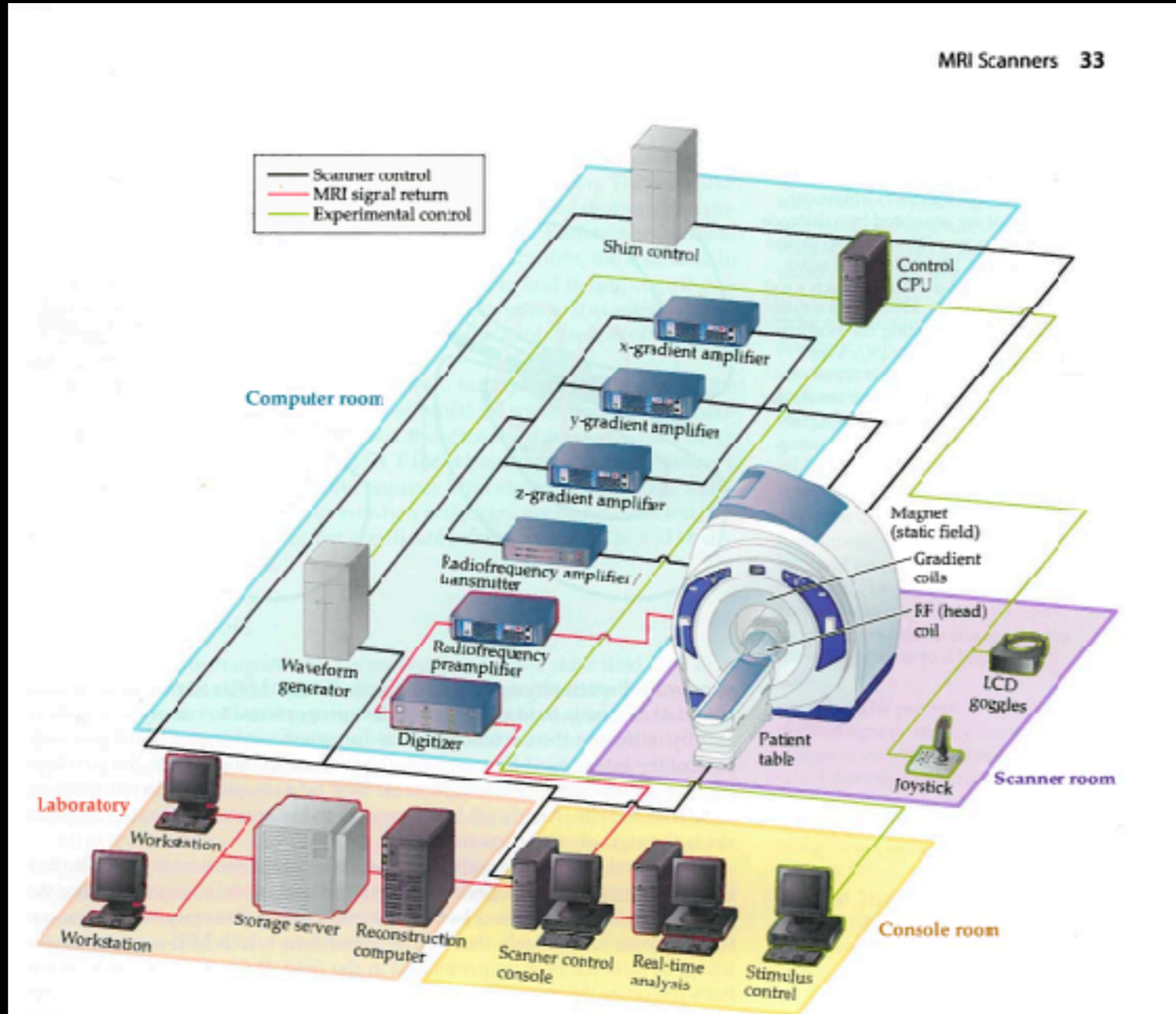


Figure 2.7 Schematic organization of the fMRI scanner and computer control systems. Two systems are important for fMRI studies. The first is the hardware used for image acquisition. In addition to the scanner itself, this hardware consists of a series of amplifiers and transmitters responsible for creating the gradients and pulse sequences (shown in black), and recorders of the MR signal from the head coil (shown in red). The second system is responsible for controlling the experiment in

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# Magnets, magnets, everywhere

- Certain nuclei (odd number of protons and/or neutrons) have magnetic properties (i.e. magnetic moment - 1952 Nobel Prize in Physics, to Bloch and Purcell).
- Include  $^{13}\text{C}$ ,  $^{23}\text{Na}$ ,  $^{31}\text{P}$ ,  $^{129}\text{Xe}$ , and ...

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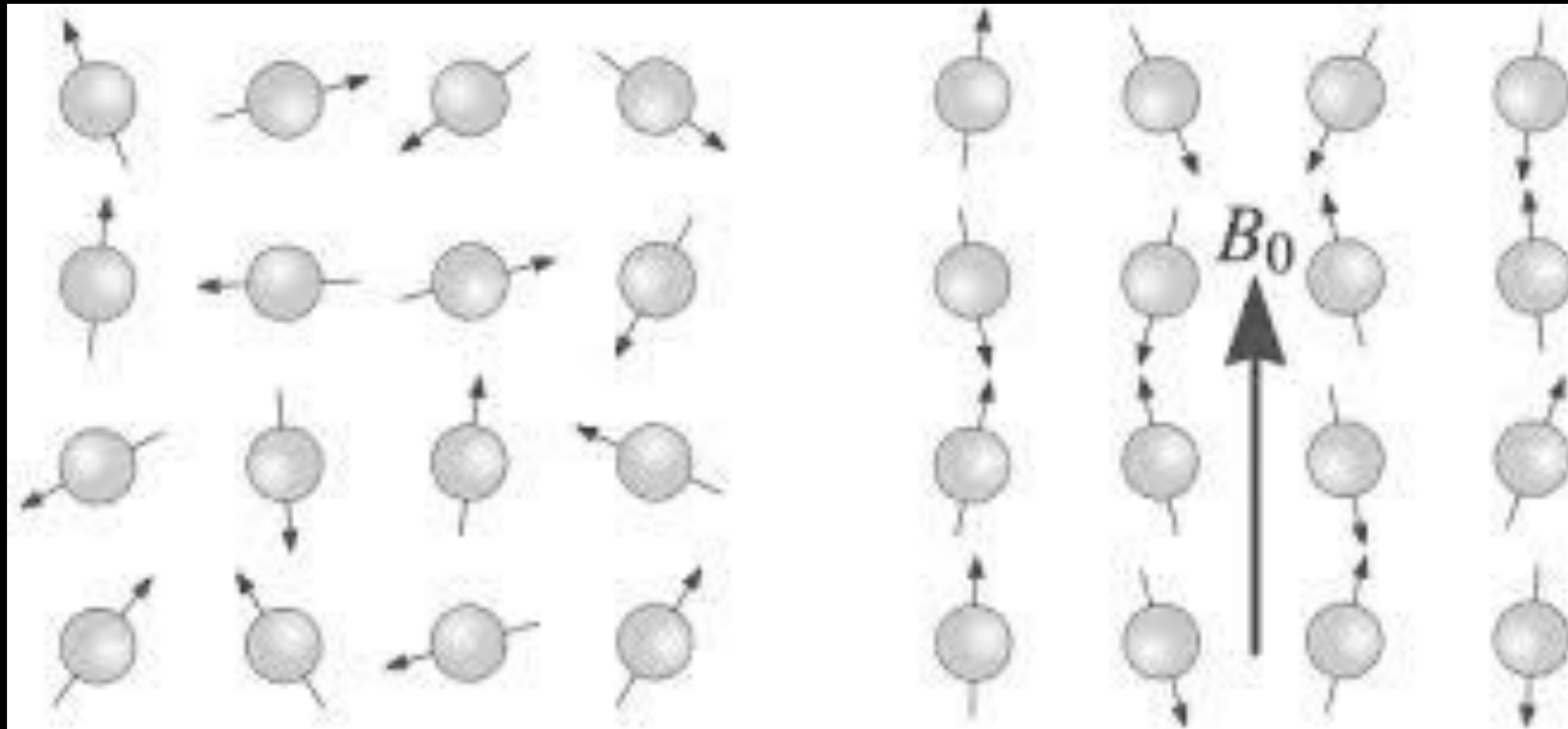
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- $^1\text{H}$  !

# Magnets, magnets, everywhere

- Protons randomly aligned naturally
- Magnetic poles line up when exposed to strong magnets

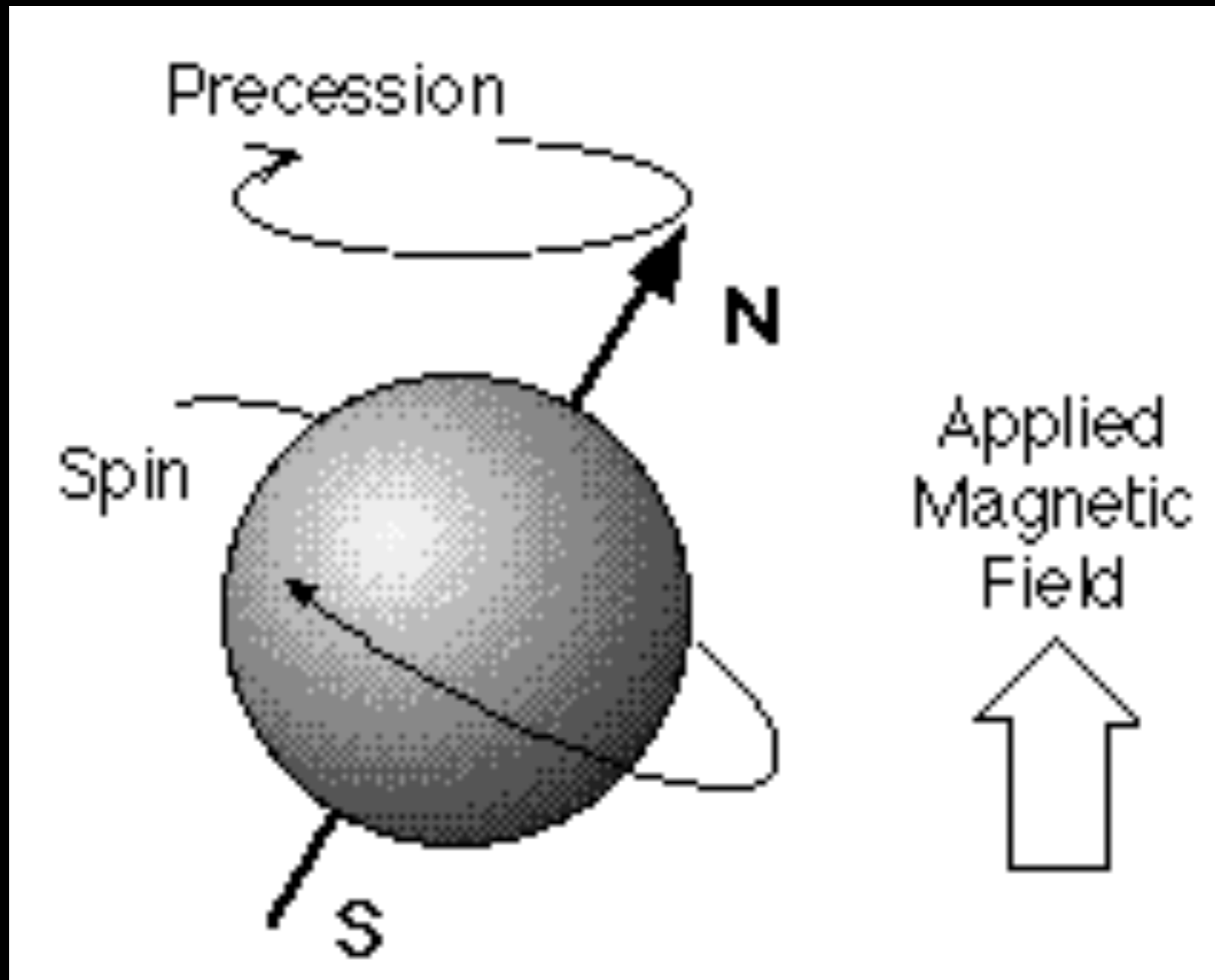


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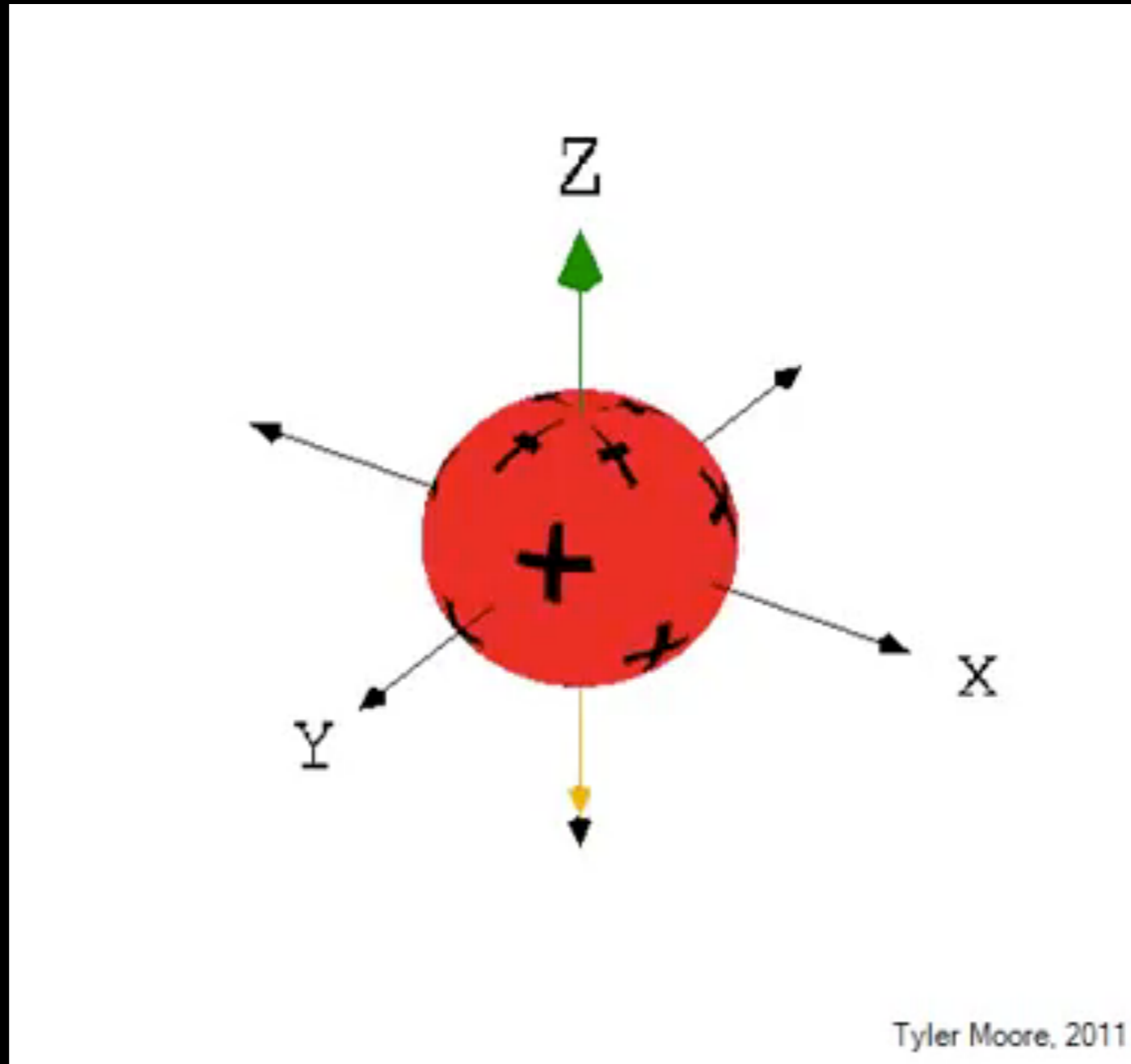
[http://wikidoc.org/index.php/Basic\\_MRI\\_Physics](http://wikidoc.org/index.php/Basic_MRI_Physics)

# Magnets, magnets, everywhere



<http://ccn.ucla.edu/BMCweb/SharedCode/TINS/FMRI-TINS.html>

# Magnets, magnets, everywhere



<https://www.youtube.com/playlist?list=PLAE12114468910462>

# Magnets, magnets, everywhere

$$\omega_0 = \gamma B_0$$

# $B_0$ Nuts and Bolts

- Stronger main field (larger  $B_0$ ) - higher frequency ( $\omega_0$ )
- More signal, i.e. larger net Magnetization (e.g. can be used to acquire higher resolution images)
- Different tissue contrast with stronger main field

# $B_0$ Nuts and Bolts

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- Different tissue contrast with stronger main field

However ...

- Higher frequency RF (larger  $\omega_0$ ) gives rise to more SAR issues
- More issues with keeping  $B_0$  uniform
- Might not be appropriate for some applications

# Outline

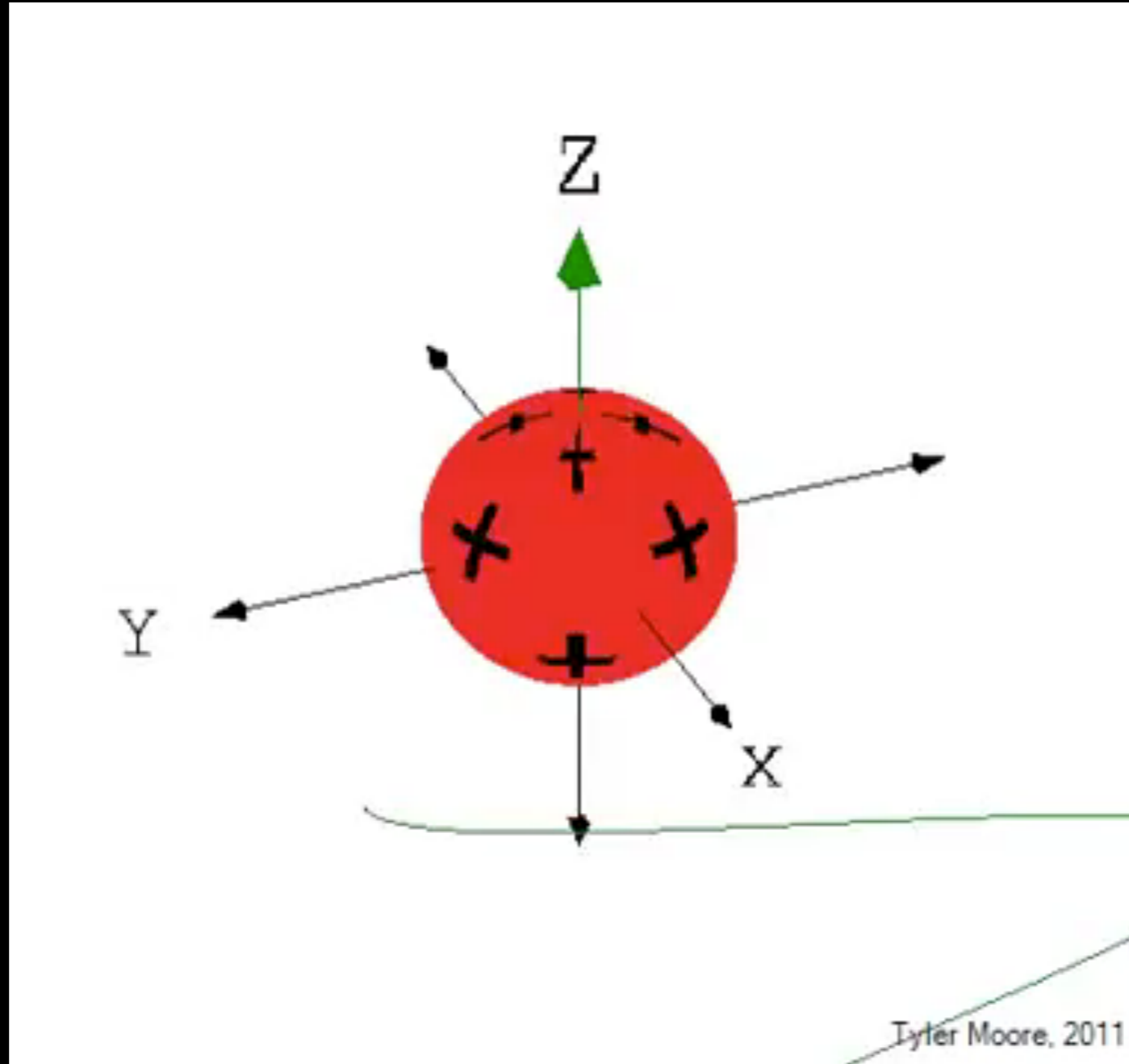
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# Resonance

- Protons aligned with main magnetic field ( $B_0$ )  
**are not** visible / detectable in MR imaging
- “Flip” / excite into visibility by applying energy  
at the same frequency as precession ...
- == Resonance !



# Resonance



<https://www.youtube.com/playlist?list=PLAE12114468910462>

# Resonance

- Perpendicular protons (partially or completely) **are** visible in typical MR experiment.
- RF must be “on resonance” for efficient excitation
- Off resonance - power deposited in sample / no signal → high SAR.
- Uniform  $B_0$  → uniform signal. Need additional info to localize signal to generate image.

# RF Nuts and Bolts

- “Flip” angle  $\approx$  degree of tip - a type of contrast
- High RF power for short time vs. low power for longer time. Same flip angle - but can give different contrast
- Types of RF pulse and timing give rise to lots of different MR tissue contrast ( $T_2$ , DTI, ASL)
- Sometimes, off-resonance excitation can be used to create contrast (MT) - high power and higher SAR experiment.
- Multi-band EPI is a higher SAR experiment than single-band

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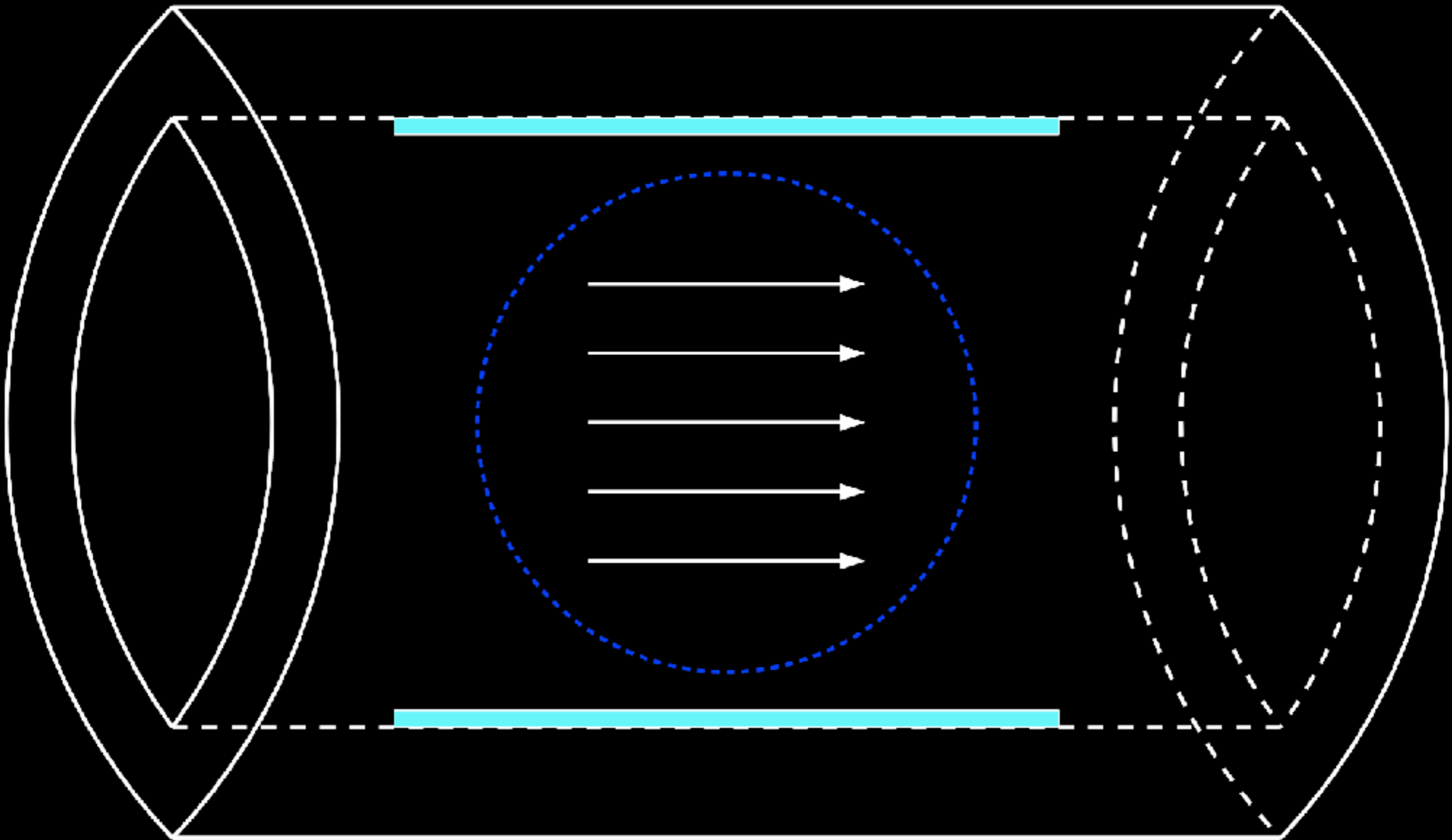
# Imaging

- Uniform  $B_0$   $\rightarrow$  uniform signal - cannot localize ...  
so how to image?

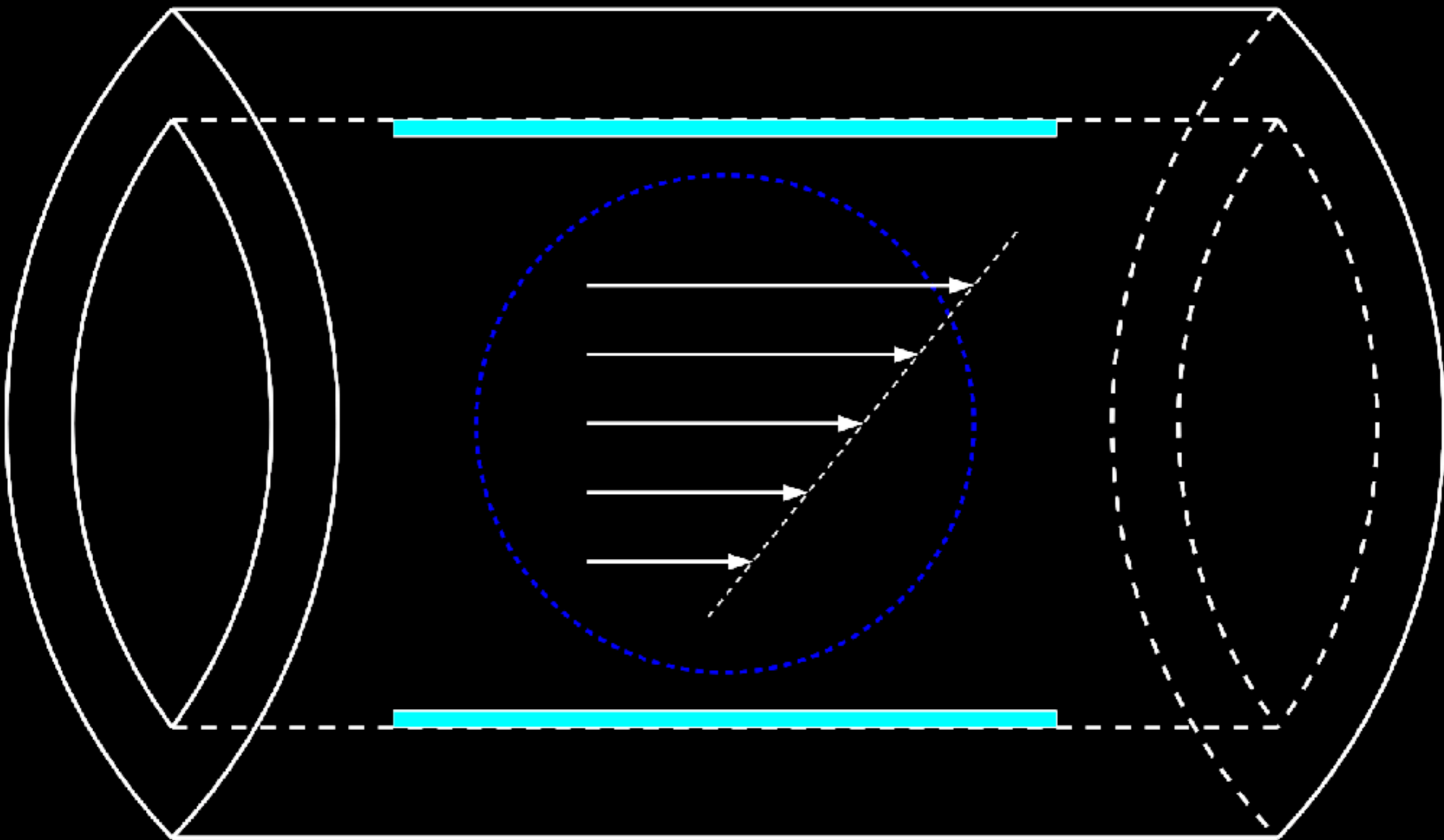
# Imaging

- Uniform  $B_0$   $\rightarrow$  uniform signal - cannot localize ...  
so how to image?
- Apply controlled distortion to  $B_0$

# Imaging



# Imaging





# Imaging

- Uniform  $B_0$   $\rightarrow$  uniform signal - cannot localize ...  
so how to image?
- Apply controlled distortion to  $B_0$
- $\rightarrow \rightarrow \rightarrow$  Spatially varying frequency

# Imaging

$$\omega_0 = \gamma B_0$$

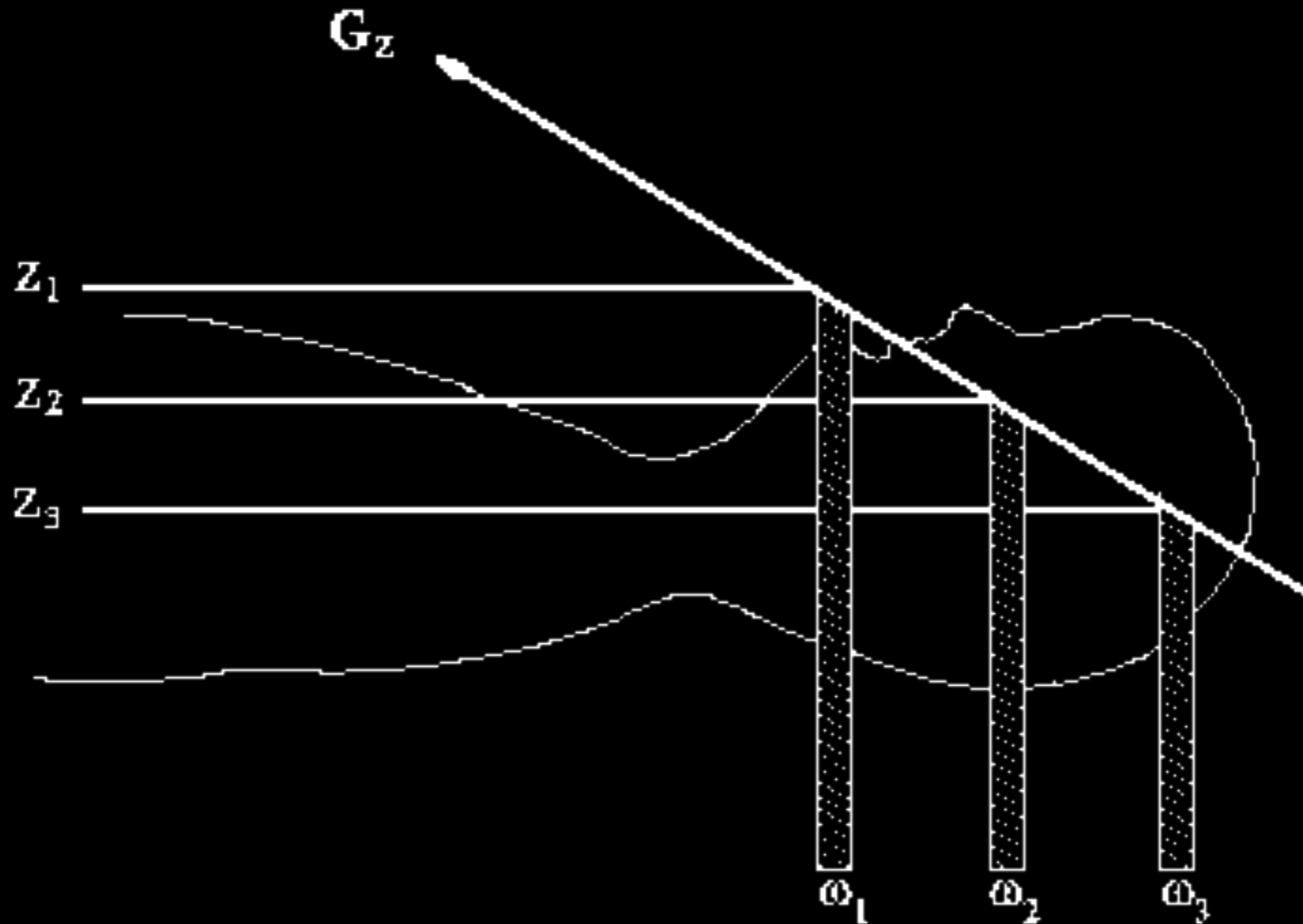
# Imaging

$$\omega_x = \gamma B_x$$

# Imaging

$$\omega_x = \gamma (B_0 + G_x)$$

# Imaging

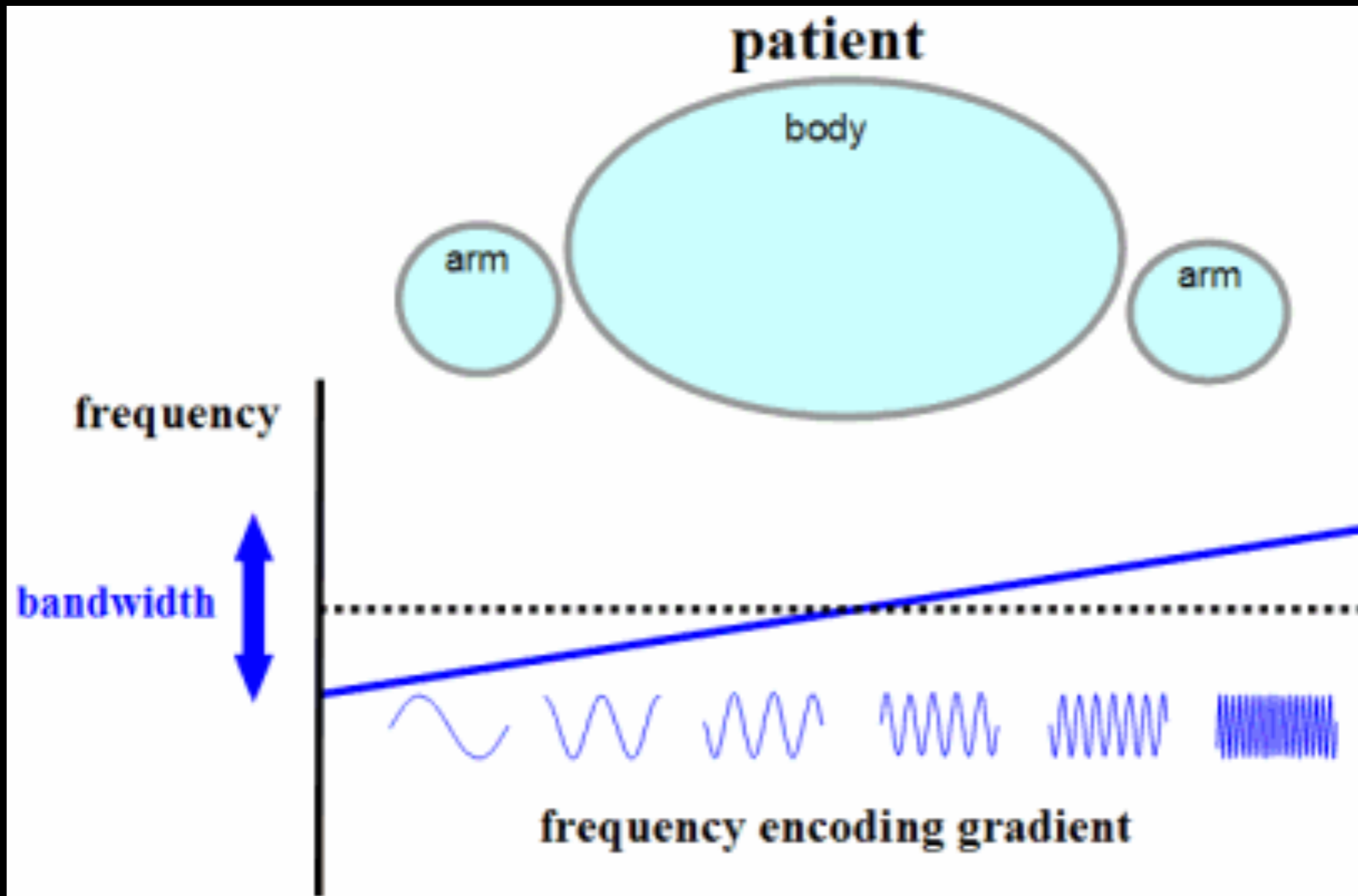


[http://sfb649.wiwi.hu-berlin.de/fedc\\_homepage/xplore/ebooks/html/csa/node255.html](http://sfb649.wiwi.hu-berlin.de/fedc_homepage/xplore/ebooks/html/csa/node255.html)

# Imaging

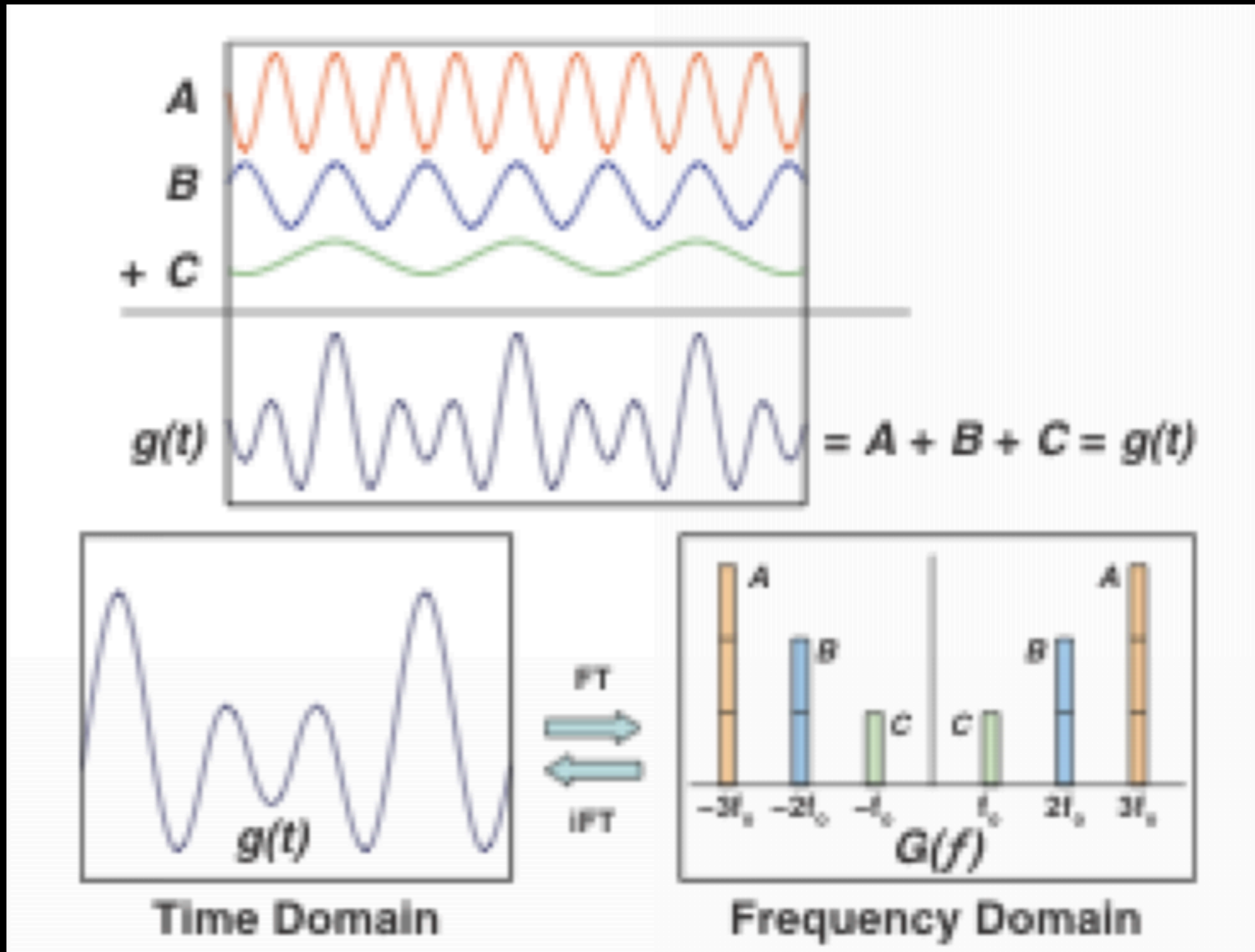
- Extend frequency change to other dimensions (x, y) for image encoding.
- 1<sup>st</sup> dimension → frequency encoding
- 2<sup>nd</sup> dimension → phase encoding

# Imaging



[http://www.revisemri.com/questions/creating\\_an\\_image/frequency\\_encoding\\_gradient](http://www.revisemri.com/questions/creating_an_image/frequency_encoding_gradient)

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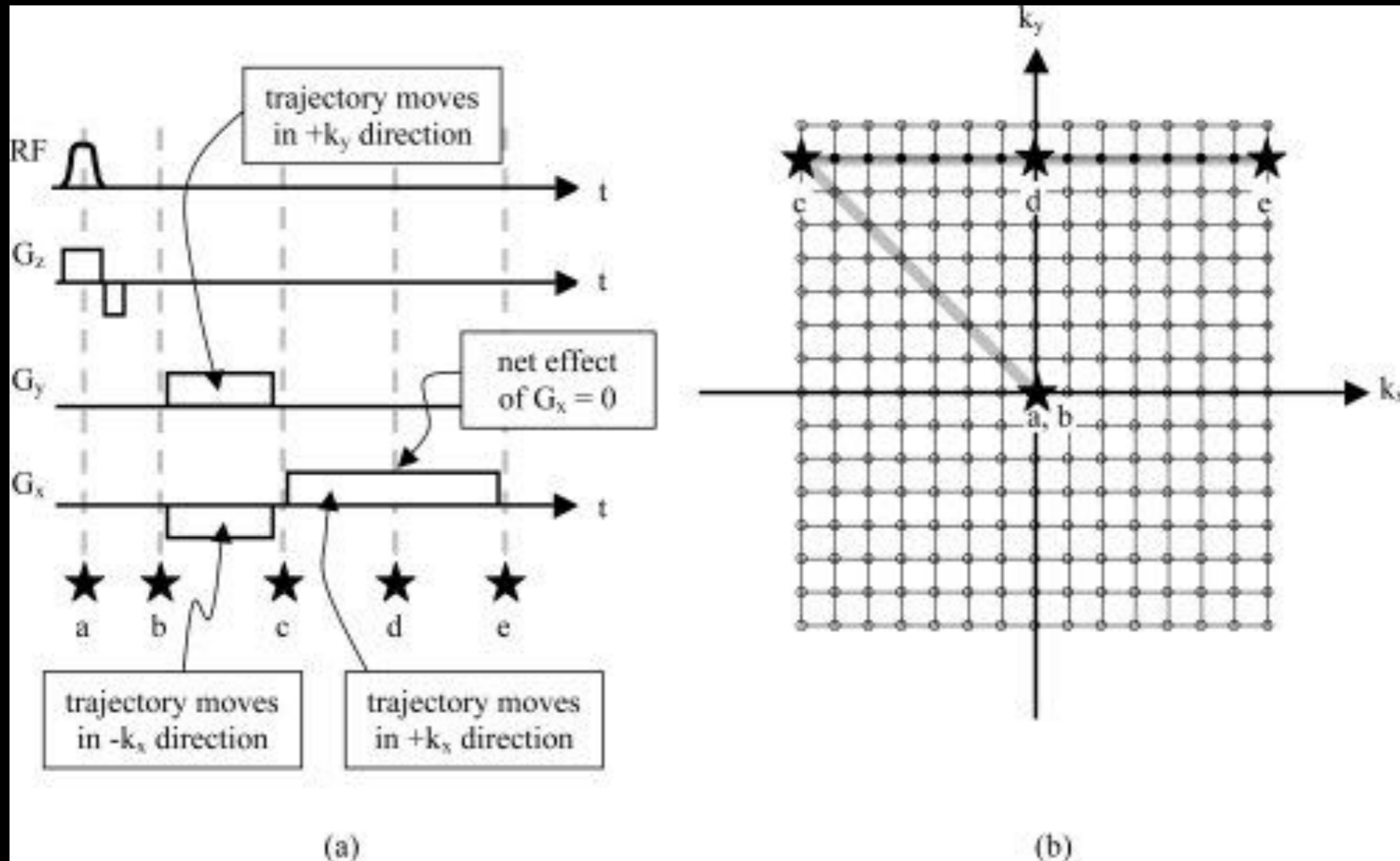




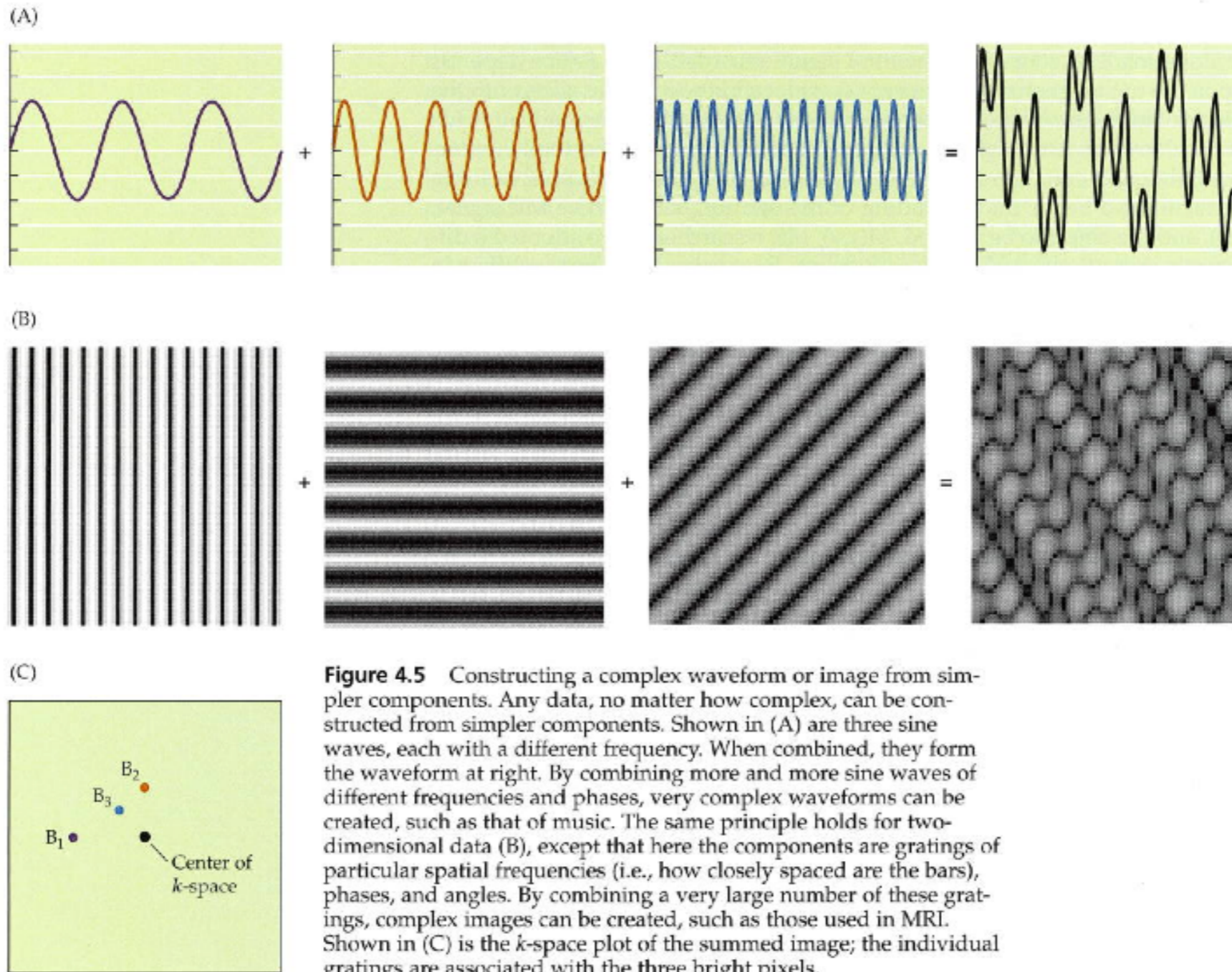
# Imaging

- Extend frequency change to other dimensions (x, y) for image encoding.
- 1<sup>st</sup> dimension → frequency encoding
- 2<sup>nd</sup> dimension → phase encoding
- Effects of gradients encodes “*k*-space”

# Imaging



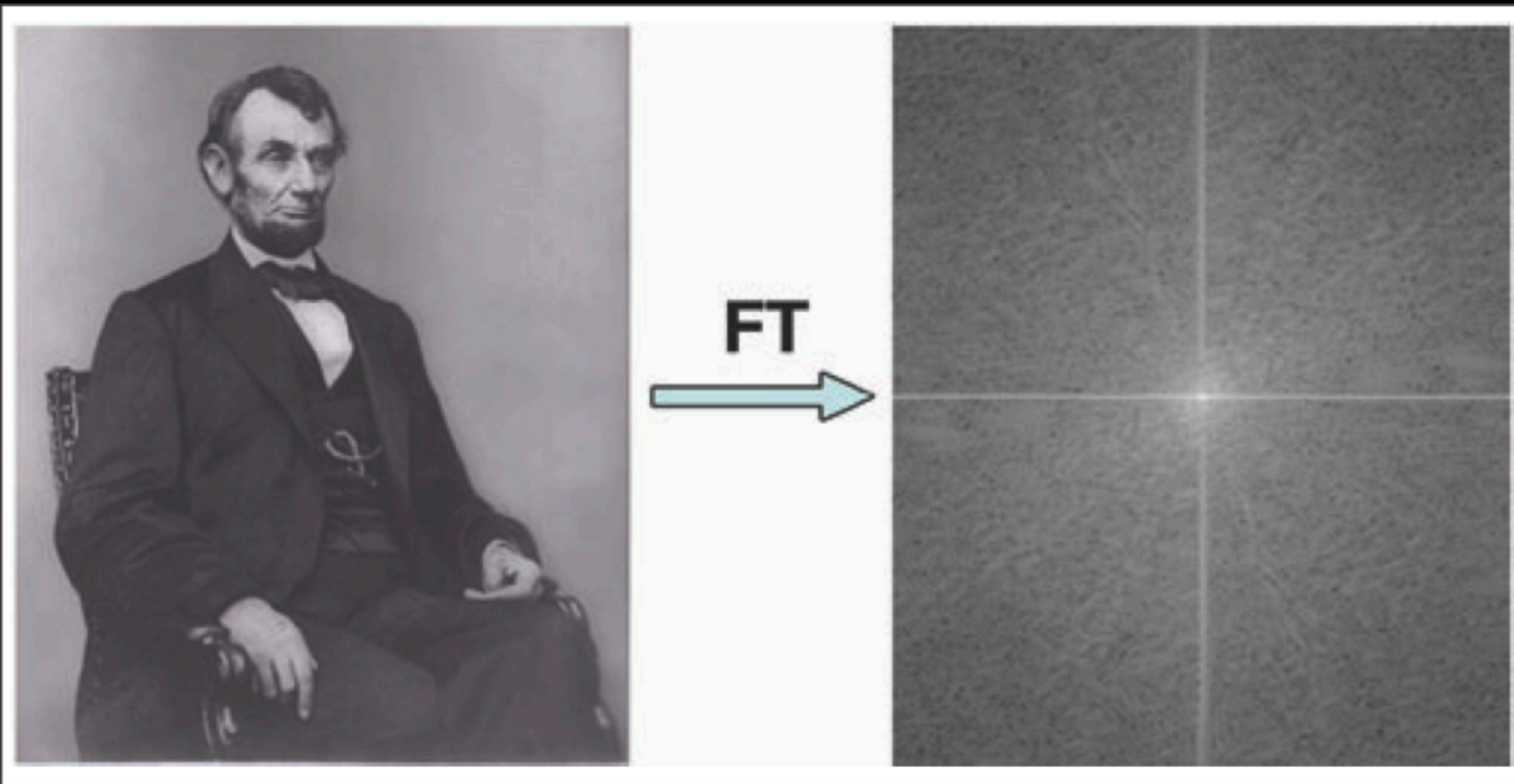
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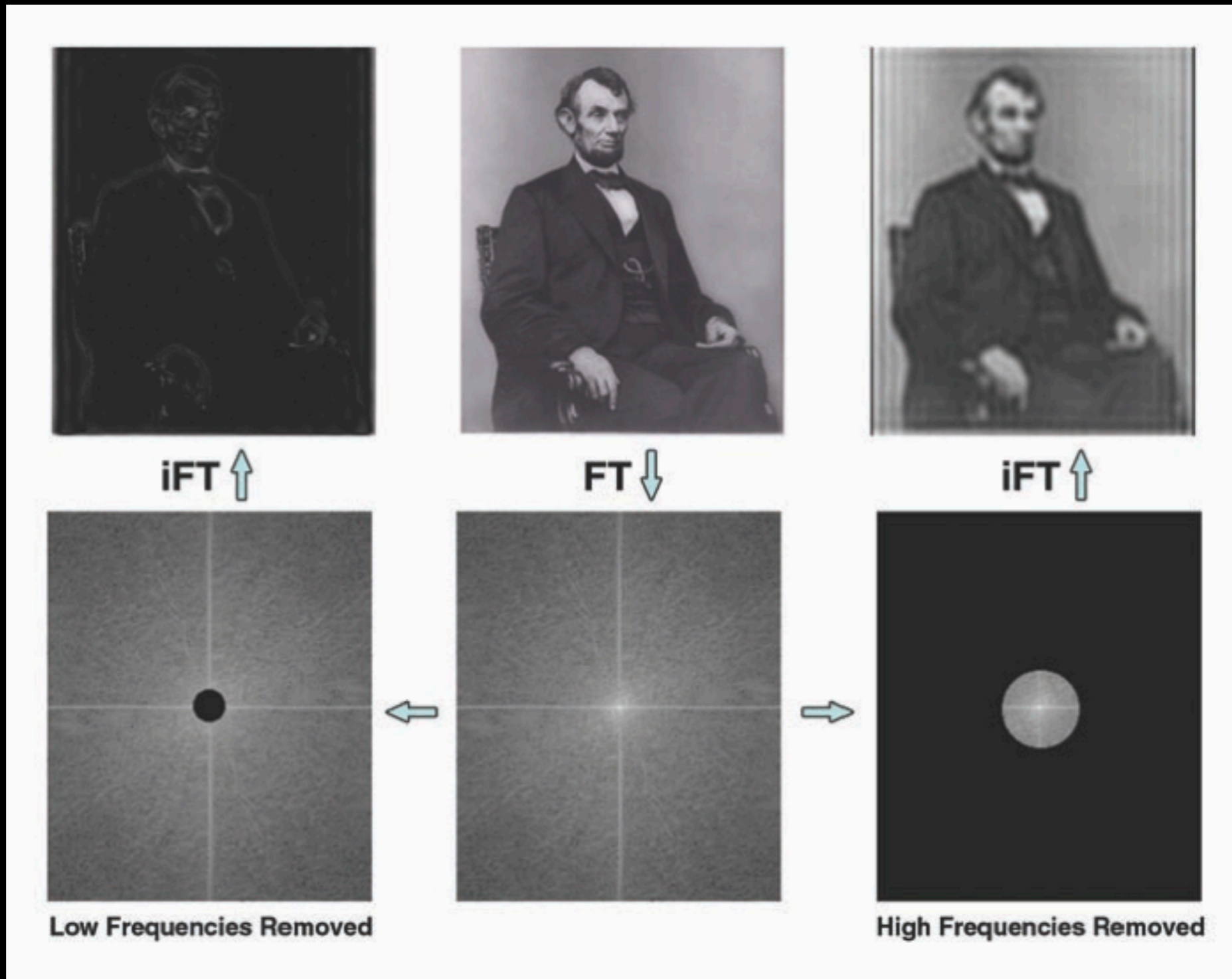
# Signal (Fourier Transform) Equation in MRI

$$s(t) = \int_{\vec{r}} M_{xy}(\vec{r}, 0) e^{-i2\pi\vec{k}(t)\cdot\vec{r}} d\vec{r}$$

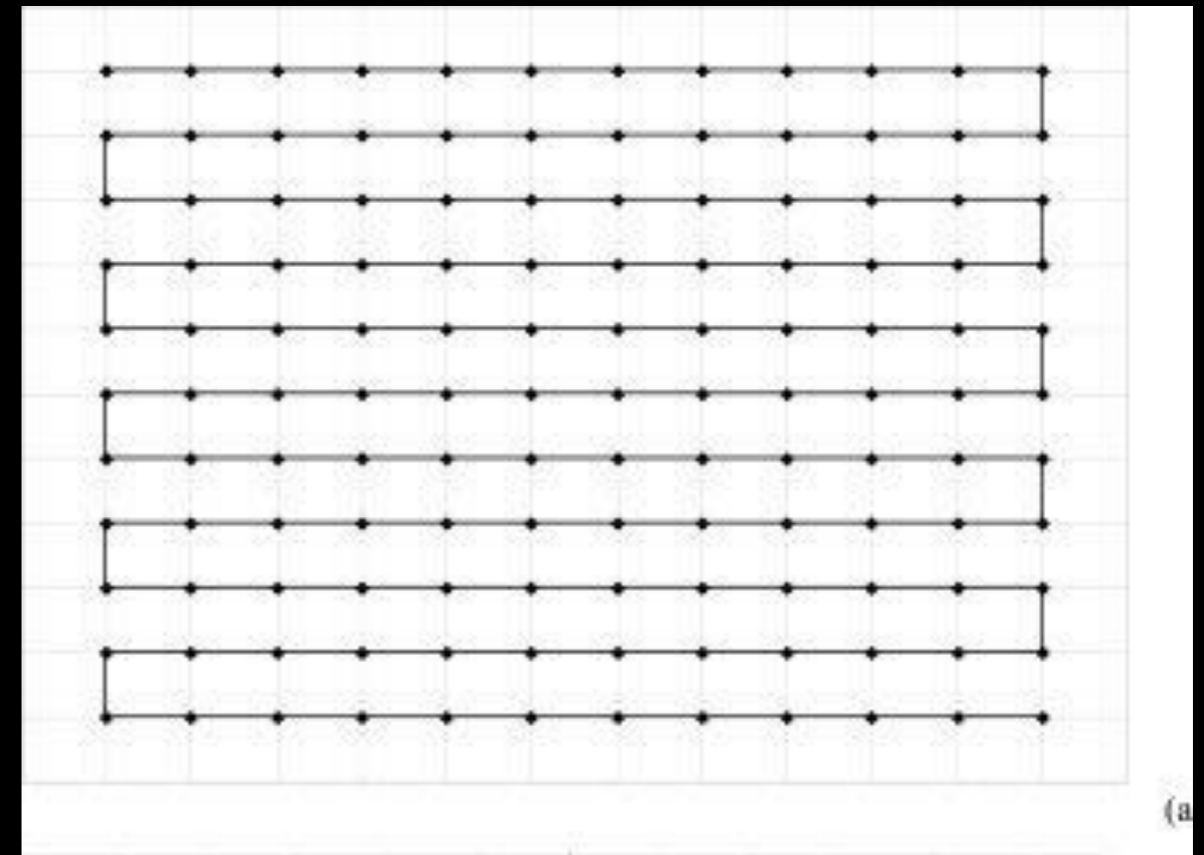
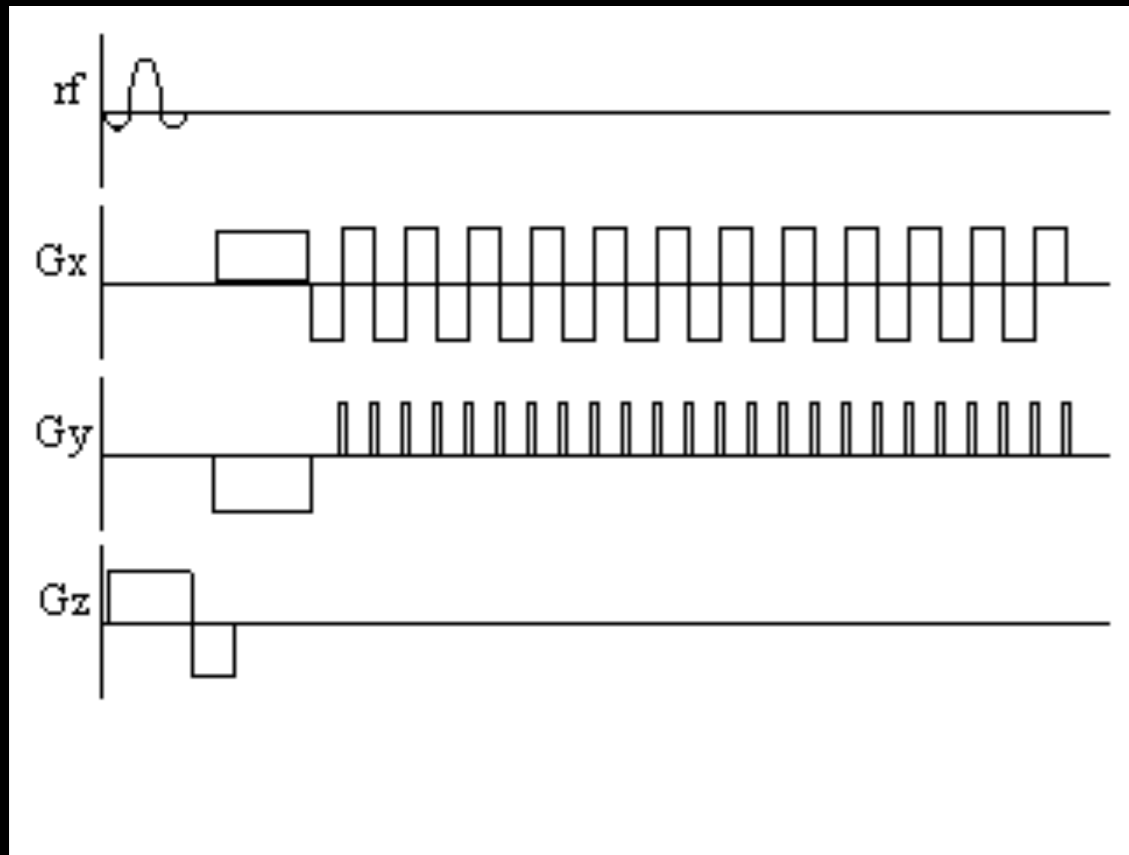
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# Imaging



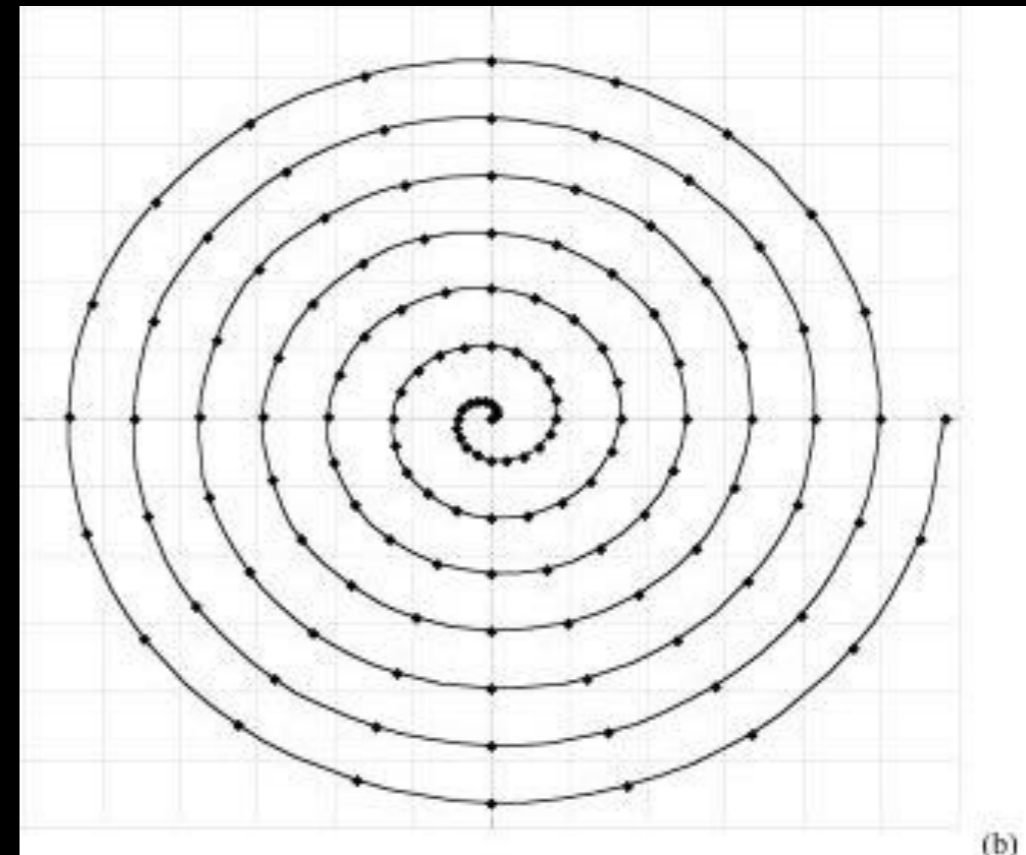
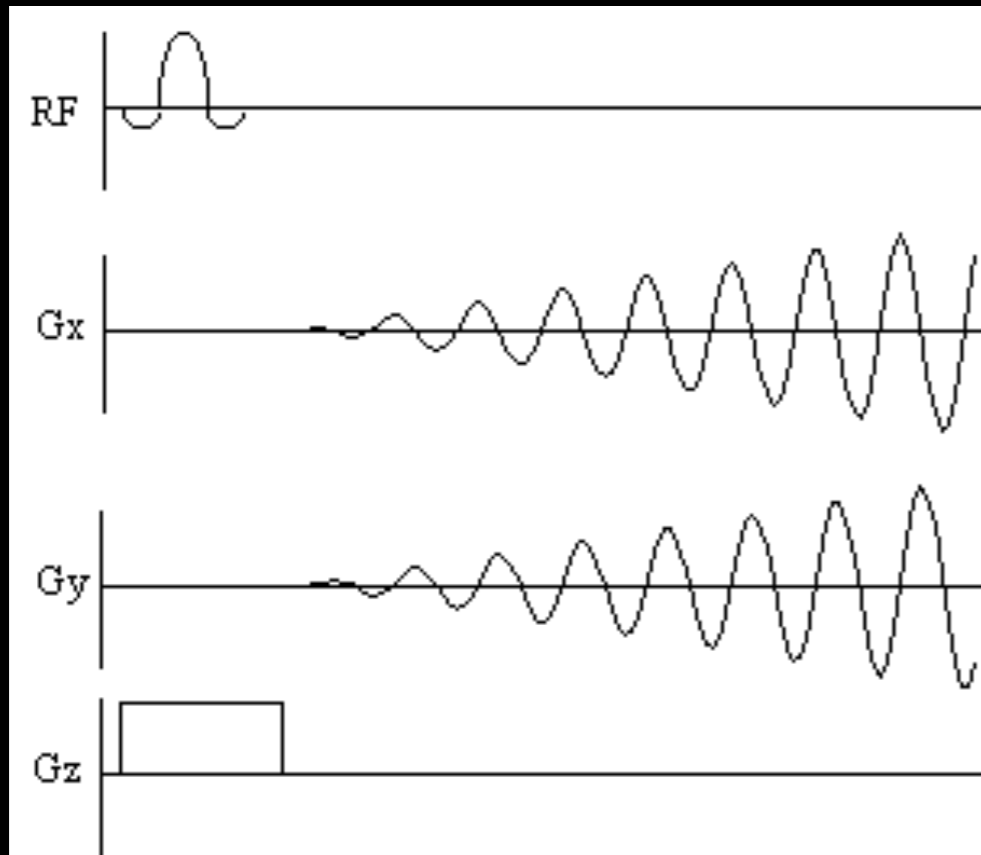
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[https://users.fmrib.ox.ac.uk/~stuart/thesis/chapter\\_2/section2\\_3.html](https://users.fmrib.ox.ac.uk/~stuart/thesis/chapter_2/section2_3.html)

JMRI, Paschal and Morris, DOI: 10.1002/jmri.10451

# Imaging



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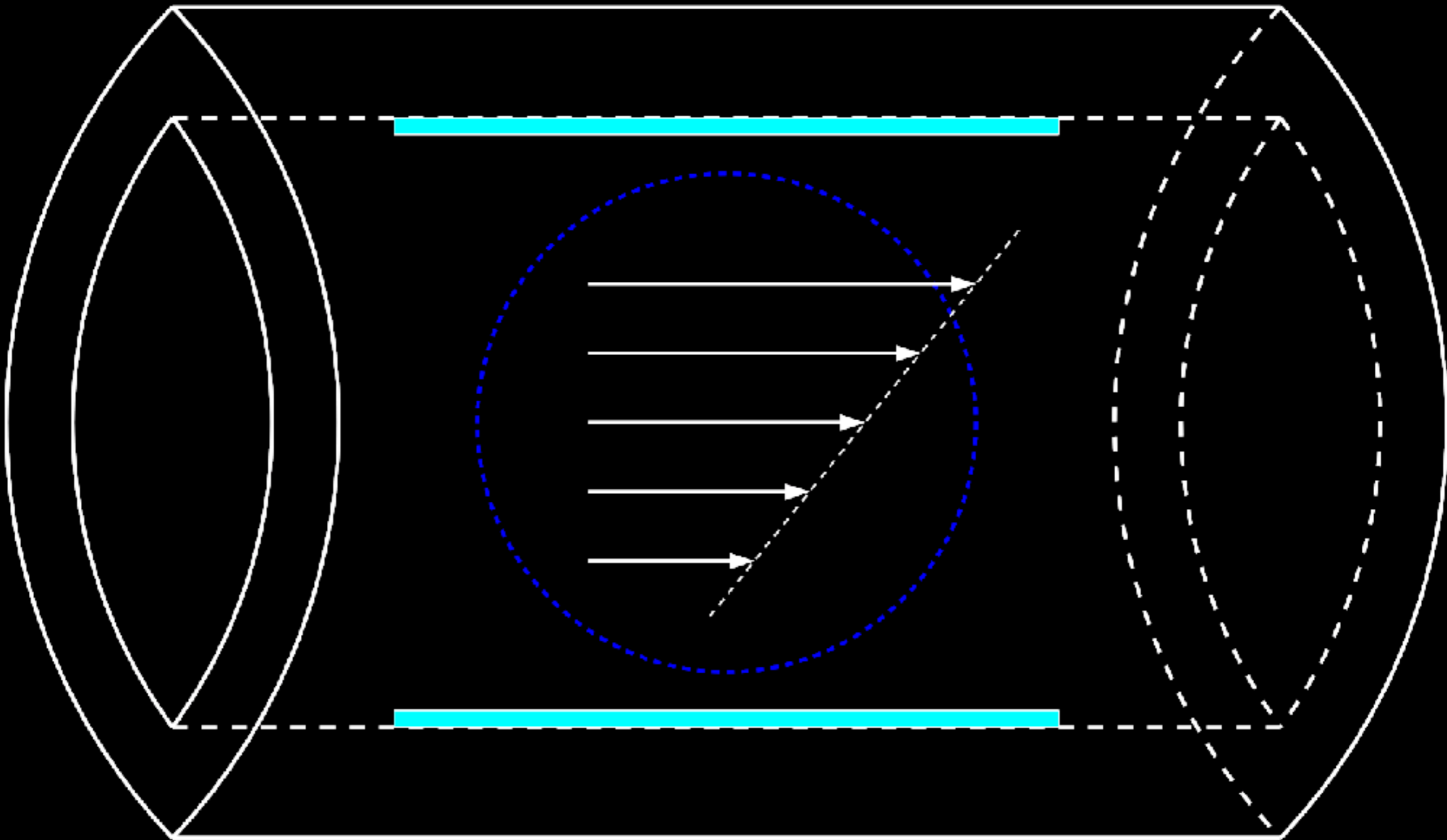
JMRI, Paschal and Morris, DOI: 10.1002/jmri.10451



# Gradients Nuts and Bolts

- Space / step size in  $k$ -space is inversely proportional to FOV.
- Extent in  $k$ -space is inversely proportional to voxel size.
- Covering  $k$ -space requires strong **and** fast gradients.
- Gradient switching rate FDA limited (200 mT/m/ms).  
Detectable below this threshold - subject comfort issues.
- “Local” gradient coils present a possible solution to address FDA limits and power requirements.

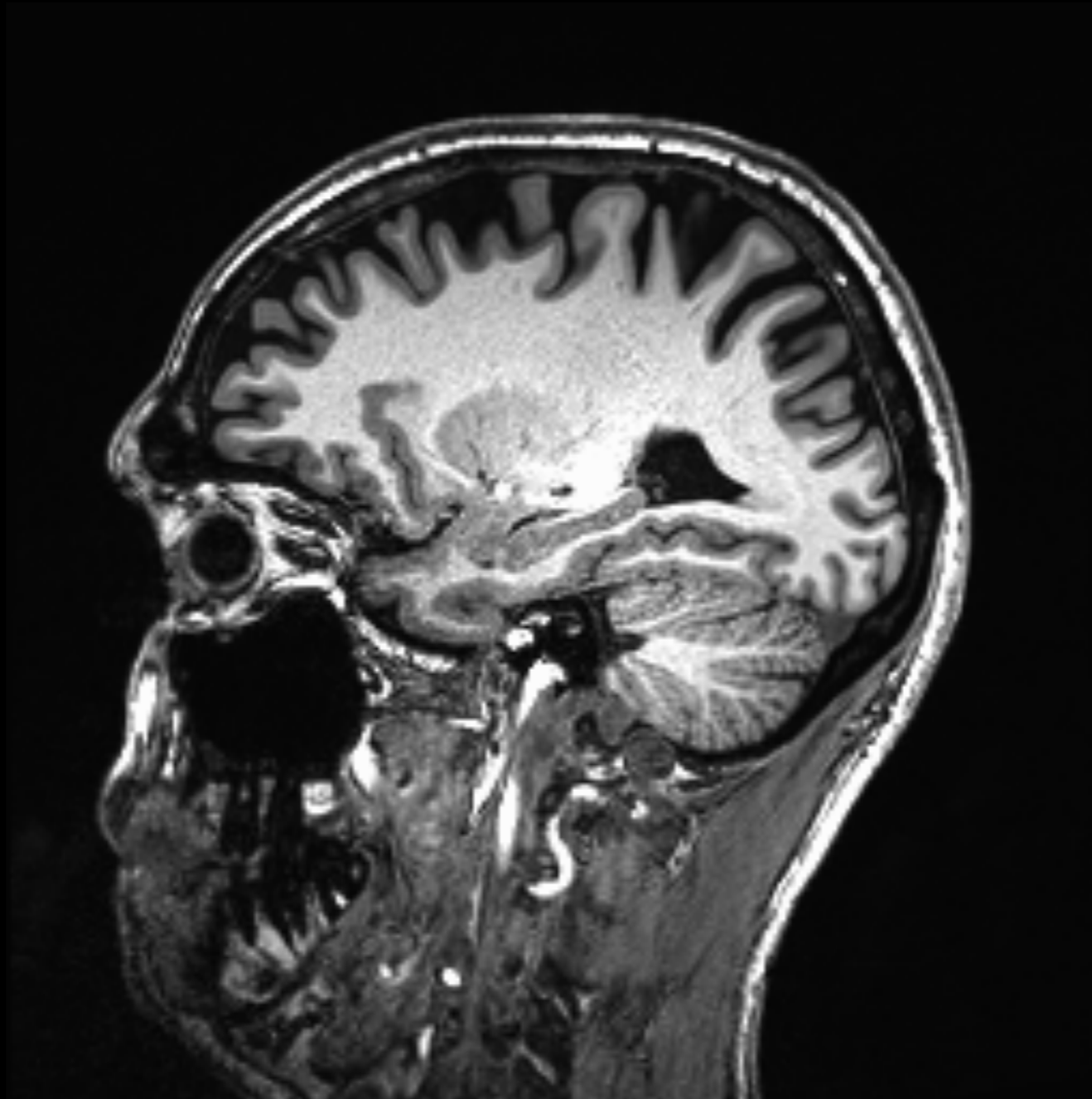
# Gradients Nuts and Bolts



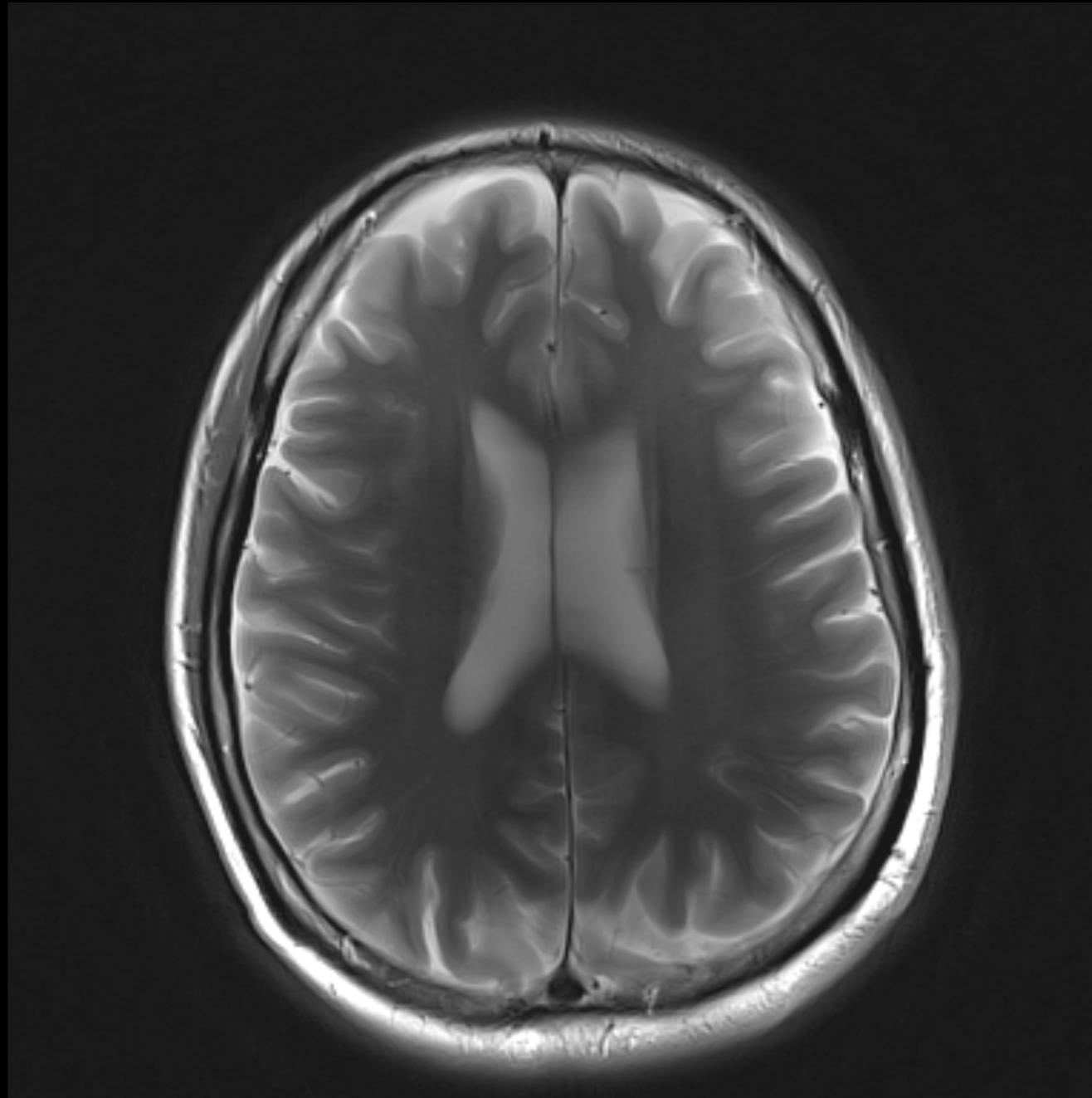
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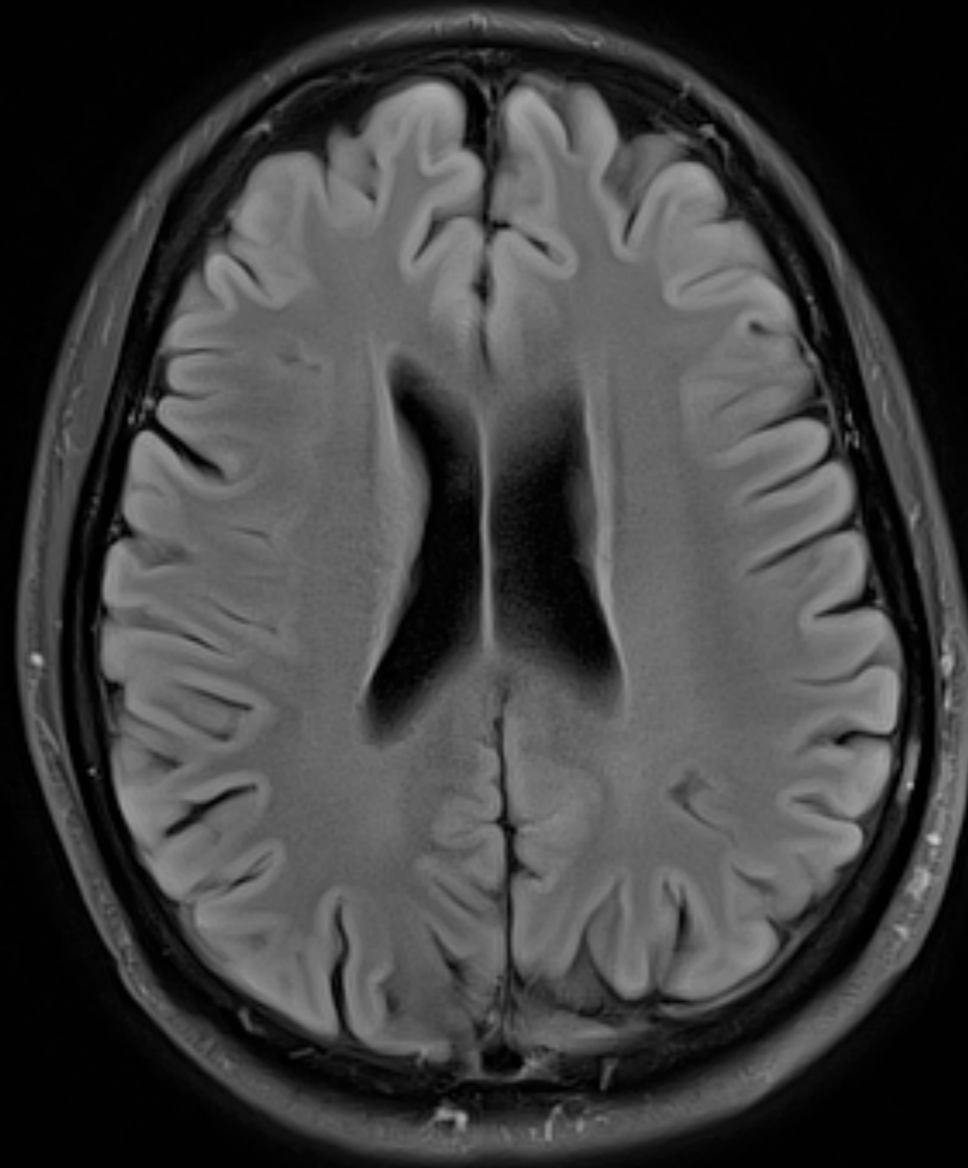
# Contrast - T<sub>1</sub>



# Contrast - T<sub>2</sub>

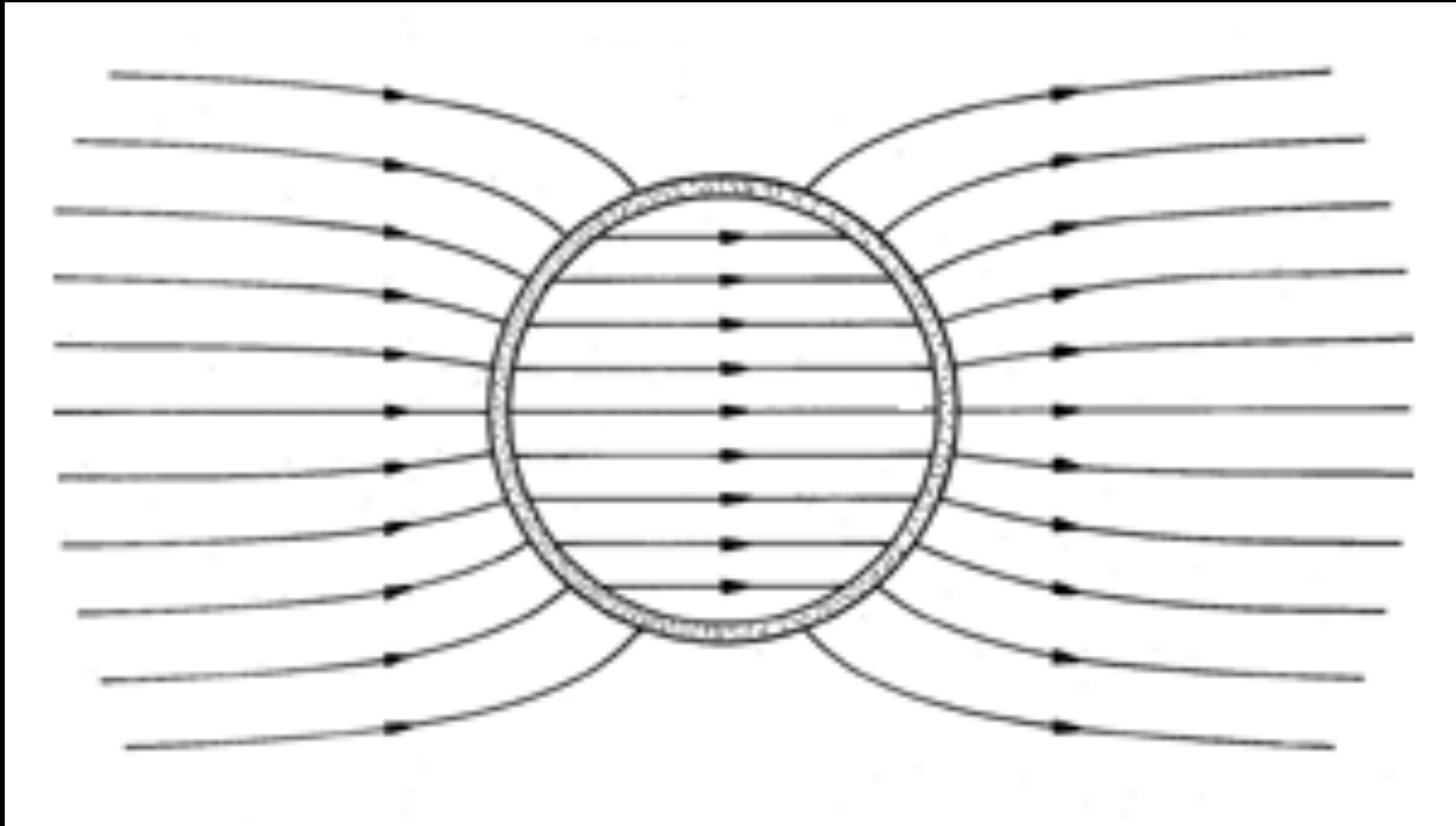


# Contrast - T<sub>2</sub> FLAIR



# Contrast - BOLD

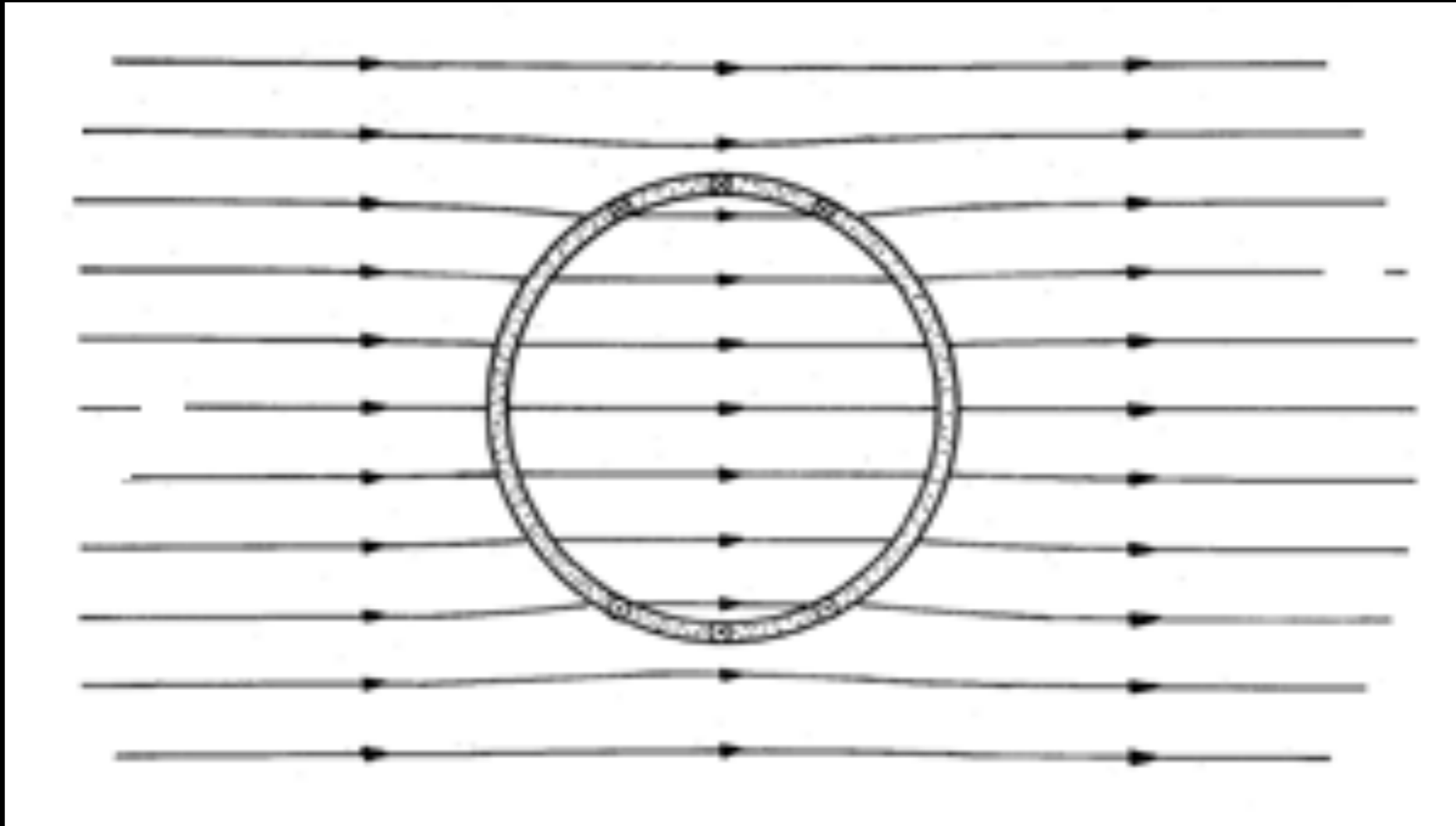
# Contrast - BOLD



[http://web.mit.edu/6.013\\_book/www/chapter10/10.4.html](http://web.mit.edu/6.013_book/www/chapter10/10.4.html)

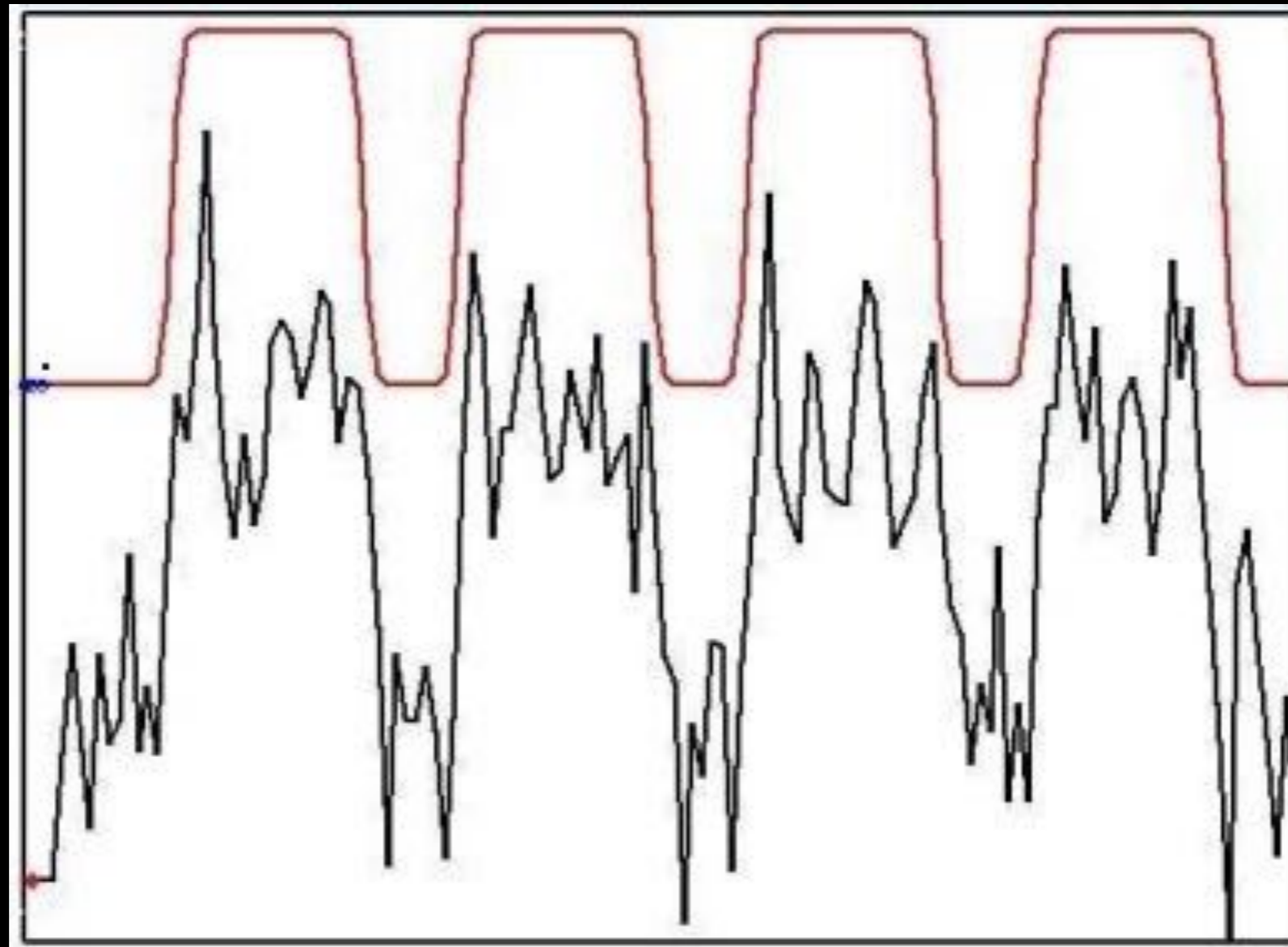


# Contrast - BOLD

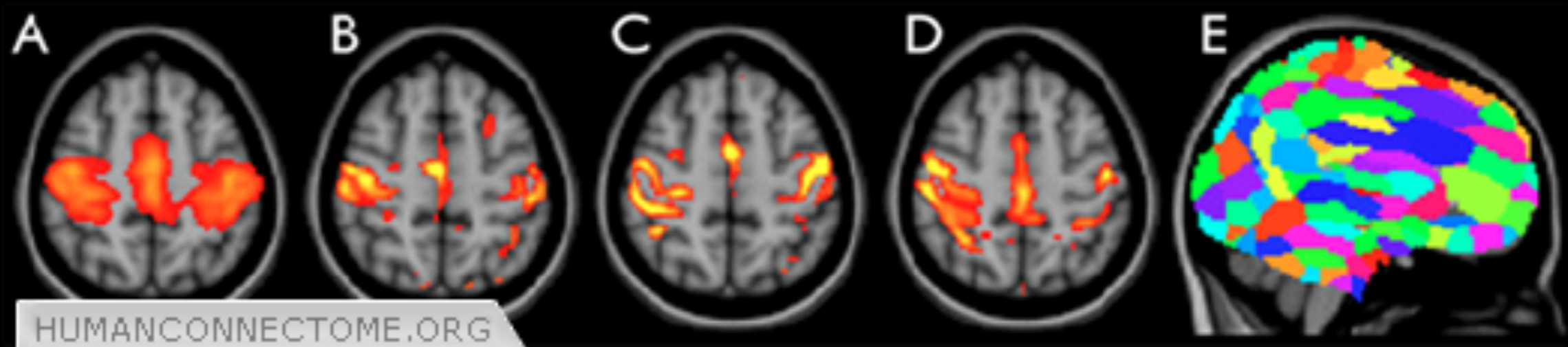


[http://web.mit.edu/6.013\\_book/www/chapter10/10.4.html](http://web.mit.edu/6.013_book/www/chapter10/10.4.html)

# Contrast - BOLD



# Contrast - BOLD



# Contrast

- BOLD ==  $T_2^*$
- FLAIR (Fluid Attenuated Inversion recovery)
- Magnetization Transfer (MT) - MRM, 1989 Vol 10:135-144 - Wolff and Balaban
- Perfusion imaging - MRM, 1992 Vol 23:37-45 - Detre et.al.
- Diffusion imaging - Nature Reviews Neuroscience 4, 469-480 (June 2003) - DOI:10.1038/nrn1119 (review paper)
- Phase imaging - PNAS, 2007 Vol 104(28):11796-11801 - Duyn et.al.
- ...

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MRI Scanners 33

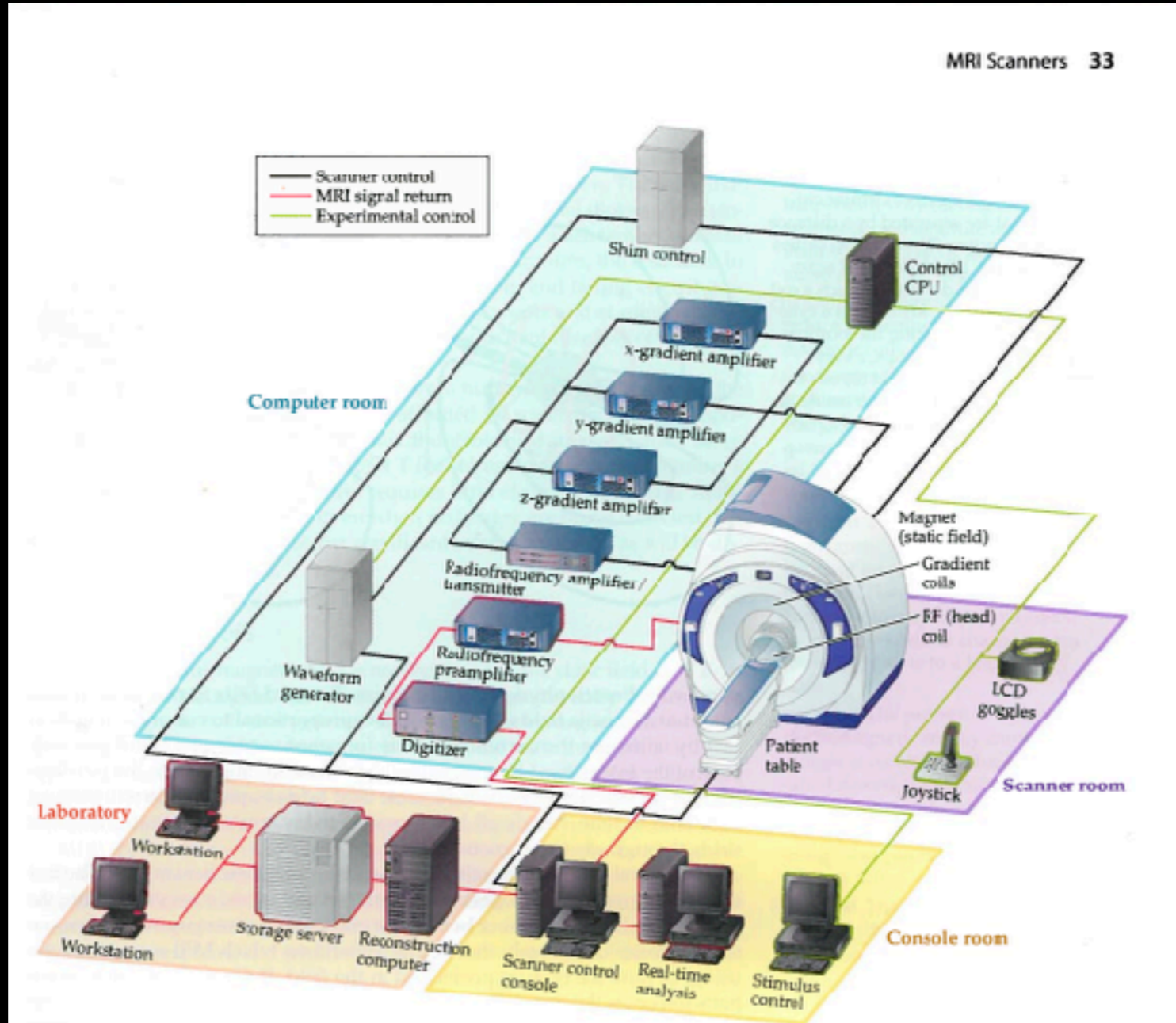


Figure 2.7 Schematic organization of the fMRI scanner and computer control systems. Two systems are important for fMRI studies. The first is the hardware used for image acquisition. In addition to the scanner itself, this hardware consists of a series of amplifiers and transmitters responsible for creating the gradients and pulse sequences (shown in black), and recorders of the MR signal from the head coil (shown in red). The second system is responsible for controlling the experiment in